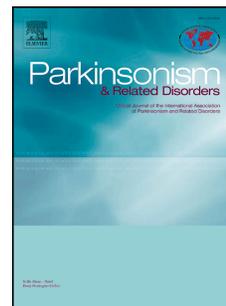


Journal Pre-proof

The use of wearable/portable digital sensors in Huntington's disease: a systematic review

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PII: S1353-8020(21)00021-3

DOI: <https://doi.org/10.1016/j.parkreldis.2021.01.006>

Reference: PRD 4625

To appear in: *Parkinsonism and Related Disorders*

Received Date: 1 July 2020

Revised Date: 13 October 2020

Accepted Date: 8 January 2021

Please cite this article as: Tortelli R, Rodrigues FB, Wild EJ, The use of wearable/portable digital sensors in Huntington's disease: a systematic review, *Parkinsonism and Related Disorders*, <https://doi.org/10.1016/j.parkreldis.2021.01.006>.

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1 **The use of wearable/portable digital sensors in Huntington's disease: a systematic**
2 **review**

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9 **Keywords:** Huntington's disease; biomarkers; digital technology; wearable sensors; portable
10 sensors.

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20

21 **Highlights**

22 • Wearable/portable sensors have been proposed to detect and quantify manifestations
23 of many neurodegenerative diseases

24 • No systematic review so far has examined their use in Huntington's disease (HD)

25 • This work draws a broad picture of the digital wearable-based landscape in HD

26 • The utility of wearables in clinical practice and therapeutic research still needs to be
27 proved

28 • Collaborative efforts are needed to further investigate their clinical use in HD

29

30

1 **Funding:**

2 RT's salary is funded by a research grant from F. Hoffmann-La Roche to UCL

3 EJW's salary has been funded by Medical Research Council, CHDI Foundation, and F.
4 Hoffmann La Roche

5

6 **Authors' contribution**

7 EJW and RT conceived the study. FBR constructed and ran the electronic search. RT and
8 FBR independently screened and selected the references. RT wrote the manuscript. EJW and
9 FBR reviewed and revised the manuscript.

10 All authors have approved the final article.

11

12 **Declarations of interest**

13 RT, FBR and EJW are University College London employees.

14 EJW is the PI of the "Digital-HD study", sponsored by University College London with a
15 grant by Hoffmann-La Roche. RT and FBR are both involved in this study.

16 FBR has provided consultancy services to GLG and F. Hoffmann-La Roche Ltd.

17 EJW reports grants from, Triplet Therapeutics, PTC Therapeutics, Shire Therapeutics, Wave
18 Life Sciences, Mitoconix, Takeda, Loqus23. All honoraria for these consultancies were paid
19 through the offices of UCL Consultants Ltd., a wholly owned subsidiary of University
20 College London. University College London Hospitals NHS Foundation Trust has received
21 funds as compensation for conducting clinical trials for Ionis Pharmaceuticals, Pfizer and
22 Teva Pharmaceuticals.

23

1 Abstract

2 In chronic neurological conditions, wearable/portable devices have potential as innovative
3 tools to detect subtle early disease manifestations and disease fluctuations for the purpose of
4 clinical diagnosis, care and therapeutic development. Huntington's disease (HD) has a unique
5 combination of motor and non-motor features which, combined with recent and anticipated
6 therapeutic progress, gives great potential for such devices to prove useful. The present work
7 aims to provide a comprehensive account of the use of wearable/portable devices in HD and
8 of what they have contributed so far. We conducted a systematic review searching
9 MEDLINE, Embase, and IEEE Xplore. Thirty references were identified. Our results
10 revealed large variability in the types of sensors used, study design, and the measured
11 outcomes. Digital technologies show considerable promise for therapeutic research and
12 clinical management of HD. However, more studies with standardized devices and
13 harmonized protocols are needed to optimize the potential applicability of wearable/portable
14 devices in HD.

15

16

1 **Introduction**

2 Huntington's disease (HD) is an autosomal dominant neurodegenerative disorder caused by
3 an expanded trinucleotide CAG repeat in the *HTT* gene.[1] Clinically it is characterized by
4 motor, behavioural, and cognitive signs and symptoms.

5 The natural history of *HTT* expansion carriers is divided into premanifest and manifest
6 phases, with "clinical onset" diagnosed on the basis of "unequivocal" motor signs such as
7 chorea.[2, 3] However, a long prodromal phase, lasting a decade or more, frequently precedes
8 this point and brings subtle motor, cognitive and behavioural features that can nonetheless be
9 disabling.[4]

10 Furthermore, signs and symptoms in HD can be extremely heterogeneous among patients and
11 can also vary over time in the same patient in a non-linear manner. For example, motor
12 impairment can range from the classical hyperkinetic involuntary movements to a more
13 subtle hypokinetic impairment of voluntary movements, as well as impairment of motor
14 coordination.[5] Additionally, signs and symptoms can also display short-term fluctuations.

15 Phenotypic variability and the difficulty in consistently detecting subtle early clinical
16 manifestations pose challenges to therapeutic development as well as clinical management.

17 The Unified Huntington's Disease Rating Scale Total Motor Score (UHDRS TMS), has been
18 "recommended" by the International Parkinson and Movement Disorder Society (MDS) for
19 the assessment of motor signs in HD[6] and included by the National Institute for
20 Neurological Disorder and Stroke HD group in a list of recommended sensitive outcome
21 measures to be used as primary or secondary endpoints HD clinical trials.[7] However, its use
22 in clinical trials has shown limited sensitivity, especially in the pre-manifest stage of HD.[3,
23 8] It is also unreliable in capturing day-to-day or minute-to-minute variability of motor signs
24 which could easily dwarf any treatment effect. In addition to more reliable measures, there is

1 therefore face value in assessing manifestations of HD over a longer period, with high-
2 frequency or continuous monitoring.

3 Quantitative measures of motor and cognitive alterations in HD can be an optimal tool to
4 detect and monitoring subtle modifications even in pre-manifest HD.[9, 10] However, such
5 quantitative assessment is mainly based on expensive and cumbersome technology that can
6 only be used in-clinic settings for limited time periods.[11]

7 Recently, advances in wearable/portable sensors, information and communication
8 technologies, have enabled a continuous monitoring of chronic diseases. The use of
9 wearable/portable sensors allows the collection of high-dimensional data from multiple
10 domains and during everyday activities, in order to obtain a detailed, objective and precise
11 picture of disease manifestations. In addition, GPS data can provide evidence on real-world
12 mobility and be a surrogate of social activity, while smartphones and other devices can also
13 be used to implement questionnaires about symptoms or cognitive tasks. The high spatial and
14 temporal resolution of the registered data allows the monitoring of long-term trends and
15 short-term fluctuations of symptoms, as well as the detection of “soft” signs and symptoms of
16 disease onset/progression, or of therapeutic response that would otherwise go unnoticed. By
17 improving signal to noise ratios, this could be useful to increase the power of clinical trials
18 for new drug discovery. The term ‘digital biomarkers’ is sometimes used to denote the
19 meaningful outputs derived from electronic sensor data, whether or not the equipment used is
20 wearable/portable.

