

1 Moving beyond small solute clearance; what evidence is there for more
2 permeable dialyzers and haemodiafiltration ?

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6 Andrew Davenport FRCP

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9 UCL Centre for Nephrology, Royal Free Hospital, University College London
10 Medical School, London

11

12 Andrew Davenport andrewdavenport@nhs.uk

13

14

15

16 Address for correspondence

17

18 Andrew Davenport

19 UCL Centre for Nephrology

20 Royal Free Hospital

21 University College London

22 Rowland Hill Street

23 London NW3 2PF

24

25 tel 44-2074726457

26 fax 44-2073178591

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43 Abstract

44 Dialysers were initially developed for diffusive clearance of uraemic
45 toxins. Diffusion most effectively clears small uncharged solutes from plasma
46 water, such as urea. Sessional urea clearance targets have been shown to be
47 important for short term patient survival, but over the longer term, although
48 low flux dialysis can prolong patient survival, accumulation of middle sized
49 uraemic toxins, such as β_2 microglobulin can lead to disabling arthropathy.
50 Although the introduction of high flux dialysers, designed to increase β_2
51 microglobulin clearance, has reduced the prevalence of arthropathy, this has not
52 been translated into a demonstrable significant improvement in patient survival.
53 However, analysis of individual patients recruited into trials of haemo-
54 diafiltration reported that greater convective clearance was associated with
55 better survival, although the individual trials reported mixed outcomes. Most
56 haemodiafiltration trials were not designed to study the effect of convective
57 dose, so although reported patient survival was greater for those receiving
58 greater convective volume exchange, these results could potentially be
59 confounded by patient or centre effects. An alternative approach to increasing
60 middle sized solute clearances would be to use more permeable dialyzers, but as
61 yet there are no trials reporting survival with larger cut-off dialysers. As such,
62 although there is increasing evidence that increasing middle sized molecular
63 uraemic solute clearance is associated with improved patient survival, further
64 prospective trials are required to determine whether as with K_t/V_{urea} there is

65 a threshold effect of how much convective or middle sized solute clearance is
66 required to improve patient survival.

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68 Introduction

69 Haemodialysis is a well-established treatment for patients with chronic
70 kidney disease. Initially all dialyzer membranes were low-flux which allowed
71 solute clearance by diffusion. Urea, a by-product of protein turnover,
72 accumulates in kidney failure patients, and being a relatively small uncharged
73 molecule free in plasma water is readily cleared by diffusion. The National Co-
74 operate Dialysis Study demonstrated that a minimum amount of dialysis
75 sessional urea clearance was required to maintain health over 12 months [1].
76 This was described as Kt/V_{urea} to allow for comparison between different sized
77 patients, and subsequently the sessional target was increased from 1.0 to 1.2 by
78 consensus. Later trials, such as the Haemodialysis trial (HEMO study) did not
79 demonstrate any significant overall survival advantage for greater dialyser
80 sessional urea clearance [2]. However, although some dialysis centres, such as
81 Tassin in France, reported impressive patient survival with low-flux dialysis,
82 after 10 years they noted that their patients were at greater risk of
83 developing carpal tunnel compression and arthropathy [3]. These complications
84 were associated with the deposition of β 2-microglobulin (β 2M) [4].

85

86 High-flux haemodialysis

87

88 Loss of kidney function leads to the accumulation of compounds which are
89 normally filtered by the glomerulus and then reabsorbed into the proximal
90 tubular cells and degraded. As such, the serum concentrations of many
91 inflammatory mediators and hormones increase in the dialysis patient.
92 Traditional low flux dialysis does not adequately clear middle sized uraemic
93 toxins, defined as a molecular weight > 500 Daltons, and as such these
94 accumulate in dialysis patients (table 1). Dialyzer flux is currently defined by
95 β 2M clearance, with increasing clearance from low to mid to high-flux, with high
96 flux dialysers having a β 2M sieving coefficient of > 0.6 [5]. As such dialyser flux
97 is independent of membrane composition [6]. Although synthetic high flux
98 membranes were developed in the 1980s, due to cost differentials, only a small
99 proportion of patients were initially treated with these dialysers. The use of
100 high-flux dialysers was reported to reduce the incidence of carpal tunnel
101 neuropathy and arthropathy associated with β 2M deposition in observational
102 reports [7]. Despite the reduction in the long-term complications of β 2M
103 deposition, prospective shorter-term studies of high-flux dialysis did not show
104 an overall survival advantage for treatment with high flux dialysers [2,8].
105 Although sub-analysis of the HEMO study did suggest a survival advantage with
106 high flux haemodialysis for patients who had been previously dialysed for more
107 than 3.5 years, potentially suggesting an advantage for high flux haemodialysis
108 for those patients who had lost residual renal function [2]. In addition, re-
109 analysis of HEMO study did suggest an association between increasing serum
110 β 2M and mortality [9]. However residual renal function is a major determinant

111 of serum β_2M , and preservation of residual renal function is associated with
112 survival. A later prospective European trial, the Membrane Permeability Outcome
113 (MPO) study reported that high flux dialysis increased survival for some defined
114 patient groups, namely those with diabetes and reduced serum albumin, [8].

