Filtration-histogram based magnetic resonance texture analysis (MRTA) for glioma IDH and 1p19q genotyping

Running Title: MRTA for glioma IDH/1p19q genotyping

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Abbreviations:

Isocitrate Dehydrogenase - IDH

Isocitrate Dehydrogenase mutation - IDH^{mut}

Isocitrate Dehydrogenase wild type - IDH^{wt}

Isocitrate Dehydrogenase mutation gliomas with combined deletion of the short arm of chromosome 1 and the long arm of chromosome 19 - $IDH^{mut}1p19q^{del}$

Isocitrate Dehydrogenase mutation gliomas with intact short arm of chromosome 1 and the long arm of chromosome 19 - $IDH^{mut}1p19q^{int}$

Magnetic resonance imaging texture analysis - MRTA

Spatial scale filter – SSF

World Health Organization - WHO

Standard deviation – s.d.

Mean positive pixels – m.p.p.

Abstract

Background To determine if filtration-histogram based texture analysis (MRTA) of clinical MR imaging can non-invasively identify molecular subtypes of untreated gliomas.

Methods Post Gadolinium T1-weighted (T1+Gad) images, T2-weighted (T2) images and apparent diffusion coefficient (ADC) maps of 97 gliomas (54=WHO II, 20=WHO III, 23=WHO IV) between 2010 and 2016 were studied. Whole-tumor segmentations were performed on a proprietary texture analysis research platform (TexRAD, Cambridge, UK) using the software's freehand drawing tool. MRTA commences with a filtration step, followed by quantification of texture using histogram texture parameters. Results were correlated using non-parametric statistics with a logistic regression model generated.

Results T1+Gad performed best for IDH typing of glioblastoma (sensitivity 91.9%, specificity 100%, AUC 0.945) and ADC for non-Gadolinium-enhancing gliomas (sensitivity 85.7%, specificity 78.4%, AUC 0.877). T2 was moderately precise (sensitivity 83.1%, specificity 78.9%, AUC 0.821). Excellent results for IDH typing were achieved from a combination of the three sequences (sensitivity 90.5%, specificity 94.5%, AUC=0.98). For discriminating 1p19q genotypes, ADC produced the best results using unfiltered textures (sensitivity 80.6%, specificity 89.3%, AUC 0.811).

Conclusion Preoperative glioma genotyping with MRTA appears valuable with potential for clinical translation. The optimal choice of texture parameters is influenced by sequence choice, tumour morphology and segmentation method.

Introduction

Gliomas exhibit considerable genetic and clinical diversity, even amongst tumors of the same World Health Organization (WHO) histological grade (1). Over 100 DNA mutations have been implicated in glioma genesis (2), from which tumors may be stratified into distinct molecular subgroups of prognostic and predictive value (2-4). As a biomarker, the Isocitrate Dehydrogenase (IDH) gene is pivotal, because a de novo IDH mutation (IDH^{mut}) probably represents the initiating event that distinguishes lower grade (WHO II-III) gliomas from primary glioblastoma (WHO IV) (5). The most common mutation is IDH1R132H, present in > 90% of lower grade gliomas and in secondary glioblastoma (6). Absence of an IDH mutation (IDH wild-type, IDH^{wt}) is a key feature of primary glioblastoma and defines malignant lower grade gliomas within the same genetic disease spectrum (3). IDH^{mut} gliomas with combined deletion of the short arm of chromosome 1 and the long arm of chromosome 19 (IDH^{mut}1p19q^{del}) are mostly oligodendrogliomas with a better prognosis, which can be distinguished from 1p19q intact (IDH^{mut}1p19q^{int}) gliomas that are predominantly astrocytomas, with an intermediate prognosis.

Glioma genotyping by immunohistochemistry depends on tissue sampling and requires facilities for testing, with potential geographical restrictions on turnaround times. Presurgical mutational analysis could influence the timing and extent of tumor resection (7) and predict adjuvant therapy response, for example the sensitivity to temozolomide is greater in IDH^{mut} gliomas (8).

Morphological assessment can contribute to glioma molecular subtyping (9, 10), but limitations include observer dependence and lack of quantitative thresholds. Filtration-histogram based MR imaging texture analysis (MRTA) provides quantitative information about tumor microstructure beyond the limits of visual perception, as reflected by the distribution of pixel values within the lesion (11). MRTA requires no programming skills and is operated by performing a manual tumor segmentation using workstation-integrated software, with calculations initiated via mouse-click. The application commences with a filtration step, which serves to remove image noise, extracts and enhances tissue features of different sizes before measuring signal intensity histogram parameters. The interpretation of results as a reflection of biological processes depends on the tumor type examined, but broadly MRTA provides a measure of tissue heterogeneity. The software has previously

undergone a qualification process for glioma histological grading and differential diagnosis (12-14). In this study, we investigated whether filtration-histogram based MRTA could predict glioma IDH and 1p19q genotypes using MR images acquired in routine clinical practice.

Materials and methods

Patient cohort

Ethics review board approval was obtained with informed consent waived for this retrospective study of anonymized imaging data. Cases were identified randomly from attendances for operative planning (n=124) between 2010 and 2016. 14 patients were excluded due to a non-glioma histological diagnosis, 11 patients due to prior surgery, and 2 studies had corrupted imaging data. In total, 97 gliomas were eligible for MRTA (**Figure 1, SHARDS diagram**). The sample size for this analysis was chosen based on previous work with the software algorithm.

MRI Imaging Acquisition

96 patients had available T2-weighted (T2) sequences, 91 had T1-weighted post Gadolinium (T1+Gad) imaging and 82 had ADC maps (ADC). Our institution is a quaternary neurosurgical centre, therefore the conventional MRI sequences in this study originated from multiple referrers. The imaging was acquired on 44 different machines (67 at 1.5 T, 30 at 3T) from all major vendors: 6 GE, 26 Siemens, 11 Phillips and 1 Hitachi scanner. No single MRI machine supplied more than 20% gliomas of one molecular subtype or WHO grade. The median [min, max] values of the parameters of the T2-weighted images were: TE = 99 [17, 140] ms; TR = 4690 [1205, 6300] ms; in plane resolution 0.65 x 0.5 [0.45 x 0.45, 1.13 x 0.95] mm^2, slice thickness = 5 [4, 7] mm, interslice gap = 6.5 [4, 7.15] mm. For T1+Gad, the median [min, max] values of the parameters were: TE = 10 [2.28, 26.38] ms; TR = 470 [160, 740] ms; in plane resolution 0.575 x 0.525 [0.45 x 0.375, 1.5 x 1.9] mm^2, slice thickness = 5 [0.9, 7] mm, interslice gap = 6.5 [0.9, 7.15] mm. All DWI acquisitions included three diffusion gradients with weighting values b = 0s/mm^2 and b = 1000s mm^2; the median [min, max] of the other parameters were: TE = 95 [55, 136] ms; TR = 3972 [2873, 8570] ms; in plane resolution 1.25 x 1.2 [1.15 x 1.15, 1.8 x1.8] mm^2, slice thickness = 5 [4,6] mm, interslice gap = 6.5 [4.5, 7] mm.