21 Such technologies are still in their infancy when it comes to implementation in such settings.

22 Wearable/portable sensors, have been already used in numerous neurological disorders, such
23 as Parkinson’s disease (PD) and Alzheimer’s disease (AD) and other dementias [12, 13] and
24 in 2017 an Alzheimer’s Association Research Roundtable concluded with a strong

1 recommendation to pharmaceutical companies to include digital tools as secondary endpoints
2 in AD clinical trials in parallel with other already accepted and widely-used measures.[14]

3 We undertook a systematic review to provide a comprehensive overview of the use of such
4 devices in HD and provide an evidence basis to comment on possible future directions.

5

6 **Materials and methods**

7 *Search strategy and selection criteria*

8 An electronic database search was performed on April 29th 2019 on MEDLINE, Embase, and
9 IEEE Xplore in order to identify articles related to the use of wearable/portable sensors in
10 HD. In line with the PRISMA statement,[15] an additional manual search was performed
11 among the references of selected articles.

12 We developed detailed search strategies for each database searched. Please see Appendix 1
13 for the MEDLINE search strategy, Appendix 2 for the Embase search strategy, and Appendix
14 3 for the IEEE Xplore search strategy. The research was performed independently on the
15 three databases on Rayyan QCR web application[16] and duplicates were excluded
16 automatically with EndNote X9 and manually during the study selection process.

17 We included original articles and abstracts/conference proceedings of any language reporting
18 studies performed in humans that investigated the use of wearable/portable sensors to assess
19 motor, behavioural or cognitive signs/symptoms in pre-manifest and/or manifest HD. We
20 excluded review articles or book chapters. A wearable device was defined as an electronic
21 technology or computer designed to be worn on the body, or embedded into watches,
22 bracelets, clothing, and similar items. [17] A portable device was defined as any device that
23 can easily be carried or worn on a belt or in a pocket. Studies reporting quantitative motor or

1 cognitive assessment in HD using non-wearable sensors (e.g.: GAITRite instrumented
2 carpet[18] or the Saccadometer Advanced[19]) were excluded from this review.

3 ***Review process***

4 Two review authors independently screened for eligibility the titles and abstracts of all
5 identified references. The full-text of all potentially eligible reports were retrieved and
6 screened using the same procedure. Disagreements were resolved by discussion, or by
7 consulting a third author.

8 ***Validity analysis***

9 We conducted a validity analysis of the included wearable/portable devices/tools. We
10 followed the strategy proposed by the Movement Disorder Society Committee on Rating
11 Scales Development to appraise clinical assessment tools in HD.[6, 20-23] We included
12 seven criteria with a Yes/No/Not Applicable response, namely: 1- used in HD, 2- used in HD
13 by more than one group, 3- test-retest reliability, 4- ability to discriminate cases from
14 controls, 5- ability to capture disease stage/severity, 6- ability to capture changes over time,
15 7- ability to detect therapeutic response. The answer “Not Applicable” referred to the fact that
16 that criterion has never been investigated for that specific device/tool in HD.

17

18 **Results**

19 ***Search results***

20 The electronic search returned 2489 records (MEDLINE 382; Embase 1711; IEEE Xplore
21 396), resulting in 2119 records after removal of duplicates. Title and abstract screening
22 excluded 2086 records not meeting the inclusion criteria. We assessed 33 full-texts, of which
23 16 were conference abstracts/proceedings and 17 were full-text original articles. Five
24 conference abstracts were excluded because of duplications; and 2 conference abstracts due

1 to study outcomes (1 did not specify the inertial/wearable sensors used, and another presented
2 no results). Additional four original articles were included after a manual search across the
3 references of the assessed full-texts. At the end of the evaluation process, according to the
4 eligibility criteria, 30 references were included in the final review (*Figure 1*). Two
5 references[24, 25] refer to the same study, but present different analyses and results, so we
6 did not consider them as duplicates.

7 *General characteristics of the included studies*

8 The main characteristics of the included studies are listed in *Table 1*. Twenty-one of them
9 were published in indexed journals, while 9 were presented at international conferences.[26-
10 34] The included studies cover an extensive time period, with three studies reporting the use
11 of accelerometers before the year of 2000.[5, 35, 36]

12 The majority of the studies were focused on manifest HD, with only six including pre-
13 manifest HD participants,[24, 29, 37-40] one focusing on pre-manifest only,[41] and two,
14 performed before the availability of the HD genetic test, involving “at-risk” individuals.[35,
15 36] Six studies also included patients with other neurological diseases, like PD,[24-26, 32,
16 42] degenerative ataxia,[43] tic disorders,[43] stroke,[42, 44] and amyotrophic lateral
17 sclerosis.[32] All studies but four[26, 31, 36, 39] compared the patient data with healthy
18 volunteers. The study setting was “in-clinic” for 17 of the included studies, at the
19 participant’s home for 8,[5, 28, 31, 40, 41, 45-47] and both in-clinic and at home for the
20 remaining four.[24-26, 34, 48] The monitoring duration ranged from a few minutes (in-clinic
21 studies) to 8 weeks in the home environment.[31] All studies but three[31, 34, 46] were
22 cross-sectional. The mean follow-up was 2.0 years in one,[46] not specified in another,[34]
23 while Lipsmeier et al., although with a longitudinal study design, only reported preliminary
24 results of 8 weeks of monitoring.[31]

1 *Types of sensors*

2 Accelerometers were the type of sensors used most, initially uniaxial and later mainly tri-
3 axial. Only Saadeh and colleagues[32] proposed the use of a Flexi-force sensing resistor
4 (FSR: <https://www.tekscan.com/products-solutions/force-sensors/a201>. *Figure 2a*), a thin,
5 flexible piezoresistive force sensor. The sensor was placed unobtrusively into the shoe sole,
6 and was able to translate the force applied in a designed sensing area into gait data,
7 subsequently acquired and processed in a detection processor able to extract the
8 discriminating features to classify different neurodegenerative diseases. The acquired
9 information was then transferred to a mobile phone through a Bluetooth/Cloud network.[32]
10 The studies of Waddel and colleagues and Lauraitis and colleagues didn't use any kind of
11 motor sensor and they were based on an app for smartphone or tablet.[34, 47]