115 In addition to the increased diffusional clearance of middle molecules
116 (>500 Daltons) from the plasma water, there is also increased convective
117 clearance compared to low flux haemodialysers, not only due to ultrafiltration,
118 but also convective clearance. As, depending upon the hydraulic permeability of
119 the high flux dialyser, there will be a varying amount of internal diafiltration
120 due to the relative differences in hydrostatic pressures at the dialyser inflow
121 and out-flow between the blood and dialysate compartments [10].

122

123 Haemodiafiltration

124 On the assumption that middle sized uraemic solutes contribute to the
125 increased risk of mortality for dialysis patients, then there has been a strive to
126 increase larger solute clearance. As the trials of high-flux dialysis did not
127 demonstrate a substantial survival benefit, there has been increased interest in
128 the additional convective clearance obtained with haemodiafiltration. There
129 have been a number of trials of haemodiafiltration, and although
130 haemodiafiltration reduced the risk of intra-dialytic hypotension, most of the
131 trials did not show any survival benefit [11-13]. However, these trials were not
132 designed to determine whether the amount of convective clearance was
133 important. As there is a variable amount of internal diafiltration with high-flux

134 dialysis, then re-analysis of these trials showed a survival advantage for those
135 patients who had received the greatest dose of convective clearance. This
136 concept was supported by one prospective trial of high volume on-line
137 haemodiafiltration [14], and the individual patient analyses of these trials
138 [15,16]. As such, this would suggest that there may be a survival advantage for
139 the greater convective clearance achieved with higher volume
140 haemodiafiltration. Only one study included patients who could achieve a
141 prespecified amount of convective volume exchange. As such the amount of
142 convective volume exchange in the other studies could have been confounded, as
143 patients who can achieve higher convective volumes may have been generally
144 healthier with better vascular access than those who cannot [17]. Other studies
145 have reported that centre practices may also influence the convection volumes
146 exchanged [18].

147 To minimise costs, most centres practice post-dilutional on-line
148 haemodiafiltration [19], but this requires faster blood flows to achieve the
149 higher convective target volumes now proposed (Table 2). Different dialysis
150 machine manufacturers use different algorithms to regulate the amount of
151 convection according to the pre- and post-dialyser pressures, as too high a
152 filtration fraction risks haemoconcentration within the dialyser and clotting
153 within the fibre bundle. Although haemodiafiltration requires a high flux
154 dialyser, high flux dialysers differ in hydraulic permeability and design. To allow
155 for the removal of large volumes of plasma water, hydraulic permeability is
156 important. However, as the hydrostatic pressure in the blood compartment falls

157 with increasing distance from the blood inlet, there will come a point when the
158 relative pressures in blood and dialysate compartments are similar and no net
159 convection takes place, and distally greater pressure in the dialysate
160 compartment will lead to dialysate entering the blood compartment. Whereas
161 greater surface area is important to increase diffusional losses, the length of
162 the dialyser designed for haemodiafiltration should be shorter compared to that
163 designed for diffusion, so that convective clearance occurs all along the fibre
164 length. Similarly, whereas dialysers designed for diffusion traditionally have
165 very narrow internal fibre diameters to minimise the distance for diffusion,
166 designed to increase diffusive clearance, narrow diameter fibres potentially
167 increase the risk of haemoconcentration and clotting when used for
168 haemodiafiltration. So, high flux dialysers designed for haemodiafiltration have
169 wider internal diameter fibres [20].

170 In paediatric practice, blood flows are generally much slower than in
171 adult practice, and as such pre-dilutional haemodiafiltration is the more
172 commonly performed. Pre-dilution reduces haemoconcentration, and although in
173 theory would allow greater convective clearances, in clinical practice the removal
174 of larger solutes such as alpha-1 macroglobulin do not differ between pre- and
175 post-dilution modes, due to increased membrane adsorption with the post-
176 dilution mode. Pre-dilution mode requires greater exchange volumes, and as such
177 mid-dilution dialyzers have been developed to try and obtain some of the
178 benefits of pre-dilution, but without using very large volumes of dialysate.