Histopathology

Following fixation as paraffin blocks, all tissue samples underwent analysis at our institution's neuropathology department according to World Health Organization (WHO) 2016 guidance on

immunohistochemistry testing and previous published methodology (15). For IDH R132H immune-negative tumors, multiple gene Sanger sequencing was performed to exclude alternative IDH mutations. A quantitative polymerase chain reaction based copy number assay was used to determine 1p/19q status.

Image segmentation

All image interactions were performed blinded to histological and molecular diagnosis, using proprietary texture analysis research software (TexRAD version 3.3, TexRAD Ltd, www.texrad.com, part of Feedback Plc, Cambridge, UK). Segmentations were performed slice by slice with the software's freehand drawing function. For T2, the entire volume of signal abnormality was segmented (**Figure 2**). For T1+Gad, 3 different types of segmentation were completed: the entire region of T1 signal abnormality (enhancing + non-enhancing tissue, **Seg A**), the enhancing lesion inclusive of necrosis (enhancing + necrosis, **Seg B**) and enhancing tissue only (enhancing tissue – necrosis, **Seg C**) (**Figure 3**). ADC volumes of interest were defined by manually copying the area of T2 signal abnormality **(Figure 2)**. Segmentations were undertaken by one researcher (M.L.), trained and supervised by a board-certified radiologist specialized in neuro-oncology (S.T., 7 years experience). Slices containing very few (< 250) pixels of signal abnormality were excluded to avoid partial volume effects (mean slice size 4803 pixels, range 349 – 15499). In addition, the image with the largest glioma cross-section based on pixel count was subjected to a separate (single slice) evaluation.

MR Texture Analysis (MRTA)

MRTA in this study follows a previously published method (13, 16). The filtration used here corresponds to the spatial scale filter (SSF) values of 0, 2 mm, 3 mm, 4 mm, 5 mm and 6 mm in width (radius). SSF=0 hereby means no filtration, SSF = 2 mm equals a fine texture scale, SSF = 3-5 mm a medium texture scale, and SSF = 6 mm translates to a coarse texture scale **(Figure 4)**. This was followed by quantification of the image texture via measuring histogram and statistical parameters (mean, standard deviation, entropy, mean of positive pixels, skewness, kurtosis) with slice data mathematically interpolated.

Statistical analysis

All statistical testing was performed with SPSS 24 (IBM). For each sequence, the ability of the texture features (with and without filtration) to differentiate between the presence and absence of IDH was evaluated using non-parametric Mann Whitney testing. For 1p19q genotyping, Kruskal-Wallis 1 way ANOVA was used. This was repeated over different subgroup analyses e.g. according to WHO grade. For statistically significant results, a receiver operating characteristic (ROC) analysis was undertaken, to determine the area under the curve (AUC), and optimum cut-offs for sensitivity and specificity calculations. A multivariate logistic regression model was generated, to combine the best results from all sequences for IDH genotyping. Pearson coefficient was used to test associations between volumetric and single slice results. Statistics advice was obtained at our institute.

Results

Participants

50 females and 47 males with an average age of 43.3 (27-77) years were included in the study. The histological and molecular characteristics of the patient population are listed in **Table 1**.

MRTA using T1+Gad

T1+Gad volumes for IDH typing

Table 2 summarizes the most significant T1+Gad results for molecular subtyping. For IDH typing, filtered texture parameters produced the best results. When examining all Gadolinium enhancing gliomas (WHO II-IV) together, coarse texture mean derived from **Seg A** permitted moderately accurate IDH status prediction (sensitivity 72.2%, specificity 74%, AUC = 0.801), with mean signal intensity values being higher in the IDH^{wt} group.

In glioblastoma, using **Seg A,** mean was the best parameter for IDH genotyping (sensitivity 91.7%, specificity 88.9%, AUC = 0.935). Using **Seg B**, SD represented the most distinctive parameter to predict IDH status (sensitivity 87.5%, specificity 100%, AUC 0.906 – 0.969). With **Seg C**, kurtosis was the best IDH status predictor across all filters (sensitivity 91.9%, specificity 100%, AUC = 0.945) (**Figure 5**).

T1+ Gad volumes for 1p19 typing

Combining WHO grades II-III, T1+Gad using **Seg A** demonstrated moderate results with unfiltered skewness as the best predictor (sensitivity 77.4%, specificity 77.8%, AUC 0.736). For WHO III alone, the algorithm performance for mean was better (AUC 0.871).

MRTA using ADC maps

ADC volumes for IDH typing

Table 3 summarizes the ROC analysis using ADC volumes for MRTA. Combining WHO II-IV, ADC skewness without filtration performed best for IDH genotyping (sensitivity 77.8%, specificity 68.7%, AUC = 0.791).

Including all gliomas with available ADC maps (n=82), unfiltered mean ADC performed moderately for a threshold of 1135 mm/s^2 (sensitivity 64.1%, specificity 66.7%, AUC 0.694). When excluding cases with macroscopic necrosis (n=11) from the analysis, the mean ADC area under the curve improved (sensitivity 68.3%, specificity 91.9%, AUC 0.818). By additional exclusion of cases with enhancement lacking necrosis (n= 13), the results improved minimally further. For non-enhancing gliomas, the prediction using ADC mean (sensitivity 70.6%, specificity 100%, AUC 0.840) was near that of kurtosis (sensitivity 85.7%, specificity 78.4%, AUC 0.877). When removing 1p19q codeleted gliomas from the analysis, the accuracy of ADC to distinguish IDH^{wt} and IDH^{mut}1p19^{int} was greater across WHO II-IV with further improved results for ADC mean (AUC 0.888), and kurtosis (AUC 0.949).

The algorithm was less able to distinguish IDH^{wt} and IDH^{mut}1p19^{del} ADC features with only one significant result observed for unfiltered skewness (AUC 0.690). But when applied only to non-enhancing gliomas, mean ADC and kurtosis could separate IDH^{wt} and IDH^{mut}1p19q^{del} better (AUC 0.79, AUC 0.807 respectively).