12 With advances in technology, the tested devices became lighter, smaller, and characterized by
13 higher sample frequency, longer life and bigger memory capacity. Furthermore, they became
14 flexible and dynamic. Other inertial measurement modules, such as gyroscopes, were added
15 to accelerometers. This allowed the collection of data about rotation around three axes in
16 addition to linear acceleration. Trojaniello and co-workers, Mannini et al., and Youdan et al.
17 used a magnetic and inertial measurement unit (MIMU) (OpalTM, APDM, Inc, Portland, OR,
18 USA. *Figure 2b*) attached to the subject ankles, wrists and lumbar spine and able to measure
19 accelerations, angular velocities and local magnetic fields.[30, 33, 42, 44] Dinesh and
20 colleagues and Adams and colleagues used technologically advanced multi-mode adhesive
21 flexible sensors (BioStampRc sensors, MC10 Inc, Lexington, MA, USA. *Figure 2c*) with a
22 weight of only 7 gr, and the possibility to operate in different modes including accelerometer,
23 electrocardiogram, electromyography, and gyroscope functions.[24, 25] They could be
24 positioned on several parts of the body, like regular plasters, being unobtrusive and well-
25 tolerated by the participants.[24]

1 Successive iterations made devices easier to wear and more comfortable. The sensors used by
2 Folstein and colleagues (dimensions: $3 \times 3 \times 6$ cm) needed to be taped to the dorsal surface
3 of both the subject's hands;[35] the Opal APDM sensors used by Trojaniello et al., Mannini
4 et al., and Youdan et al. were smaller (dimensions: $4.8 \times 3.6 \times 1.3$ cm) but still need to be
5 strapped at the subject ankles, wrists or over the subject lumbar spine with a semi-elastic
6 waist belt.[30, 33, 42, 44] In the same way, many other proposed IMUs and sensors needed to
7 be strapped at other body regions.[29, 37, 38, 43, 48, 49] Kegelmeyer et al. used two iPods
8 attached to two belts.[50] It is evident that all these solutions encompass a certain grade of
9 discomfort for the participant and preclude the wide use of the sensors in the home
10 environment, during the activities of daily living and for a long time interval. Later studies
11 used adhesive sensors or wrist-worn watch-type devices that can be worn with the minimum
12 discomfort. Hogarth and colleagues used devices fitted into shoes.[28] Lipsmeier and
13 colleagues proposed the use of paired smart-watches and smartphones that can be easily worn
14 in social situations (*Figure 2d*),[31] as well as other studies used small wrist-worn actigraphy
15 devices.[39-41]

16 ***Measured disease characteristics***

17 All the investigated disease characteristics are graphically summarised in *Figure 3*. The range
18 of motor characteristics quantitatively measured by wearable tools in HD encompassed both
19 involuntary and voluntary movements. Measured voluntary movements included specific
20 tasks, such as finger tapping, reaction time and movement time,[35] Timed up and go
21 test,[29, 30] and Money Box Test as a measure of upper limb motor activity,[27, 51] or other
22 structured motor tasks.[24] Other studies used wearable sensors to monitor sleep-wake
23 activity (time spent asleep and motor activity during sleep),[45] as well as sleep
24 measurements (total sleep time, sleep latency, sleep efficiency, and wake after sleep
25 onset),[39] or circadian rhythm.[40, 41] Several studies have investigated balance[38] and

1 walking/gait characteristics.[25, 26, 28, 30, 32, 33, 37, 38, 42, 44, 48, 52] Kegelmeyer et al.
2 made a quantitative biomechanical assessment of trunk control, measuring the trunk stability
3 during standing, sitting and walking, and the ability of individuals to modify trunk position
4 responding to some auditory cues.[50] Other studies considered a more general concept of
5 “activity level” during the performance of daily activities[5, 46] and quantitatively assessed
6 the daytime motor activity in a passive monitoring mode.[24, 48] The study proposed by
7 Lipsmeier et al using a wearable smartwatch and a portable smartphone, was the first to
8 provide a combination of passive monitoring and active tests, both in clinic and in the home
9 setting.[31] The active tests, performed using a portable smartphone app, included
10 questionnaires about mood, quality of life, and general wellbeing; cognitive tests, namely the
11 Symbol-digit Modalities Test and the Stroop Word Reading Test; motor tasks, such as the
12 Speed Tapping Test, the Draw a Shape Test, the Chorea Test, the Balance Test, and the U-
13 Turn Test. Furthermore, the smartphone was equipped with a GPS, in order to register the
14 daily activities of the participants (*Figure 3*). Both the devices were designed for long-term
15 monitoring and able to directly transmit the acquired data when connected to a Wi-Fi
16 network.[31] Also the smartphone app proposed by Waddel et al. contained tests to assess
17 several disease characteristics, like gait, chorea, voice, balance, dexterity, bodily motion, and
18 socialization,[34] whereas the tablet app proposed by Luraitis and co-workers was able to
19 track tremor and cognitive impairment using three tasks with touch and visual stimulus
20 modalities.[47]

21 Finally, only one study investigated the participants’ experience with the sensors through an
22 electronic survey about comfort, security of adhesion, and removal of sensors.[24] They
23 showed that the majority of participants found the sensors “comfortable” and “easy to
24 remove”, while there was a general dissatisfaction about the sensors’ adhesion.[24]

1 ***Performance of wearable devices in HD: what did they add to our knowledge?***

2 Despite the increasing use of wearable/portable sensors in HD, their contribution in
3 understanding the natural history of the disease or in better defining disease characteristics is
4 still limited. Some of the studies have been focused on evaluating the sensor performance and
5 the level of agreement between the registered parameters and some gold standards. Gait
6 parameters measured by wearable/portable sensors have been demonstrated having a strong
7 agreement with gold standard measurements, such as the GAITRite mat.[38] On the other
8 hand, wearable devices used for the assessment of circadian rhythm or sleep-wake activity,
9 produced poor agreement with the gold standard, polysomnography, especially in identifying
10 the awake periods in both asymptomatic and symptomatic individuals. The study of Townhill
11 and colleagues demonstrated that the Actiwatch Activity monitoring system (Cambridge
12 Neurotechnology Ltd) overestimated periods of wakefulness compared to EEG data.[40]
13 Maskevich and co-workers showed that both commercially available activity monitors (Fitbit
14 and Jawbone) and a research-based actigraph (Actiwatch Spectrum Pro, Philips/Respironics,
15 Murrysville, PA), presented low-agreement with polysomnography, significantly
16 overestimating or underestimating different sleep parameters.[39] Nevertheless, they have
17 been used in a few studies, demonstrating the general utility of actigraphy in distinguishing
18 between manifest HD and controls, with HD patients sleeping for a longer time period
19 compared to controls and presenting a higher percentage of involuntary movements during
20 sleep,[45] and even between pre-HD and controls based on sleep efficiency.[41]

21 The most interesting, common and reproducible information that wearable/portable
22 technologies have added to the HD field so far is related to their utility in automatically
23 distinguishing between patients and controls based on features of a specific trait or disease
24 characteristic. The most investigated trait has been gait/walking ability. Spatio-temporal gait
25 parameters, like velocity, step length, stride length, gait symmetry/regularity and postural

