Harnessing recombinase polymerase amplification for rapid multi-gene detection of SARS-CoV-2 in resource-limited settings

Dounia Cherkaoui, Da Huang, Benjamin S. Miller, Valérian Turbé, Rachel A. McKendry

PII: S0956-5663(21)00365-1

DOI: https://doi.org/10.1016/j.bios.2021.113328

Reference: BIOS 113328

To appear in: Biosensors and Bioelectronics

Received Date: 27 January 2021

Revised Date: 26 April 2021

Accepted Date: 7 May 2021

Please cite this article as: Cherkaoui, D., Huang, D., Miller, B.S., Turbé, V., McKendry, R.A., Harnessing recombinase polymerase amplification for rapid multi-gene detection of SARS-CoV-2 in resource-limited settings, *Biosensors and Bioelectronics*, https://doi.org/10.1016/j.bios.2021.113328.

This is a PDF file of an article that has undergone enhancements after acceptance, such as the addition of a cover page and metadata, and formatting for readability, but it is not yet the definitive version of record. This version will undergo additional copyediting, typesetting and review before it is published in its final form, but we are providing this version to give early visibility of the article. Please note that, during the production process, errors may be discovered which could affect the content, and all legal disclaimers that apply to the journal pertain.

© 2021 Elsevier B.V. All rights reserved.

- <sup>1</sup> Harnessing recombinase polymerase amplification for
- 2 rapid multi-gene detection of SARS-CoV-2 in resource-

## 3 limited settings

- 4 Dounia Cherkaoui<sup>a,b,1</sup>, Da Huang<sup>a,1</sup>, Benjamin S. Miller<sup>a</sup>, Valérian Turbé<sup>a</sup>, & Rachel A.
- 5 McKendry<sup>a,b</sup>\*
- <sup>a</sup> London Centre for Nanotechnology, University College London, London, United Kingdom
- 7 <sup>b</sup> Division of Medicine, University College London, London, United Kingdom

- 9 <sup>1</sup>These authors contributed equally to this work.
- 10 \* Corresponding author
- 11 Name: Professor Rachel McKendry
- 12 Address: London Centre for Nanotechnology, University College London, 19 Gordon Street,
- 13 London, United Kingdom
- 14 E-mail: <u>r.a.mckendry@ucl.ac.uk</u>
- 15 Telephone number: +44 (0)20 7679 9995

#### 16 Abstract

17 The COVID-19 pandemic is challenging diagnostic testing capacity worldwide. The mass 18 testing needed to limit the spread of the virus requires new molecular diagnostic tests to 19 dramatically widen access at the point-of-care in resource-limited settings. Isothermal 20 molecular assays have emerged as a promising technology, given the faster turn-around time 21 and minimal equipment compared to gold standard laboratory PCR methods. However, unlike PCR, they do not typically target multiple SARS-CoV-2 genes, risking sensitivity and 22 23 specificity. Moreover, they often require multiple steps thus adding complexity and delays. 24 Here we develop a multiplexed, 1-2 step, fast (20-30 minutes) SARS-CoV-2 molecular test 25 using reverse transcription recombinase polymerase amplification to simultaneously detect two conserved targets - the E and RdRP genes. The agile multi-gene platform offers two 26 27 complementary detection methods: real-time fluorescence or dipstick. The analytical sensitivity of the fluorescence test was 9.5 (95% CI: 7.0-18) RNA copies per reaction for the 28 29 E gene and 17 (95% CI: 11-93) RNA copies per reaction for the RdRP gene. The analytical 30 sensitivity for the dipstick was 130 (95% CI: 82-500) RNA copies per reaction. High 31 specificity was found against common seasonal coronaviruses, SARS-CoV and MERS-CoV 32 model samples. The dipstick readout demonstrated potential for point-of-care testing in 33 decentralised settings, with minimal or equipment-free incubation methods and a user-34 friendly prototype smartphone application. This rapid, simple, ultrasensitive and multiplexed 35 molecular test offers valuable advantages over gold standard tests and in future could be 36 configurated to detect emerging variants of concern.

37

38 Keywords: nucleic acid testing, multi-gene, isothermal amplification, recombinase

39 polymerase amplification, SARS-CoV-2, real-time detection, dipstick.