ADC volumes for 1p19q typing

For the detection of the 1p19q co-deletion in IDH^{mut}, ADC was the most useful sequence. Combining WHO II-III, unfiltered textures predicted 1p19q genotype well (sensitivity 80.6%, specificity of 89.3%, AUC 0.811). The algorithm performance for ADC mean was marginally greater in WHO II alone (sensitivity 90%, specificity 85%, AUC 0.905). In WHO grade III, kurtosis generated the best results (sensitivity 88.9%, specificity 100%, AUC 0.952).

MRTA using T2

T2 volumes for IDH typing

Table 4 shows the numerical results for the T2 image segmentation. Overall, T2 texture parameters were less distinctive, but the results reached statistical significance. Combining WHO II-IV, the ability to predict IDH status was highest for unfiltered skewness (sensitivity 83.1%, specificity 78.9%, AUC =

0.821). There was no improvement in accuracy when excluding necrotic or non-necrotic enhancing gliomas from the T2 analysis.

T2 volumes for 1p19q typing

T2 appeared more limited for 1p19q typing across WHO grades II-III with medium filtered skewness as the best parameter (sensitivity 75.7%, specificity 62.5%, AUC 0.728). An improved result was observed for WHO III gliomas alone (unfiltered skewness AUC 0.843).

Sequence combination for IDH typing

A logistic regression model was generated combing the best results from T1+Gad, T2 and ADC volumes, merging all WHO grades (n= 80, 63 IDH^{mut}/17 IDH^{wt}). Since the filtering precedes MRTA, 6 different logistic regressions were undertaken. Each filter was selected in turn and a regression undertaken using the 18 textures derived from the 3 sequences. This was a fast operation, taking less than 30 seconds after tabulating the texture results. Using a ROC analysis of the predicted probabilities (AUC = 0.98 (CI 0.955, 1)), the regression model yielded a high sensitivity of 90.5 % and specificity of 94.1 % (SSF 4). The model was statistically significant (Hosmer and Lemeshow test = 0.999, omnibus p < 0.001) and demonstrated predictive accuracy (Nagelkerke R Square = 0.826).

Single slice analysis for IDH typing

For T1+Gad, mean remained significant in the single slice analysis, with best results achieved for medium to coarse scale filtration, consistent with volumetric results (sensitivity 72.2%, specificity 69.9%, AUC 0.786). ADC results showed a profile comparable to volumetric assessment for unfiltered mean (sensitivity 60.9%, specificity 80.9%, AUC 0.727). The T2 segmentation produced unfiltered skewness as the only significant marker (sensitivity 68.6%, specificity 79.2%, AUC 0.816), also consistent with volumetric analysis. For those textures, which generated significant results in both volumetric and single slice use, the Pearson correlation between the two methods was excellent (r = 0.956) (**Figure 6**).

Discussion

MRTA has shown ability to identify microstructural disease patterns, including cancer genotypes and chemotherapy response (17, 18). We demonstrated its potential value for the non-invasive assessment of glioma IDH and 1p19q status. To our knowledge, this is the first study to present results for low and high grade glioma molecular subtyping using a filtration histogram approach based on conventional MR sequences.

Preoperative genotyping matters for several reasons: in IDH^{mut} astrocytoma even small residual volumes of tumour reduce survival (19), however, molecular results are not usually available during surgery. Glioblastoma therapy is considered appropriate for WHO II-III IDH^{wt} gliomas, consisting of maximum safe resection followed by radiotherapy and chemotherapy. But morphologically 'low grade' IDH^{wt} gliomas are at risk of receiving observation only (20).

All three MRI sequences tested in this study could contribute to non-invasive genotyping, whereby T1+Gad generated the best results in glioblastoma. Gadolinium enhancement occurs in rapidly proliferating gliomas as a result of pathological neovascularity and blood brain barrier disruption (21). It has been suggested that the extent and morphology of new vessel formation differs by mutational status, with greater vascularity in IDH^{wt} compared to IDH^{mut} (22). These processes are known to develop gradually and could explain why enhancement patterns become more precisely recognized by MRTA towards WHO IV. The comparison of three different T1+Gad segmentation methods highlights that the performance of texture parameters is technique-dependent. Using **Seg A**, mean values were most diagnostic of IDH status, which may relate to overall tumor contrast uptake intensity. In support of this, a recent study by Yamauchi et al. observed dense contrast-enhancement preferentially in IDH^{wt} gliomas (23). With **Seg B**, SD performed best, probably reflecting greater variability of signal intensity values according to the extent of necrosis. Using the same segmentation technique (**Seg B**) and parameter (SD), Skogen et al. were able to non-invasively predict glioma WHO grade with MRTA (13). When applying **Seg C**, kurtosis was most significant suggesting additional differences in microstructural enhancement heterogeneity, which appeared greater for IDH^{wt} gliomas. Our results are consistent with a recent machine learning study, in which T1+Gad supported IDH status prediction especially for WHO IV (24).

Diffusion-weighted imaging has been widely recognized as a biomarker of cellularity in neoplasia (25). Reduced ADC values are a feature of malignant gliomas (26, 27), however, the occurrence of increased diffusivity in necrosis may confound quantitative assessment. In a previous diffusion tensor study by Tan et al., the accuracy of ADC for IDH typing diminished towards WHO IV (28). Our analysis confirms that macroscopic 'high grade' features impact on diffusion quantification: Mean ADC values showed limited sensitivity and specificity when examining WHO II-IV together, with skewness and kurtosis as markers of heterogeneity (29) achieving better results in this context. On the contrary, kurtosis and mean ADC were both valuable for IDH typing of gliomas with 'low grade' appearances. This is consistent with recent studies, which highlighted that low mean ADC values are predictive IDH^{wt} status in lower grade gliomas (10, 27, 30). Amongst IDH mutant gliomas, mean ADC values were best at predicting 1p19q genotype in this study, especially for WHO II. $IDH^{mut}1p19^{del}$ glioma ADC values tend to be intermediate, which may impede its distinction from IDH^{wt}, despite marked differences in survival.

The T2 texture signatures identified as predictive of IDH status were similar to those identified for ADC. This result is in keeping with previous research showing associations between ADC, T2 signal and tissue cellularity in glioma, medulloblastoma and lymphoma (31). However, our T2 derived results are less accurate than reported for WHO II gliomas alone (32).

The single slice analysis showed a strong correlation with the volumetric findings, although it was less distinctive. Using this strategy, MRTA appears sufficiently rapid to be integrated into clinical reporting. Further prospective evaluation is required to determine the respective benefits of whole tumor versus largest cross-section texture analysis in terms of precision versus time expense.