1 sway, derived by tri-axial accelerometers or inertial sensors, were able to differentiate
2 manifest HD from pre-manifest HD and/or healthy controls.[28, 38] The discrimination
3 ability of gait parameters between HD patients and healthy controls seems to increase at
4 home with a longer period of observation. Andrzejewski and colleagues showed that during
5 the in clinic visit, step time variability was increased in HD, compared to controls, while at
6 home differences were observed for all the considered gait parameters.[48] In addition, in the
7 home setting, all the analysed gait measures were able to differentiate HD based on their level
8 of motor impairment (i.e. patients with TMS < 50 from those with TMS \geq 50).[48] So, in the
9 home setting, the variability of the motor measures detected by the sensors was generally
10 greater than those observed in the controlled clinical environment, and with more
11 observations at home, additional differences in gait were detected.[48] Collett et al, proposed
12 the measurement of gait variability parameters as a tool to discriminate between manifest
13 HD, pre-manifest HD and controls, showing that manifest HD patients presented a higher gait
14 variability compared to pre-manifest and healthy controls.[37] Interesting, one of the
15 parameters of gait variation (Ratio ∇ , namely the ratio between the spatiotemporal variability
16 and the temporal variability of consecutive wave forms from vertical movements of a walk
17 test) was also smaller in pre-HD compared with controls and showed a high discrimination
18 ability between the two groups (AUC = 0.81).[37]

19 Other movement features extracted from wearable/portable sensors have been investigated
20 and proposed as potentially able to automatically and accurately classify HD and controls.
21 Among those, selected features extracted from the accelerometer data registered during a
22 multitasking active test for upper limbs (namely the Money Box Test),[27, 51] specific trunk
23 movements,[50] and angular trunk displacement[49] were the most interesting. Grimberger
24 and co-workers showed that patients with HD had greater angular trunk displacement
25 compared with controls and this increase in trunk sway was more pronounced in fallers than

1 in non-fallers and positively correlated with clinical chorea scores.[49] In the study of
2 Kegelmeier and colleagues, wearable accelerometers were used for rehabilitation purposes in
3 order to adjust trunk movements and reflexes in HD patients.[50] Youdan and colleagues
4 showed dual-task impairment in HD, reporting an increased total sway area, decreased gait
5 speed and decreased correct response to cognitive tasks in HD participants who performed
6 motor and cognitive tasks at the same time.[30]

7 Extracting meaningful and useful outcomes from high-dimension datasets is a major
8 challenge as digital biomarker technology becomes ever more complex. That was the reason
9 why some of the studies focused on advanced machine learning approaches and new
10 algorithms or analysis methods to extract parameters with the best discrimination ability and
11 increase the classification accuracy between HD and controls.[25, 32, 37, 44, 51, 52]
12 However, none of the proposed algorithms has been reproduced in a replication cohort.

13 ***Validity analysis***

14 The results are reported in *Supplementary Table 1*. Only one of the included devices/tools
15 fulfilled more than 3 of the proposed criteria.[5, 46] The majority of them had a positive
16 response to two criteria over seven. Six of them were positive to three criteria, and five of
17 them to one only.

18

19 **Discussion and future directions**

20 This work provides a comprehensive overview of the wearable/portable sensors applied for
21 the measurement of several disease characteristics in HD patients, both in the pre-manifest
22 and manifest stages of the disease.

23 This topic has risen in prominence during the COVID-19 pandemic, in which digital and
24 remote healthcare and monitoring technologies have been increasingly leveraged in order to

1 provide care and clinical trial continuity while minimising viral transmission; it is probable
2 that such technologies will continue to be used to a higher extent than before the
3 pandemic.[53]

4 Our results confirm that, in common with other neurodegenerative diseases,
5 wearable/portable technologies are of large interest in HD, so far mainly as a tool for
6 automatic discrimination of patients from healthy subjects, and to detect early signs and
7 symptoms of the disease. It is now clear that measurements of involuntary movements as well
8 as of other disease characteristics like trunk sway or sleep patterns/movements using
9 wearable/portable devices can be a reliable approach to identify patients in the manifest stage
10 of the disease and they are promising in the characterization of the pre-manifest and early
11 manifest phases as well. This is of a huge interest because advanced wearable technologies
12 represent a revolutionary approach in collecting data. They are able to measure objective
13 parameters in a tolerable way and to collect a large amount of data in “ecological”
14 environments, like homes or community settings in order to reduce measurement errors of in-
15 clinic assessments.[54, 55] Furthermore, wearable sensors and systems are able to maximize
16 the temporal and spatial resolution of motor and non-motor phenomena that are expected to
17 change over time, to be rare and occasional, or to happen by definition over long time
18 periods,[56] providing a more accurate and realistic report of the behaviour of interest.[57]

19 However, in the current scenario, as highlighted by the results of the validity analysis, a
20 major pitfall for the applicability of wearables/portables in clinical practice and therapeutic
21 investigations is the lack of validation of the proposed devices. The majority of them have
22 been used in a single population, with no data about reliability and reproducibility of the
23 acquired data and derived results.[58] Most studies used different hardware and methods, so
24 the wearable devices and acquired data cannot be readily compared, and most of the studies
25 lacked a validation cohort. Another limitation is the fact that the methodologies for the

1 analysis of the huge amount of collected data to obtain meaningful disease-related signal
2 from background noise, are a completely open field of discussion as well.[56] Furthermore,
3 as with any rapidly growing field of interest, there is no gold standard for the validation of
4 new proposed monitoring systems. Quantitative motor systems, such as GAITRite mats, can
5 be a good gold standard for wearable sensors which measure gait parameters, but there are no
6 corresponding reference electronic quantitative measures for wearables which measure other
7 disease characteristics. On the other hand, the use of clinical scales as gold standards for
8 validation of the proposed devices and collected features has several limitations related to the
9 discrete and rater-dependent nature of these scales and to their low temporal and spatial
10 resolution.[45, 59, 60] Finally, in the use of wearables/portables, selection bias must be
11 considered. Socio-cultural factors such as age and enthusiasm for technology may influence
12 recruitment and there is a lack of studies concerning the influence of relatives, gender,
13 education, and working condition on the use of wearable/portable technologies. Furthermore,
14 disease stage and functional status can play a role, as wearable/portable devices may not have
15 the same applicability or tolerability across all disease stages.