#### 40 **1. Introduction**

At the end of December 2019, a public health alert was released from Wuhan, Hubei 41 42 province, in China reporting cases of "viral pneumonia of unknown cause" observed in 43 several patients with severe acute respiratory syndrome (Wu et al., 2020). Eventually, the 44 newly identified virus was designated as severe acute respiratory syndrome coronavirus 2 45 (SARS-CoV-2) (Gorbalenya et al., 2020) and the disease caused by the virus was named COVID-19 (World Health Organization, 2020d). As of 8<sup>th</sup> January 2021, a year after the 46 47 discovery of the human coronavirus SARS-CoV-2, the World Health Organization reported 48 globally over 86.4 million confirmed cases and 1.8 million deaths from COVID-19 (World 49 Health Organization, 2021).

50

Rapid development of diagnostic tests for detection of SARS-CoV-2 has been vital to limit 51 52 the spread of the virus (World Health Organization, 2020c). Molecular diagnosis is necessary 53 to identify patients actively infected when COVID-19 symptoms are not clearly differentiable 54 from other coronaviruses, for instance HCoV-NL63, HCoV-OC43 and HCoV-229E, causing 55 common cold, or the deadly Severe Acute Respiratory Syndrome Coronavirus (SARS-CoV) 56 and Middle East Respiratory Syndrome Coronavirus (MERS-CoV). These tests are also 57 needed to identify asymptomatic cases (not showing symptoms) or pre-symptomatic cases 58 (not showing symptoms at the time of test but developing symptoms later), which can be 59 infectious (Furukawa, Brooks, & Sobel, 2020). Since the early stages of the pandemic, the 60 World Health Organization has recommended the use of quantitative reverse transcription 61 polymerase chain reaction (qRT-PCR) for nucleic acid amplification as the gold standard 62 diagnostic for SARS-CoV-2 (World Health Organization, 2020b). In-house qRT-PCR protocols were swiftly developed and recommended for wide use in reference laboratories, 63 64 such as Hong Kong University (National Institute for Viral Disease Control and Prevention,

65	2020), Charité Institute of Virology Universitätsmedizin Berlin (Charité-Berlin) (Corman et
66	al., 2020) and United States Centers for Disease Control (US CDC) (Centers for Disease
67	Control and Prevention, 2020). Although targeting various conserved regions of SARS-CoV-
68	2, these qRT-PCR protocols all function with multiple gene targets to make the test more
69	sensitive and specific (Supplementary Fig. 1), following specific criteria for laboratory-
70	confirmed cases set by the World Health Organisation early on in the pandemic (WHO,
71	2020). Moreover, the importance of multi-gene detection is also important due to the rise of
72	variants of concern (Peñarrubia et al., 2020). For example, the S gene mutations in the
73	B1.1.17 variant, first detected in the UK, led to "S gene target failure" in some molecular
74	tests (Public Health England, 2020). The risk of target failure is minimised by multi-gene
75	detection and targeting of the most highly conserved regions of the viral genome.
76	
77	Despite the World Health Organisation's recommendation to use qRT-PCR technology for
78	detection of SARS-CoV-2, the pandemic has highlighted major issues in relying on only one
79	technology: a worldwide shortage of qRT-PCR reagents and instruments considerably slowed
80	down testing (FIND, 2020; Vandenberg, Martiny, Rochas, van Belkum, & Kozlakidis, 2020).
81	The massive number of tests needed to contain the spread of the virus could not be met for
82	many months, even in high-income countries (GOV.UK, 2020). Having viable alternatives to
83	qRT-PCR for acute COVID-19 that are as sensitive, but faster and simpler to use –
84	particularly in decentralised and resource-limited settings in the low and middle income
85	countries - could increase the testing capacity and reduce community transmission (Sheridan,
86	2020).
87	

88 A plethora of new diagnostics technologies have been reported (Choi, 2020), including

89 electrochemical sensing (Chaibun et al., 2021; Simoska & Stevenson, 2019; Yousefi et al.,

2021), paper-based testing (Carrell et al., 2019; Choi et al., 2016; Rodriguez, Wong, Liu,
Dewar, & Klapperich, 2016) and SERS-based biosensing (Carlomagno et al., 2021), targeting
antigen and molecular biomarkers. Antigen testing, based on the detection of viral proteins,
has some advantages over PCR, as these tests are often low-cost, fast and can be performed
outside the laboratory (Guglielmi, 2020). However, their sensitivity is often significantly
lower than nucleic acid amplification-based tests, missing up to 60% of PCR-positive
asymptomatic patients (University of Liverpool, 2020).