The combination of T1+Gad, ADC and T2 sequences appears excellent in the absence of advanced MRI techniques, which might otherwise be employed to assist presurgical glioma subtyping. The diagnostic results presented here are at least equivalent to the best performing 2HG MR spectroscopy (33), perfusion (22) and artificial intelligence approaches published to date, with potential advantages for clinical translation. In summary, MRTA is an easily applicable image workstation tool with potential to perform IDH and 1p19q genotyping of untreated gliomas based on conventional MRI sequences.

Limitations

Our patient cohort included a limited number of IDH^{wt} tumours, particularly in WHO grade II and III. It is unknown whether with a larger sample the MRTA software could achieve IDH genotyping by solely using T1w post Gadolinium sequences as suggested by one previous study (34). Further software development is required to optimize transposing regions of interest from one sequence to another, which would increase time efficiency. The origin of MRI sequences from multiple institutions could have influenced measurements, but as no scanner contributed any particular WHO grade or molecular subtype, a systematic error is unlikely. As discussed in prior research, for ADC mapping the dependence from T_1, T_2 and TR settings is mathematically eliminated (30, 35).

Conclusion

MRTA is a software platform without machine learning, which can assist the distinction of glioma IDH and 1p19q molecular subtypes. Results may be optimized through tailoring the choice of MRI sequence(s) to tumor morphology. It also appears possible to predict genetic status using a sequence combination without considering specific lesion features.

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Table 1. WHO grades, IDH and 1p19 genotypes of glioma population

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WHO grade	Number of gliomas	IDH^{wt} (e/e+n)*	IDH^{mut} $1p19q^{int}$ (e/e+n)	$IDH^{mut}1p19q^{del}$ (e/e+n)
II	54	4 (0/ 0)	24 (2/1)	26 (2/0)
III	20	3 (1/0)	7 (1/0)	10 (4/1)
IV	23	12 (11/8)	10 (5/1)	1
Total	97	19 (12/8)	41 (8/2)	37 (6/1)

* (e/e+n) denotes (enhancing/enhancing+necrotic) gliomas within each molecular subgroup.

Table 2. Volumetric analysis using T1 Gad

Table 2. Volumetric analysis using T1+ Gad

T1+Gad for IDH genotyping												
	SSF	Mean	SD	Skewness	Kurtosis	Sens/Spec (%)		SSF	Mean	SD	Skewness	Kurtosis	Sens/Spec (%)

	SSF	Mean	SD	Skewness	Kurtosis	Sens/Spec (%)		SSF	Mean	SD	Skewness	Kurtosis	Sens/Spec (%)
WHO II-IV Seg A IDH^{wt}=18 IDH^{mut}=73	0	NS	**0.695****	NS	NS	66.7/61.3	**WHO IV Seg B** IDH^{wt}=8, IDH^{mut}=4	0	NS	NS	NS	NS	NS
	2	**0.752***	0.743*	0.633**	NS	72.2/71.2		2	NS	NS	NS	NS	NS
	3	**0.764***	0.718**	0.737*	NS	83.3/68.5		3	NS	**0.938***	NS	NS	75/100
	4	**0.786***	0.706**	0.759*	NS	83.3/69.9		4	NS	**0.969***	NS	NS	87.5/100#
	5	**0.800***	0.697**	0.701*	NS	72.2/69.9		5	NS	**0.906***	NS	NS	87.5/100
	6	**0.801***	0.699**	NS	NS	72.2/74#		6	NS	NS	NS	NS	NS
WHO IV Seg A IDH^{wt}=12 IDH^{mut}=9	0	NS	**0.769***	NS	NS	66.7/100	**WHO IV Seg C** IDH^{wt}=11, IDH^{mut}=5	0	NS	NS	NS	**0.836***	91.9/100
	2	0.778*	0.870*	**0.880***	NS	83.3/89.9		2	NS	NS	NS	**0.927***	91.9/100
	3	0.861*	0.870*	**0.917***	NS	83.3/100		3	NS	0.855*	0.836*	**0.891***	91.9/100
	4	**0.935***	0.852*	0.852*	NS	91.7/88.9#		4	NS	0.891*	0.782*	**0.818***	91.9/100
	5	**0.917***	0.824**	0.769**	NS	83.3/100		5	NS	**0.873***	NS	0.855*	91.9/100
	6	**0.907***	0.815**	NS	NS	83.3/77.8		6	NS	NS	NS	**0.945***	91.9/100#
T1+Gad for 1p19q genotyping of IDH^{mut} glioma													
	SSF	Mean	SD	Skewness	Kurtosis	Sens/Spec (%)		SSF	Mean	SD	Skewness	Kurtosis	Sens/Spec (%)
WHO II-III 1p19q^{int}=31, 1p19q^{del}=33	0	NS	NS	**0.736***	NS	77.4/77.8#	**WHO III** 1p19q^{int}=7, 1p19q^{del}=10	0	NS	NS	**0.800***	NS	85.7/80
	2	**0.725***	NS	NS	NS	75.8/64.5		2	**0.871***	NS	NS	NS	70/100#
	3	**0.735***	NS	NS	NS	81.8/61.3		3	**0.886***	NS	NS	NS	70/100
	4	**0.735***	NS	NS	NS	78.8/61.3		4	**0.857***	NS	NS	NS	70/100
	5	**0.738***	NS	NS	NS	75.8/61.3		5	**0.871***	NS	NS	NS	70/100
	6	**0.750***	NS	0.659	NS	75.8/61.3		6	**0.871***	NS	0.857*	0.896*	70/100

SSF = spatial scale factor, *p-value<0.005, **p-value<0.05, Bold indicates the texture with the highest AUC for which accuracy is displayed, # indicates best accuracy, NS indicates not significant