16 All these limitations, as long as the lack of integration and standardization of the measured
17 characteristics, are the major pitfalls responsible of the considerable distance between the
18 very promising role of wearable/portable sensors and other digital technologies in
19 neurodegenerative disorders, and their real adoption in clinical practice or in pharmacological
20 studies.[61] Despite at least two decades of wide spread of wearables and huge advances in
21 technologies, they have been only sporadically used as surrogates or exploratory end
22 points.[62, 63]

23 ***Future directions***

24 To advance the clinical applicability and utility of wearables/portables in HD there is an
25 urgent and essential need for standardization, harmonization, openness and validation of the

1 devices already available, which must be balanced with the pilot testing of successive
2 generations of new devices. A major effort towards international collaborations and
3 standardized and harmonized protocols for acquisition and analysis of data is needed, to
4 avoid duplication of investments and unnecessary burden on patients, to integrate the best
5 from different systems into a standard and easily accessible platform, and to increase the
6 number of study participants and the validity of the results. PD sets a positive example here.
7 A Task Force on Technology was created within the MDS in 2015
8 ([https://www.movementdisorders.org/MDS/About/Committees--Other-Groups/MDS-Task-
9 Forces/Task-Force-on-Technology.htm](https://www.movementdisorders.org/MDS/About/Committees--Other-Groups/MDS-Task-Forces/Task-Force-on-Technology.htm)) with the main aim of maximizing the diagnostic and
10 therapeutic potential of technology in the care of patients with movement disorders.[56]
11 Furthermore, in 2019, the same task force proposed a roadmap to implement patient-centred
12 digital outcome measures obtained using mobile technologies in PD.[61] They listed four
13 “unmet needs” for mobile technologies: 1- Defining relevant patient-centred digital targets
14 and outcomes to be captured with mobile health technologies (What to measure), 2- Selection
15 criteria to guide the choice of mobile health technology (How to measure), 3- Web-based,
16 open-source, modular, scalable and secure platforms for data analysis, integration, and
17 visualization (What to display), 4- Establish a roadmap for regulatory approval and adoption
18 into health care systems (How to disseminate). Subsequently they proposed a roadmap to
19 satisfy those needs, but discussed that several challenges must be fought before the roadmap
20 could be transferred to the real world.[61]

21 Aspects of HD that are currently under-investigated, such as non-motor symptoms, have the
22 potential to be studied using wearable technologies as well, adopting a more comprehensive
23 and holistic approach with the aim to measure a broader spectrum of HD features.

24 There are two ongoing clinical, prospective, observational studies of advanced multimodal
25 digital measurement systems. The first one is called “HD Wear - Wearable sensor system for

1 monitoring Huntington's chorea during activities of daily living” and is a single-centre study
2 conducted by the University of Rochester
3 (<https://clinicaltrials.gov/ct2/show/record/NCT03599076?view=record>). It started to recruit in
4 mid-2018 and it is still recruiting at the time of writing. Its main aim is to develop a wearable
5 sensor system for objective, sensitive, and continuous assessment of chorea in HD during
6 activities of daily living. It is expected to enrol 50 participants (pre-manifest HD, manifest
7 HD and healthy volunteers) and to monitoring them at home for 12 months. The second study
8 is called “Digital-HD – Digital Biomarkers in Huntington’s Disease”, a single-centre study,
9 conducted at our institution – UCL Huntington’s disease Centre – which aims to enrol 120
10 participants (40 manifest HD, 40 pre-manifest HD, and 40 healthy volunteers). The study
11 design includes three in-clinic visits (baseline, 12 months and 18 months) and a continuous
12 “passive monitoring” in the home environment wearing a smart-watch and carrying on a
13 GPS-provided smartphone during routine daily activities. Furthermore, some daily
14 smartphone-based “active tests” designed to measure a range of motor and non-motor
15 symptoms in HD are also included (*Figure 4*). The same platform is also part of two ongoing
16 clinical trials in HD, namely GENERATION-HD1, a phase III multicentre randomized,
17 placebo-controlled trial on the use of an antisense oligonucleotide against huntingtin mRNA,
18 and GEN-EXTEND, an open-label extension study regarding the same drug. This makes the
19 Digital-HD platform the first to be tested in both observational and interventional settings in
20 HD.

21 In summary, there is great promise that wearable and portable devices will contribute to a
22 new digital era of biomarkers for HD, as well as in other neurodegenerative disorders. The
23 availability of high-dimensional objective data with high spatial and temporal resolution is
24 expected to increase the statistical power and interpretability of clinical trials and to reduce
25 the sample size required to detect therapeutic effects.[64] They may eventually be used to

- 1 guide collaborative decision making for patients and clinicians, but much work is required
- 2 before such systems can be used as primary trial outcome measures or in the clinic.
- 3

Journal Pre-proof

1 Appendix 1**2 MEDLINE search strategy**

3 1 exp Huntington Disease/

4 2 (Huntingto\$ adj2 (disease or chorea)).ab,ti.

5 3 or/1-2

6 4 digital.tw.

7 5 exp Wearable Electronic Devices/

8 6 wearable\$.tw.

9 7 sensor\$.tw.

10 8 exp "Equipment and Supplies"/

11 9 device\$.tw.

12 10 tracker\$.tw.

13 11 accelerometer\$.tw.

14 12 inertial measurement unit.tw.

15 13 smartphone\$.tw.

16 14 gyroscope.tw.

17 15 or/4-14

18 16 and/3,15

19 17 (animals not humans).sh.

20 18 16 not 17

21

22 Appendix 2**23 Embase search strategy**

24 1 exp Huntington Disease/

25 2 (Huntingto\$ adj2 (disease or chorea)).ab,ti.

- 1 3 or/1-2
- 2 4 digital.tw.
- 3 5 exp Wearable Electronic Devices/
- 4 6 wearable\$.tw.
- 5 7 sensor\$.tw.
- 6 8 exp "Equipment and Supplies"/
- 7 9 device\$.tw.
- 8 10 tracker\$.tw.
- 9 11 accelerometer\$.tw.
- 10 12 inertial measurement unit.tw.
- 11 13 smartphone\$.tw.
- 12 14 gyroscope.tw.
- 13 15 or/4-14
- 14 16 and/3,15
- 15 17 (animals not humans).sh.
- 16 18 16 not 17
- 17

18 **Appendix 3**

19 IEEE XPlore search strategy

20 (huntington OR huntington's) AND (digital OR wearable OR sensor OR device OR tracker
21 OR accelerometer OR gyroscope OR unit OR smartphone)

22

23

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16

17

1 Figure legends

2 **Figure 1.** Flow-diagram for selection process.

3 **Figure 2.** Examples of wearable/portable sensors used in Huntington's disease. **a.** Flexi-force sensing
4 resistor (FRS), <https://www.tekscan.com/products-solutions/force-sensors/a201>; **b.** Magnetic and
5 inertial measurement unit (MIMU) (Opal™, APDM, Inc, Portland, OR, USA); **c.** Multi-mode
6 adhesive flexible sensors (BioStampRc sensors, MC10 Inc, Lexington, MA, USA); **d.** Smartphone
7 and smart-watch used for the Hoffmann-La Roche platform.