97

Several promising isothermal techniques have emerged as PCR alternatives, including 98 99 recombinase polymerase amplification (RPA), and loop-mediated isothermal amplification 100 (LAMP) that could meet the needs for mass SARS-CoV-2 testing .They are portable, faster, 101 usually giving results in 5-20 minutes, compared to several hours with qRT-PCR, enabling 102 testing in settings with scarce resources, without a thermocycler (Daher, Stewart, Boissinot, 103 & Bergeron, 2016; Mori & Notomi, 2009). Indeed, the first molecular test for home use to 104 receive FDA authorisation for emergency use, harnessed isothermal amplification (RT-105 LAMP) but requires higher temperature (65°C) than RPA (U.S. Food and Drug 106 Administration, 2020a). Another commercial test instrument based on isothermal 107 amplification is the rapid and portable Abbott ID NOW<sup>™</sup> COVID-19 test which needs only 5 108 minutes to deliver a positive result and 13 minutes for a negative result (Abbott, 2020), 109 however it requires a benchtop instrument. Several LAMP assays have also been successfully 110 developed, among which some multiplexed assays detect two genes but require a much 111 higher temperature (60-65°C compared to 37-42°C for RPA) and two pairs of primers instead 112 of one, making their design slightly more complex. By contrast RPA-based amplification 113 enables the reaction to be carried out with basic equipment to achieve the necessary 114 temperature, such as a water bath or a hand warmer bag.

116	To date only a few RPA-based tests for SARS-CoV-2 are reported in the literature
117	(Behrmann et al., 2020; El Wahed et al., 2021; Lau et al., 2021; Qian et al., 2020; Xia &
118	Chen, 2020; Xue et al., 2020). However, unlike PCR, they do not typically target multiple
119	SARS-CoV-2 genes, risking sensitivity and specificity. Moreover, they often require multiple
120	steps thus adding complexity and delays in the time to result. 'One-pot' reverse transcription
121	RPA (RT-RPA) can rapidly amplify viral RNA and detection of the RPA product is in
122	principle possible and has been demonstrated for other viruses by several methods, the most
123	common are by real-time fluorescence or using dipsticks. For example, an ultrasensitive
124	diagnostic assay using RPA and dipstick was successfully demonstrated for HIV using novel
125	nanoparticles (Miller et al., 2020).
126	
127	RPA also has several advantages over other protocols coupling isothermal amplification with
128	the endonuclease activity of CRISPR/Cas enzymes (Arizti-Sanz et al., 2020; Broughton et al.,
129	2020; Ding et al., 2020; Patchsung et al., 2020). Although the pairing of CRISPR
130	technologies with RPA might increase the specificity of an assay, thanks to the RNA-guided
131	cleavage, this additional CRISPR step may increase the reaction time (typically 40-50
132	minutes), the cost and complexity of the assay.
133	
134	Therefore, there is an unmet need for an RPA assay which simultaneously targets multiple
135	SARS-CoV-2 genes, to ensure the high sensitivity and specificity required for COVID-19
136	mass testing. The assay needs to have minimal number of steps (ideally 1-2) to make it
137	accessible and usable and ensure a rapid time to result. Moreover, rapid tests with mobile
138	phone-based connectivity, have emerged as an important criterion in REASSURED
139	diagnostic tests (Wood et al., 2019). The REASSURED criteria build on the previously

140	described ASSURED criteria (Mabey, Peeling, Ustianowski, & Perkins, 2004), notably
141	adding real-time connectivity and ease of specimen collection as test requirements for point-
142	of-care application. By taking advantage of their processing speeds, display, storage capacity,
143	their high resolution camera and connectivity, smartphones are useful devices to store
144	information relative to the test and the patient, analyse test results with an enhanced readout
145	compared to the naked eye, to communicate the result to a local hospital and send alerts in
146	case a new outbreak or cluster is detected (Brangel et al., 2018; Budd et al., 2020).
147	
148	Here we report the development of a rapid molecular diagnostic for the detection of SARS-
149	CoV-2 by RT-RPA (Fig. 1a) simultaneously detecting two gene targets (Fig. 1b). We aimed
150	to design two alternative readouts, which are both multiplexed: real-time fluorescence (Fig.
151	1c) and dipsticks (Fig. 1d). Offering two detection methods makes the assay more accessible
152	to different settings, depending on their resources. To the best of our knowledge, this is the
153	first one-pot multiplexed RPA-based assay for SARS-CoV-2. We also explore the use of
154	low-cost handwarmers to achieve the required temperature, and also a smartphone app to
155	capture and interpret test results.
156	
157	Fig. 1 Schematic representation of the rapid and multiplex RT-RPA assay with real-
158	time fluorescence and dipstick detection.
159	
160	2. Materials and methods
161	2.1. Reagents and equipment