Table 3. Volumetric analysis using ADC values

Table 3. Volumetric analysis using ADC values

ADC for IDH genotyping										
	SSF	Mean	Skewness	Kurtosis	Sens/spec (%)		SSF	Mean	Skewness	Kurtosis	Sens/spec (%)
WHO II-IV IDH^{wt}=18 IDH^{mut}=64	0	0.694**	**0.791***	0.734**	77.8/68.7#	**WHO II-IV** Non-enhancing IDH^{wt}=7 IDH^{mut}=51	0	0.733*	**0.843***	0.751*	71.4/88.2
	2	NS	NS	NS	NS		2	**0.824***	NS	0.745*	74.5/85.7
	3	NS	NS	**0.694***	66.7/64.9		3	**0.832***	NS	0.784**	70.6/85.7
	4	NS	NS	**0.693***	66.7/68.7		4	**0.815***	NS	0.787**	68.6/85.7
	5	0.655**	NS	**0.727***	72.2/62.5		5	0.818*	NS	**0.849***	71.4/82.4
	6	0.674**	NS	**0.736***	77.8/67.2		6	0.840*	NS	**0.877***	85.7/78.4#
WHO II-IV Excluding necrotic gliomas IDH^{wt}=11, IDH^{mut}=60	0	0.753**	**0.811***	0.755**	72.7/88.3#	**WHO II-IV** Non-enhancing IDH^{wt} = 7 versus IDH^{mut} 1p19q^{int} =28	0	0.847*	**0.939***	0.898*	100/85.7
	2	**0.785***	NS	0.736**	73.3/81.8		2	**0.872***	NS	0.796*	85.7/85.7
	3	**0.809***	NS	0.782*	71.7/81.8		3	**0.862***	NS	0.857*	85.7/71.4
	4	**0.791***	NS	0.776*	66.7/81.8		4	**0.852***	NS	0.847*	78.6/71.4
	5	**0.800***	NS	0.800*	66.7/81.8		5	0.857*	NS	**0.949***	100/85.7#
	6	**0.818***	NS	0.802*	68.3/91.9		6	0.888*	NS	**0.934***	100/85.7

ADC for 1p19q genotyping of IDH^{mut} glioma										
	SSF	Mean (WHO II only)	Kurtosis	Sens/spec (%)		SSF	Mean	Skewness	Kurtosis	Sens/spec (%)
WHO II-III 1p19q^{int} =31 1p19q^{del} =33	0	**0.811* (0.905*)**	NS	95/85#	**WHO III** 1p19q^{int} =7 1p19q^{del} =9	0	NS	0.921*	**0.952***	88.9/100#
	2	**0.708* (0.798*)**	NS	75/80		2	NS	**0.873***	NS	100/71.4
	3	**0.722* (0.808*)**	NS	70/75		3	NS	**0.937***	NS	100/71.4
	4	**0.715* (0.793*)**	NS	70/70		4	NS	**0.937***	NS	100/71.4
	5	**0.737* (0.802*)**	NS	75/70		5	NS	**0.905***	NS	100/71.4
	6	**0.736* (0.800*)**	NS	85/65		6	NS	**0.889***	NS	100/71.4

SSF = spatial scale factor, *p-value<0.005, **p-value<0.05, Bold indicates the texture with the highest AUC for which accuracy is displayed, # indicates best accuracy, NS indicates not significant

Table 4: Volumetric analysis using T2 values and single slice results for all sequences

T2 volumes for IDH genotyping

	SSF	Mean	Skew	Kurtosis	Sens/spec (%)
WHO II-IV IDH[wt]=19, IDH[mut]=77	0	NS	**0.821***	0.669**	78.9/83.1#
	2	**0.696***	NS	NS	NS
	3	**0.677***	NS	0.657**	63.6/57.9
	4	0.668**	NS	**0.717***	61.0/73.7
	5	0.658**	NS	**0.706***	63.6/73.7
	6	0.653**	NS	**0.661***	57.1/68.4

T2 volumes for 1p19q genotyping of IDH[mut] glioma

	SSF	Mean	Skew	Kurtosis	Sens/spec (%)
WHO II-IV 1p19q[int]=37 1p19q[del]=40	0	NS	**0.722***	NS	73/62.5
	2	NS	**0.717***	NS	62.2/70
	3	NS	**0.728***	NS	75.7/62.5#
	4	NS	**0.703***	NS	73/60
	5	NS	**0.678***	NS	64.9/62.5
	6	NS	**0.631***	NS	59.5/55

Single slice T1+ Gad for IDH genotyping

	SSF	Mean	SD	Entropy	Sens/spec (%)
WHO II-IV IDH[wt]=18 IDH[mut]=73	0	0.657**	0.690**	**0.694***	77.8/61.6
	2	**0.738***	0.711*	0.693**	66.7/76.7
	3	**0.747***	0.704**	0.685**	72.2/71.2
	4	**0.778***	0.695**	0.670**	88.9/64.4
	5	**0.786***	0.684**	NS	72.2/69.9#
	6	**0.771***	0.667**	NS	77.8/63

Single slice ADC for IDH genotyping

	SSF	Mean	Skew	Kurtosis	Sens/spec (%)
WHO II-IV IDH[wt]=18, IDH[mut]=64	0	**0.727***	0.722*	0.724*	67.2/66.7
	2	NS	**0.753***	NS	77.8/64.1#
	3	NS	0.654**	**0.674***	66.7/60.9
	4	NS	NS	**0.681***	66.7/57.8
	5	NS	NS	**0.663***	66.7/64.1
	6	**0.660***	NS	NS	61.1/56.3

Single slice T2 for IDH genotyping

	SSF	Mean	SD	skew	Sens/spec (%)
WHO II-IV IDH[wt]=19, IDH[mut]=77	0	NS	NS	**0.816***	84.2/66.2#
	2	NS	NS	NS	NS
	3	NS	NS	NS	NS
	4	NS	NS	NS	NS
	5	NS	NS	NS	NS
	6	NS	NS	NS	NS

Sequence combination for IDH genotyping

	SSF	AUC	Min (95% CI)	Max (95% CI)	Sens/Spec (%)
WHO II-IV (n= 80)	0	0.937*	0.877	0.998	88/88
	2	0.937*	0.887	0.987	86/94
	3	0.942*	0.894	0.990	87/94
	4	**0.980***	**0.955**	**1.000**	**90/94#**
	5	0.895*	0.857	1.000	90/88
	6	0.937*	0.869	1.000	100/83