8 **Figure 3.** Disease characteristics investigated using wearable/portable sensors in HD.

9 **Figure 4.** Graphic summary of all the tests (smartphone-based active tests, passive monitoring with
10 wearables, and in-clinic tests) included in the Digital-HD study. **Daily Qs:** daily questions; **EQ-5D-**
11 **5L:** Euro Quality of life - 5 Dimensions – 5 Levels questionnaire; **WHODAS:** World Health
12 Organization Disability Assessment Schedule; **SDMT:** Symbol Digit Modalities Test

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Table 1. Summary of the included studies

First author + YOP	Journal	n. of patients	n. of controls	Longitudinal	Type of sensor	Wearing position	Duration of use	Location of monitoring	Measured disease characteristics	Main results
Myers 1979[36]	Biol Psychiatry	10 mHD, 15 at risk HD	0	no	Accelerometer	Not specified	Not specified	Clinic	Tremor	Accelerometer measures can detect and characterize tremor in manifest and pre-manifest HD
Folstein 1983[35]	Neurobehav Toxicology and teratology	17 mHD, 27 at risk HD	10	no	Three-axial piezoelectric accelerometer (Wilcoxon Model no.139)	Dorsal surface of subject's hands	4 tasks, 5 10-second trials for each task	Clinic	Involuntary movements; some voluntary movements (simple reaction time, finger tapping, movement time)	Motor abnormalities can be detected in manifest and at risk HD; screening of motor abnormalities in the population
van Vugt 1996[5]	Movement Disorders	14 mHD	14	no	Wrist-worn activity monitor (accelerometer) (Gaehwiler Electronic, Switzerland)	Non-dominant wrist	5 successive days and nights	Home	General daytime motor activity	Higher hypokinesia in HD patients
van Vugt 2001[46]	Movement Disorders	64 mHD	67	yes	Wrist-worn activity monitor (accelerometer) (Gaehwiler	Non-dominant wrist	5 successive days and nights	Home	General daytime motor activity	Higher hypokinesia in HD patients; correlation with impaired voluntary movements, disturbed posture and gait, and reduced

					Electronic, Switzerland)					functional capacity; progresses with functional disability
Hurelbrink 2005[45]	J Neurol	8 mHD	8	no	Actiwatch-Neurologica (Cambridge Neurotechnology)	Preferred wrist	48 hours	Home	Day- and night-time involuntary movements; Sleep-wake activity	Greater activity levels in HD while awake and during sleep; HD sleep longer than controls
Grimbergen 2008[49]	Movement Disorders	45 mHD	27	no	Digitally-based angular velocity transducer (SwayStar)	Lower back	Time to walk on the GaitRite carpet)	Clinic	Trunk movements	Trunk displacement significantly greater in patients than controls; increased trunk sway in fallers compared to non-fallers; clinical chorea scores positive correlated to the range of angular trunk motion
Khalil 2010[29]	JNNP 2010-EHDN suppl	10 mHD 5 pHD	6	no	AD_BRC sensor with a three-axial accelerometer	Sternum	Time of TUG performance	Clinic	Performance of Timed Up and Go Test	Accelerometer objective measures can be useful to catch disease specific features and so to differentiate between groups
Dalton 2013[38]	Gait and Posture	14 mHD 10 pHD	10	no	AD_BRC sensor with a three-axial accelerometer	Chest	Unspecified (duration of the examination in clinic)	Clinic	Balance; gait	An accelerometer based sensor may be an effective means of differentiating between premanifest and manifest Huntington's disease subjects
Rudzinska 2013[43]	Neurologia I Neurochirurgia Polska	43 DA 28 mHD 23 tic disorders	51	no	Three-axial accelerometer (BIOPAC)	Proximal phalanx of the third finger	1.5 minutes (accelerometer registration)	Clinic	Tremor	Postural and essential type tremor found in 10% of HD; prevalence of tremor is considerably higher among patients with degenerative ataxias compared

)			with HD, tic disorder and the control group. The most common type of tremor accompanying ataxias, HD and tic disorders is essential tremor type
Norberg 2013[26]	AFMR 2013 CA	15 PD or mHD	0	no	Wireless three-axial accelerometers (UCLA Wireless Health Institute)	Both ankles	4 50-foot timed training walks + 3 days of monitoring	Clinic and home	Gait	Wireless sensors can obtain multiple measures of gait and other physical activities in an inexpensive and unobtrusive manner
Trojaniello 2014[33]	IEEE Conference 2014	10 mHD	10	no	MIMU (Opal, APDM, Inc)	Ankle	1 minute walking	Clinic	Gait	The MIMU has about 30% of errors associated to the best estimates of gait direction changes for patients, compared to gold standard (GAITRite Math)
Collett 2014[37]	Gait & Posture	7 pHD 28 mHD	22	no	IMU (Pi-node Philips, Netherlands)	Taped over the fourth lumbar vertebra	8.8 or 10 meters walking	Clinic	Gait	More variability in gait parameters in mHD compared to controls; no differences between pHD and HC, except for 1 parameter of the phase plot analysis, which also correlated with UHDRS-TMS and DBS. Phase plot analysis as a sensitive method to detect gait changes in HD

Trojaniello 2015[42]	Gait & Posture	10 stroke 10 PD 10 mHD	10	no	MIMU (Opal, APDM, Inc)	Over the subject lumbar spine, between L4 and S2	1 minute walking	Clinic	Gait	Comparison of 3 different methods to detect gait events. None of the tested methods outperformed the others in terms of gait parameter determination accuracy. Missed or extra gait events were found for all methods where pathological populations were analysed
Hogarth 2015[28]	ICPDMD 2015	5 mHD	5	no	Shoe-worn inertial sensor (APDM Inc)	Both shoes	walking hours for 7 days	Home	Gait	Gait parameters correctly identified subjects. Significant differences between HD and HC in gait parameters
Townhill 2016[40]	J Neurosci Meth	9 mHD 4 pHD	9	no	Actiwatch-Neurologica (Cambridge Neurotechnology) + ambulatory EEG	Non-dominant wrist	24 h (EEG); 7 days continuously (Actiwatch)	Home	Circadian Rhythm	Actiwatch is not a reliable tool for measuring awake/sleep periods in patients with movement disorders; no differences in circadian rhythmicity between groups
Andrzejewski 2016[48]	J of HD	15 mHD	4	no	Accelerometer-based wearable PAMSys-X (BioSensics, Cambridge, MA)	Both ankles, both wrists, and chest	7 days	Clinic and home	General daily motor activity; gait	Same level of physical activity; differences in gait measures between HD and controls; feasible use of wearable sensors
Mannini 2016[44]	Sensors	17 mHD 15 post-stroke	10	no	MIMU (Opal, APDM, Inc)	Both ankles, and over the subject's lumbar spine between L4	Unspecified (duration of the examination)	Clinic	Gait	Propose and validation of a new machine learning framework for gait classification (normal vs