179 As large volumes of dialysate are directly infused into patients during
180 haemodiafiltration, then ultra-pure dialysis water is required. In theory, ultra-
181 pure water should be used for high flux haemodialysis due to the possibility of
182 internal diafiltration with some dialysate passing into the blood compartment of
183 the dialyser. These large volumes of dialysate passing directly into the patient's
184 blood stream increase cooling during the treatment session, and it has been
185 argued that the benefits reported with haemodiafiltration may be due to the
186 additional cooling and cardiovascular stability, rather than any increased middle
187 sized solute clearance [21]

188

189 Increased permeability dialysers

190 An alternative approach to haemodiafiltration is to use a dialyzer with
191 enhanced permeability to middle sized solutes. This potentially has advantages
192 over haemodiafiltration, in that the dialysis machine does not require an
193 additional pump for the re-infusion fluid, and may not need the strict volumetric
194 control to cope with the large volumes of fluid exchanged during
195 haemodiafiltration, and the additional cost of the re-infusion line [22]. A series
196 of larger pore size superflux dialysers were developed for the intensive care
197 setting, designed to increase the removal of cytokines and other inflammatory
198 mediators [23]. However, these membranes also led to a greater loss of albumin
199 compared to high flux dialysers, and so a new generation of what have been
200 termed medium-cut off dialysers have now been developed, which allow similar
201 or even increased removal of middle sized solutes compared to

202 haemodiafiltration, but without an increased albumin loss [24]. These dialysers
203 have only been recently introduced into clinical practice, and as yet there are no
204 prospective studies to determine whether these offer a survival advantage.

205

206 Solute Adsorption

207 Although haemodiafiltration and medium-cut off dialysers increase the
208 removal of water soluble middle sized uraemic toxins they do not increase the
209 clearance of protein bound uraemic toxins. Some of the more hydrophobic
210 polymers used to manufacture dialysers, such as polymethylmethacrylate
211 (PMMA) have an affinity to adsorb proteins, and although this may increase the
212 clearance of protein bound solutes, increasing protein deposition along the
213 dialyser membrane may also reduce diffusional solute clearances [25].

214 Protein bound solutes can be removed by adsorption. So, an alternative
215 approach has been to create mix-matrix membranes, by coating the dialysate
216 side of standard dialyser fibres with activated carbon or other adsorptive
217 particles. Although these mixed membranes have been shown to increase
218 protein bound solutes in the laboratory, they are currently not commercially
219 available [26]. Sorbent cartridges or monoliths can also be used to effectively
220 remove protein-bound solutes in laboratory studies [25], but again are not
221 currently available for clinical usage.

222

223 Summary

224 Although some centres have reported substantial patient survival with
225 low-flux haemodialysis, in the longer term although surviving these patients
226 developed problems associated with β 2M deposition in and around joints and
227 bones, and visceral deposition. Although high flux haemodialysis reduces the
228 prevalence of complications associated with β 2M deposition, studies have failed
229 to demonstrate a significant survival advantage. Increasing middle sized solute
230 clearance by high volume haemodiafiltration appears to improve patient survival,
231 however as most studies were not designed to investigate the effect of
232 convection volume, this potential improvement in survival requires further study.
233 Similarly, there is currently no data on whether increased middle molecule
234 clearance using middle-cut off dialysers improves outcomes. None of these
235 dialysis techniques in current clinical practice effectively clear protein bound
236 solutes, and newer approaches are required to remove these putative toxins in
237 the anuric haemodialysis patient .

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377 Table 1: Middle sized (> 500 Daltons) solutes that potentially increase in the
 378 serum of patients with kidney failure
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Adrenomedullin
Advanced glycosylation end-products
Angiogenin
Atrial natriuretic peptide
Basic fibroblast growth factor
β endorphin
β 2 microglobulin
Brain natriuretic peptide
Calcitonin gene related peptide
cholecystokinin
Clara cell protein
Complement factor D
Cystatin C
Cytokines (interleukin 1β , interleukin 6, interleukin 18, tumour necrosis factor α)
Degranulation inhibiting protein 1
δ Sleep inducing peptide
Des acyl-ghrelin
Endothelin
Guanylin
Homocysteine
Hyaluronic acid
κ Light chains
λ Light chains
Leptin
Methionine enkephalin
Motiline
Neuropeptide Y
Oxalic acid
Oxidised low density lipoprotein
Parathyroid hormone
Resistin
Substance P
Uroguanylin
Vasoactive intestinal peptide
Vasopressin

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386 Table 2. Ideal Equipment required for high volume on-line haemodiafiltration
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Site	equipment
Dialysis machine	Pump for replacement solution
	Pre and post dialyser pressure monitoring
	Software to regulate filtration fraction
	Volumetric pump
	Re-infusion line
Dialyser	High flux
	High hydraulic permeability
	Wider internal diameter fibres
Dialysis water	Ultra-filter
	Ultrapure quality

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