SSF = spatial scale factor, *p-value<0.005, **p-value<0.05, Bold indicates the texture with the highest AUC for which accuracy is displayed, # indicates best accuracy, NS indicates not significant
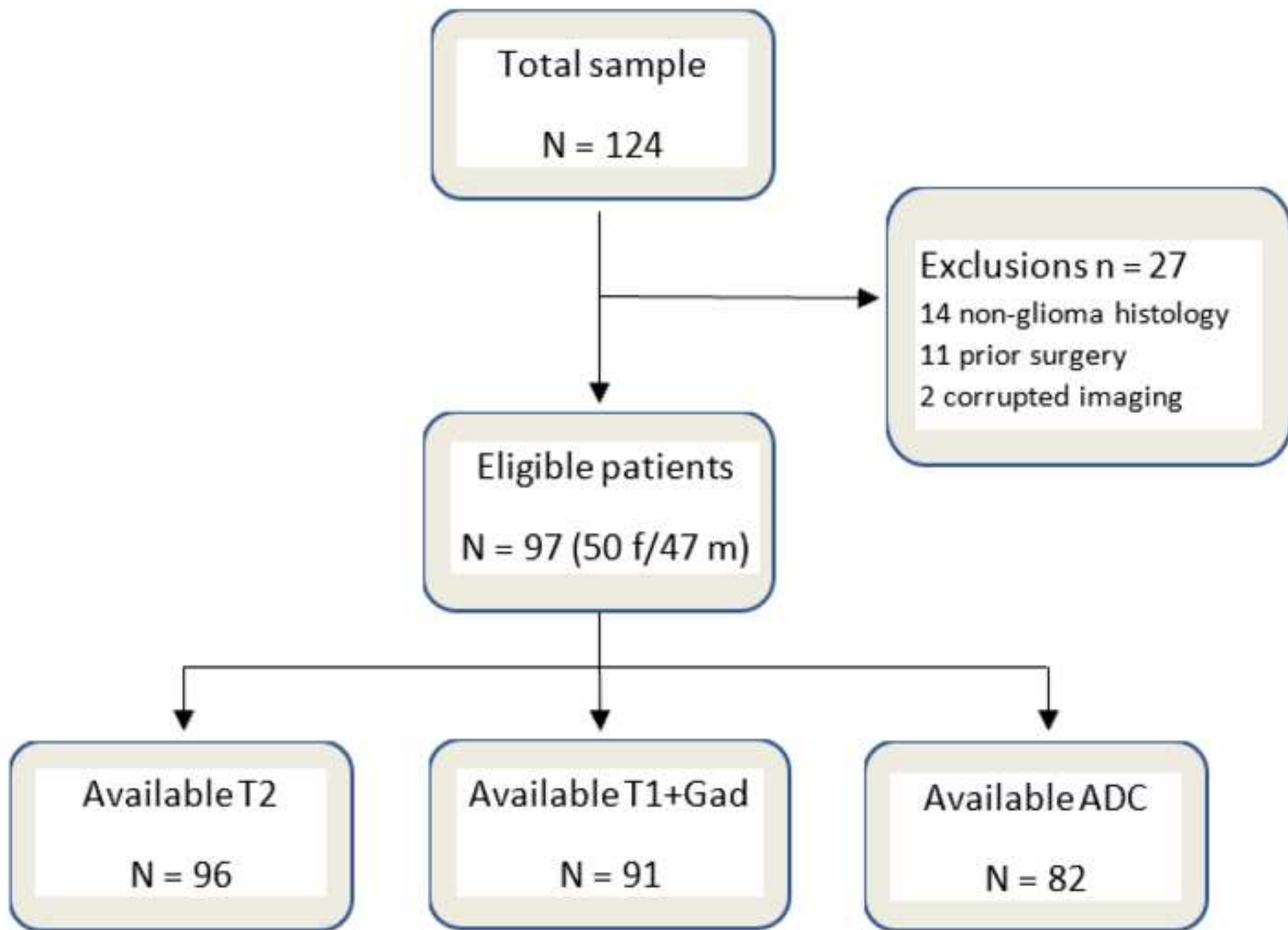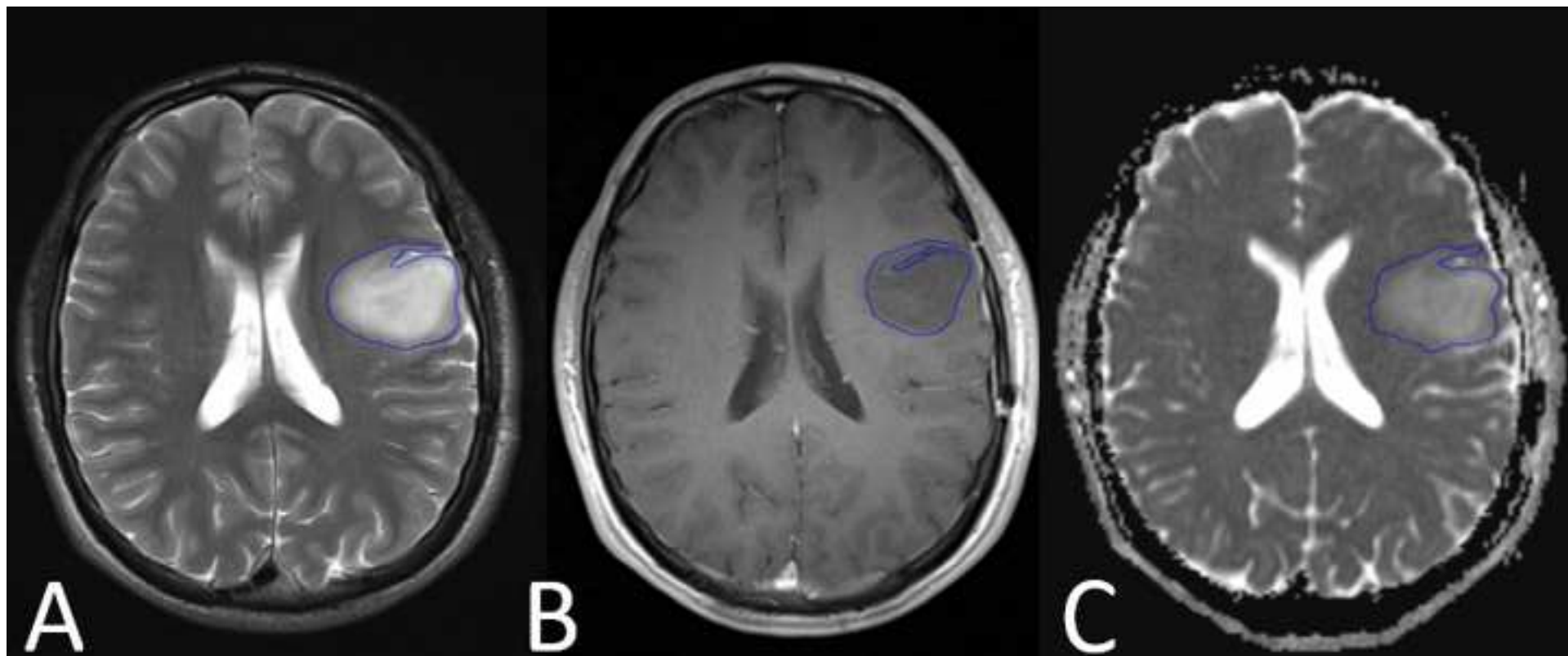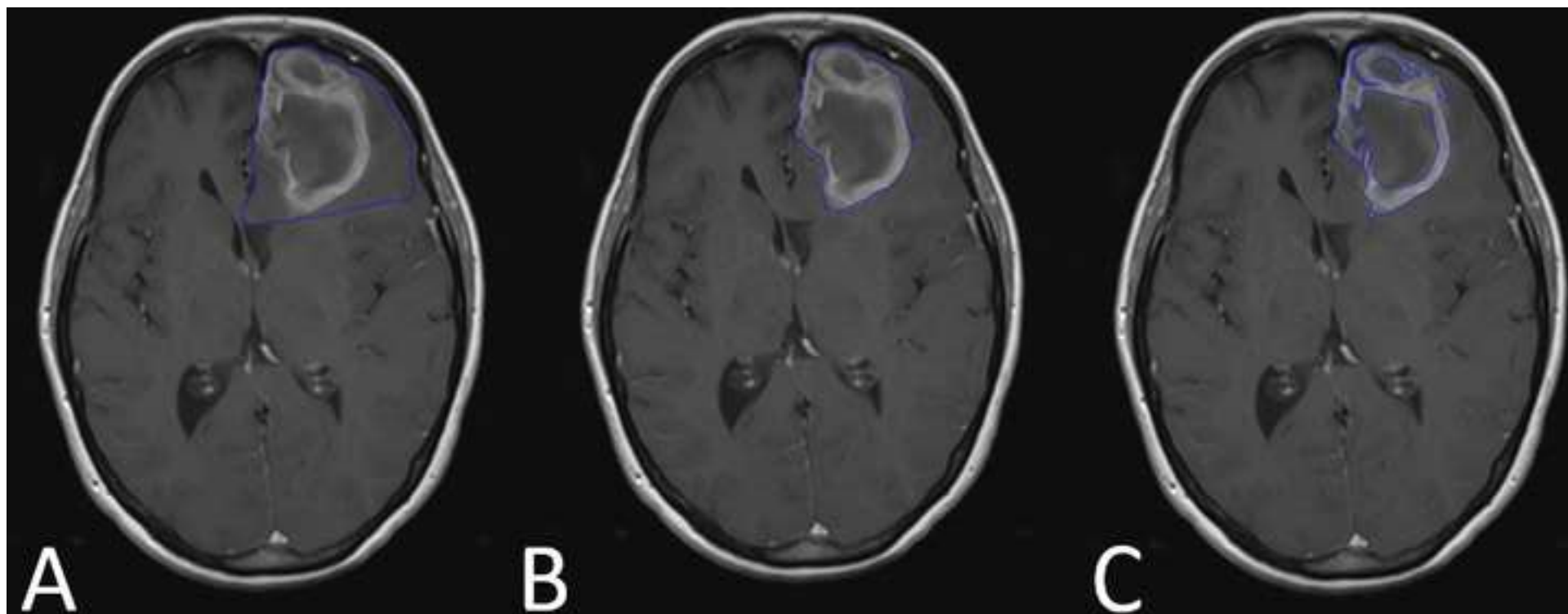
Figure 1