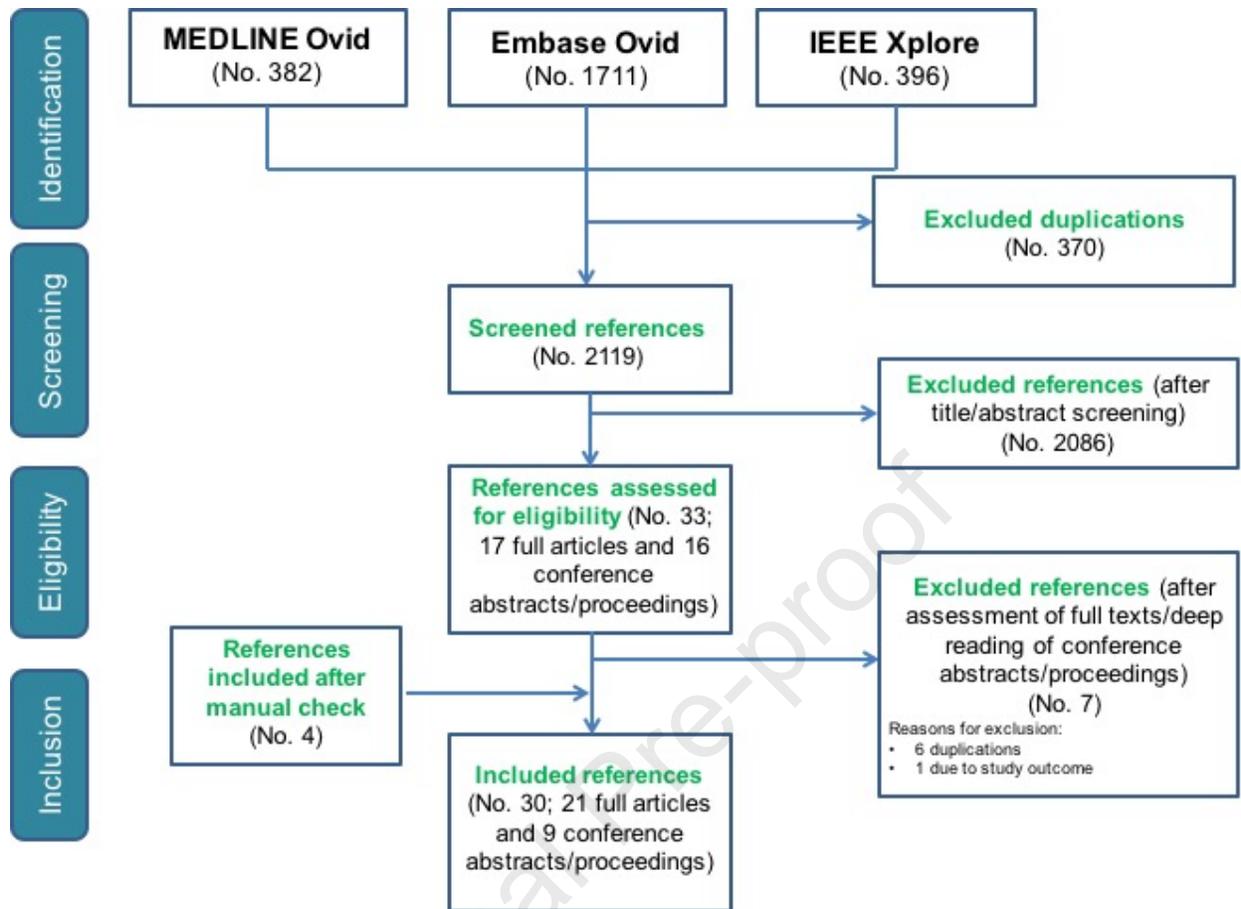
						and S2	n in clinic)			pathological)
Dinesh 2016[25]	IEEE Xplore Digital Library	16 PD 10 mHD	15	no	Accelerometer-based BioStampRC wearable sensors, MC10 Inc (Lexington, MA)	Both anterior thighs, both proximal anterior forearms, and medial chest	2 days	Clinic and home	Gait	Signal analysis of light-weight body-affixed sensors can detect motor symptoms associated with PD and HD
Bennassar 2016[27]	Procedia Computer Science (20th International Conference on Knowledge Based and Intelligent Information and Engineering Systems)	15 mHD	7	no	GENEActiv three-axial accelerometer (Activinsights Ltd, Cambridgeshire, UK)	Both wrists, and chest	Few minutes (time of completing the Moneybox-Test tasks)	Clinic	Movements of the upper limbs during the execution of the Money Box Test	Introduction of a new approach to automatically classify HD and controls (upper-limb movements)
Kegelmeyer 2017[50]	J Neurol Sci	41 mHD	36	no	iPod with the Level Belt Pro software installed	Back at the level of L5 and of the lower border of scapulae	Unspecified (duration of the examination in clinic)	Clinic	Trunk control	Significant greater amplitude of thoracic and pelvic movements in HD vs controls (++) in static than in dynamic tasks)