Figure 2
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Figure 4
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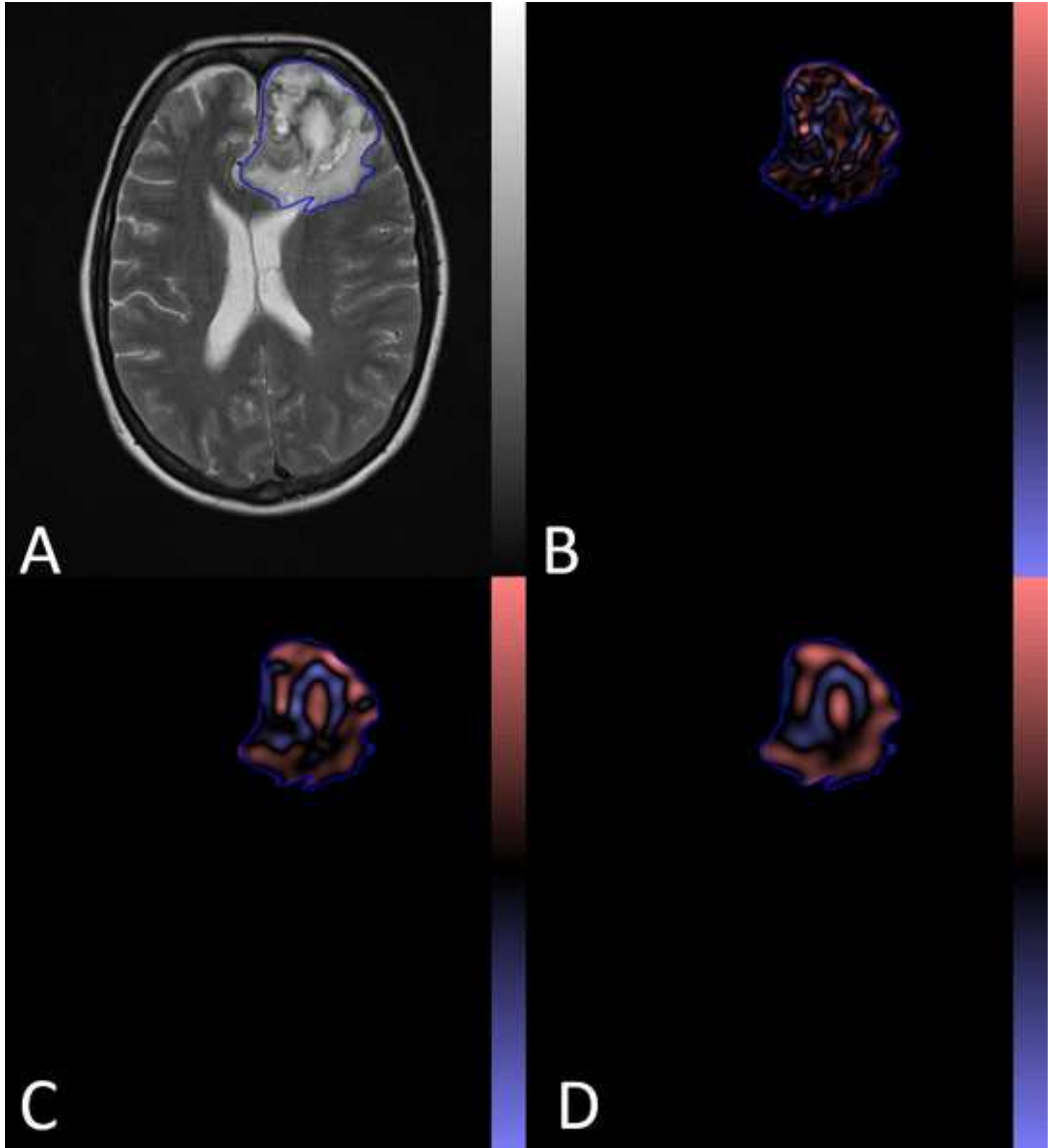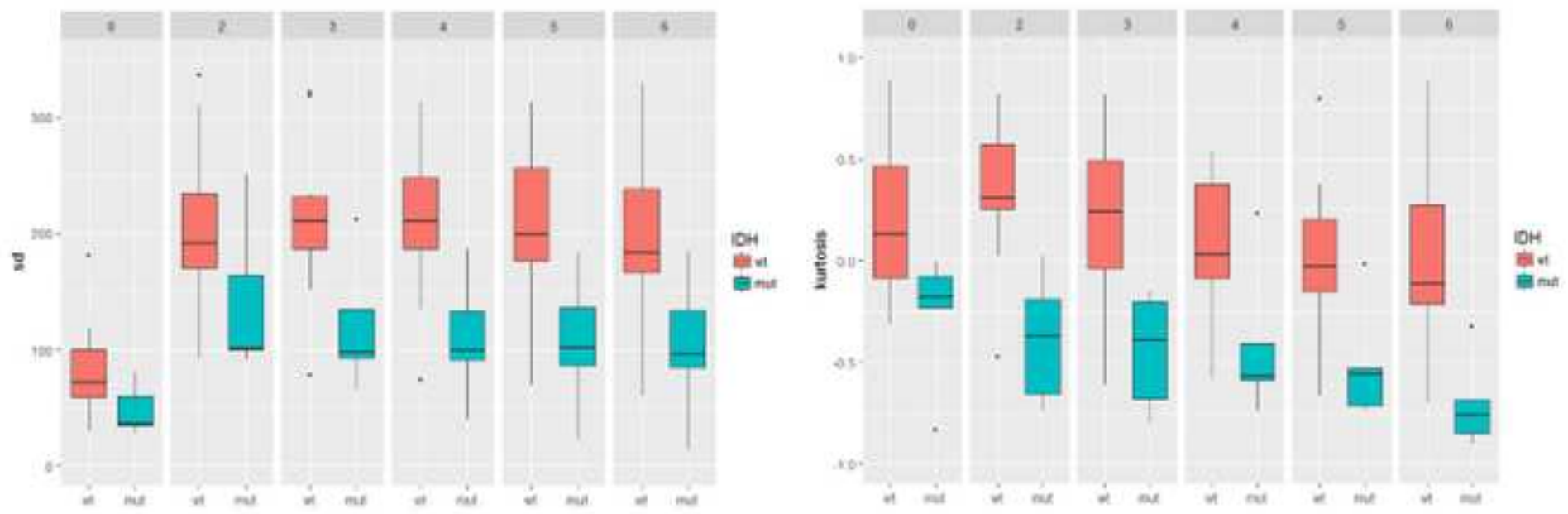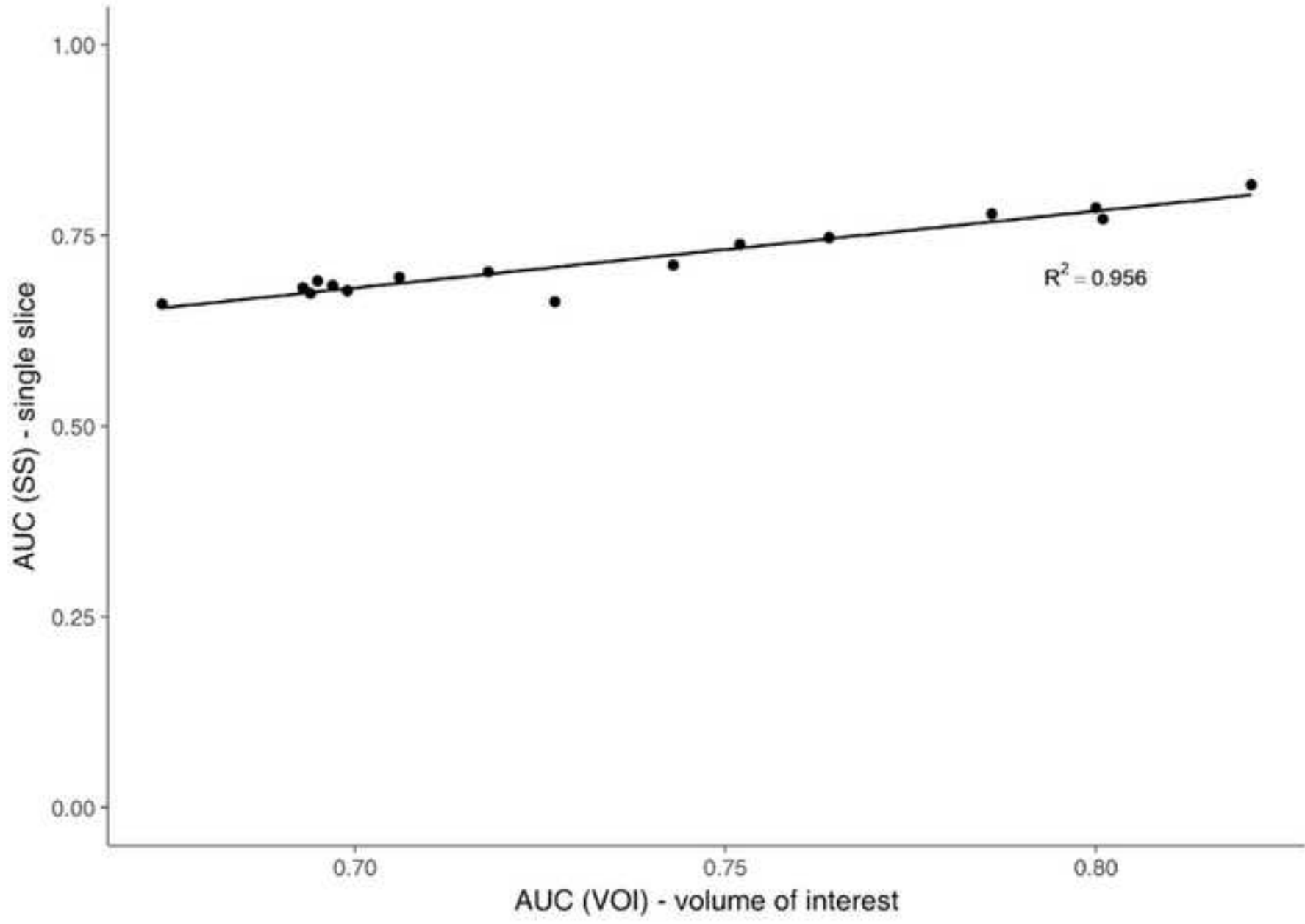**Figure 6**
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Figure 6

Figure Legends