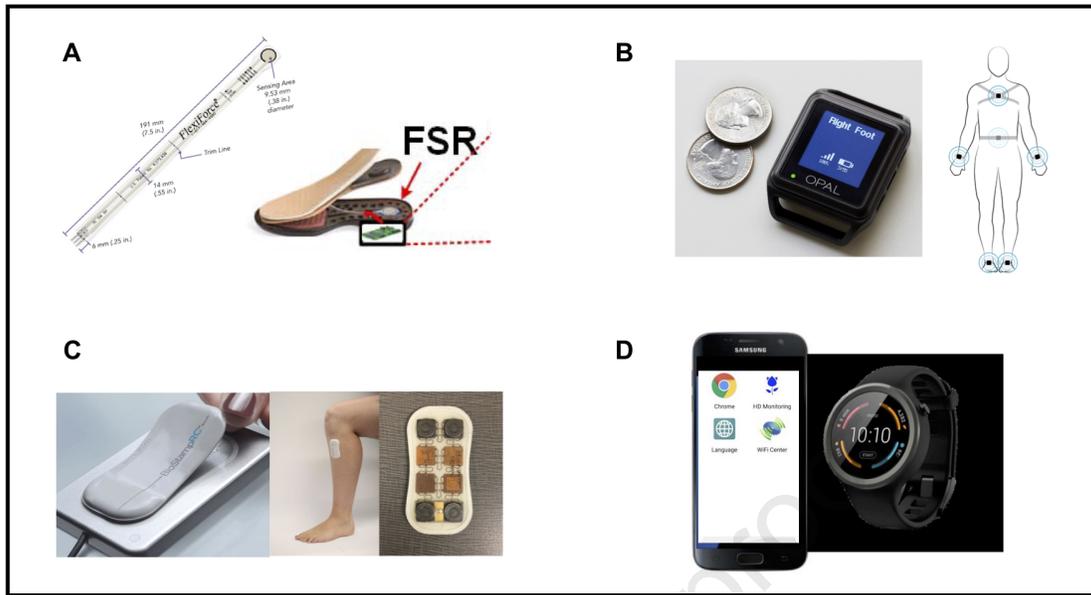
Maskevich 2017[39]	J of HD	4 pHD 3 mHD	0	no	Actiwatch Spectrum Pro (Philips/Respironics), Fitbit One and Jawbone UP2	Non-dominant wrist	Overnight	Clinic	Sleep characteristics	Three monitors less accurate of polysomnography to estimate sleep parameters in HD. Can't be a good replacement, but sufficient for overall estimations of sleep-wake patterns, and/or to assess gross level changes over time
Adams 2017[24]	Digit Biomark	15 mHD 5 pHD 16 PD	20	no	Accelerometer-based BioStampRC wearable sensors, MC10 Inc (Lexington, MA)	Both anterior thighs, both proximal anterior forearms, and medial chest	2 days	Clinic and home	General daytime motor activity	Patients with HD spent more time lying down; participants happy with the sensors
Saadeh 2017[32]	IEEE Conferences 2017	13 ALS, 20 mHD, 15 PD	16	no	Flexi-force sensing resistor (A201 Tekscan)	Shoe sole	Unspecified (used of an existing database?)	Clinic	Gait	The system classified the different groups with high sensitivity and specificity and a high classification accuracy
Youdan 2018[30]	HSG 2018	37 mHD	15	no	MIMU (Opal, APDM, Inc)	Medial chest, medial lower back, both ankles and both wrists	Time of task performing	Clinic	Gait; cognition	Dual-task impairment in HD compared to HC, as showed by increased total sway area, decreased gait speed and decreased correct response to cognitive tasks
Waddel 2018[34]	HSG 2018	14 subjects	?	yes	Android smartphone app (GEORGE)	Smartphone	1 month	Clinic and home	Gait, involuntary movements, voice, balance, dexterity, mobility,	Feasibility of the app

									socialization	
Lipsmeier 2018[31]	JNNP 2018-EHDN suppl	46 mHD	0	yes	Smartphone and Smartwatch (ROCHE platform)	Preferred wrist (smartwatch) and belt or trouser pocket (smartphone)	8- week preliminary results	Home	General daytime motor activity; motor tasks; chorea; balance; cognition; mood; quality of life	Good adherence; feasibility
Lauraitis 2018[47]	IEEE j of Biomedical and Health Informatics	11 mHD	11	no	Android tablet app	Tablet	Once or twice a week for an unspecified period	Home	Motor and cognitive abilities through three tasks	High classification accuracy of the app and useful support for automated medical examination
Acosta-Escalante 2018[52]	IEEE Special edition on trends, perspectives and prospects of machine learning applied to biomedical systems in internet of medical things	7 mHD	7	no	Movement sensors on two smartphones iPhone 5S	Both ankles	Walking on a 20-m path during visits of 7 consecutive days	Clinic	Gait	Meta-classifier algorithms useful for improving accuracy in classification and reducing the number of sensor devices needed. Best performance of Logitboost & RandomForest combination
Bennasar 2018[51]	IEEE transactions on neural systems and	44 mHD	48	no	Three-axial accelerometer GENEactiv	Both wrists, and chest	Few minutes (time of completing)	Clinic	Movements of the upper limbs during the execution	Presentation of a system for an objective and continuous assessment of motor impairment during a novel

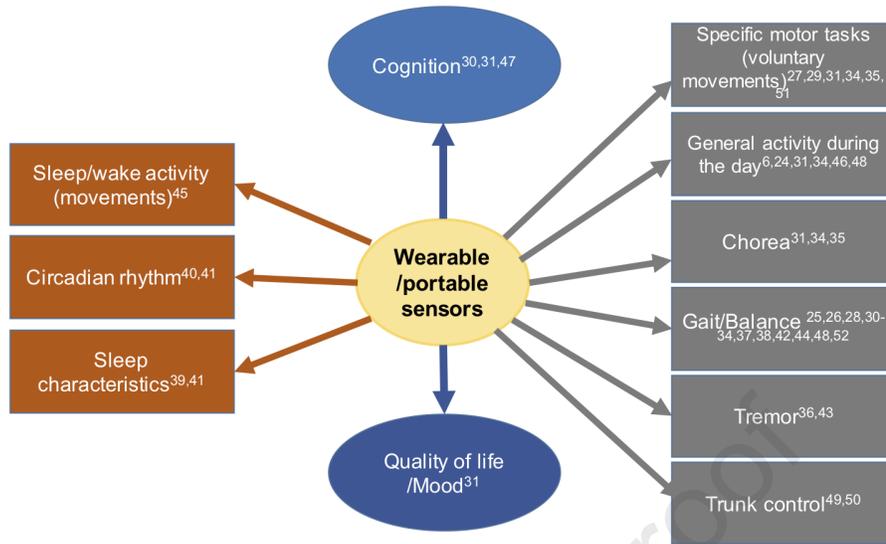
	rehabilitation engineering						the Moneybox -Test tasks)		of the Money Box Test	upper limb task for HD patients
Bartlett 2019[41]	Neurobiol of Sleep and Circadian Rhythms	32 pHD	29	no	Wrist-worn actigraphy GT3X+ ActiGraph monitor	Non-dominant wrist	7 nights	Home	Circadian rhythm and habitual sleep characteristics	Decreased habitual sleep efficiency and increased awakenings in pHD compared with HC. No association between hypothalamic volume and circadian rhythm or habitual sleep outcomes in pre-HD

YOP: year of publication; **HD**: Huntington's disease; **mHD**: manifest Huntington's disease; **pHD**: pre-manifest Huntington's disease; **PD**: Parkinson's disease; **DA**: degenerative ataxia; **ALS**: amyotrophic lateral sclerosis; **HC**: healthy controls; **IMU**: inertial measurement unit; **MIMU**: magnetic inertial measurement unit; **UHDRS-TMS**: unified Huntington's disease rating scale – total motor score; **DBS**: disease burden score.





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ACTIVE TESTS										
PROs			Cognitive Tests		Upper Body Motor Tests			Stability and Gait		
Daily Qs	EQ-5D-5L	WHODAS	SDMT	Word Reading	Speeded Tapping	Draw a Shape	Chorea	Balance	U-Turn	2-min Walk
										
Daily	Weekly	Monthly	Weekly	Weekly	Daily	Daily	Daily	Daily	Daily	Daily

PASSIVE MONITORING			IN CLINIC TESTS		
Activities of Daily Living			All Active Tests	Stability and Gait	
Gait	Chorea	Activity Levels		Timed Up and Go	Berg Balance
					