162 RPA primers and the cDNA control for the N gene were obtained from Integrated DNA

163 Technologies. The cDNA controls for the E, RdRP and Orf1ab genes were supplied by

164 GenScript Biotech (pUC57-2019-nCoV-PC:E, pUC57-2019-nCoV-PC:RdRP, pUC57-2019-

165 nCoV-PC:ORF1ab). The coronavirus specificity panel (SARS-CoV-2, SARS-CoV, MERS-166 CoV, HCoV-NL63, HCoV-OC43 and HCoV-229E) was obtained from the European Virus 167 Archive (EVAg). These RNA samples were supplied as full-length virus RNA with reported 168 cycle threshold (Ct) values between 28-30 from qRT-PCR assays. The fluorescent probes 169 were synthesized by Eurogentec. The RPA reactions kits were ordered from TwistDX. The QIAquick Gel Extraction and PCR Purification kits were ordered from Qiagen. The 170 Phusion<sup>TM</sup> High-Fidelity DNA Polymerase kit and the M-MLV reverse transcriptase were 171 172 from Thermo Fisher Scientific. The in vitro transcription and the RNA purification was performed with the HiScribe<sup>TM</sup> T7 Quick High Yield RNA Synthesis kit and Monarch RNA 173 CleanUp kit from New England Biolabs Ltd. SUPERase In<sup>TM</sup> RNase inhibitor from 174 175 Invitrogen was added to the RNA standards. Human saliva from healthy and pooled donors (cat. 991-05-P-PreC) was purchased from Lee Biosolutions, Inc. cDNA concentrations were 176 measured on a Nanodrop<sup>TM</sup> One/One<sup>C</sup> microvolume UV-Vis spectrophotometer. RNA 177 concentrations were measured on a Qubit 4 fluorometer using the Qubit<sup>TM</sup> RNA HS Assay 178 Kit (Invitrogen). Fluorescent readings were done on the microplate reader SpectraMax<sup>®</sup> iD3 179 from Molecular Devices, for initial screening of SARS-CoV-2 genes, then the Axxin<sup>®</sup> T16-180 ISO was used for the duplex diagnostic platform. The dipsticks and running buffer were 181 182 obtained from Abingdon Health.

183

## 184 2.2. Screening of four different genes (N, E, RdRP and Orf1ab genes) by real-time 185 RPA

186 RPA primers and probes with a FAM fluorophore were designed for four targets

187 (Supplementary Table 1) and screened using the TwistAmp® exo RPA reactions. The 50 µL

188 reactions contained TwistAmp® exo RPA pellets resuspended in 29.5 µL Rehydration Buffer

189 (TwistDX), 2.1 µL of forward primer (at concentration 10 µM), 2.1 µL of reverse primer (at

190 concentration 10 µM), 0.6 µL of probe (at concentration 10 µM), 1 µL of corresponding 191 cDNA template and 12.2 µL of nuclease-free water. Finally, 2.5 µL of magnesium acetate (at 192 concentration 280 mM) was added to start the reaction. Three cDNA concentrations (50, 500, 193 5000 copies) were tried along with a non-template control (NTC). The reactions were 194 incubated at 39°C for 30 minutes and real-time fluorescence was recorded using a microplate 195 reader (excitation wavelength 495 nm and emission 520 nm). The screen was done in 196 technical replicates (N=2). Background correction was done to remove potential variation 197 due to initial mixing and normalised the data to compare relative fluorescence increase. The 198 measurement at  $\approx 60$  seconds was used to set the fluorescence to zero, as initial mixing of 199 reactions can lead to variations in fluorescence. This method of background subtraction 200 allowed to set all first measurement values to zero, remove potential variation due to initial 201 mixing and enabled to compare relative fluorescence increase. Then, the average values of 202 duplicates were plotted on GraphPad Prism along with error bars, corresponding to the 203 standard deviation. The fluorescence threshold value for the RPA screen of the four genes 204 with cDNA was set to 25,000. This threshold value was calculated by averaging fluorescence 205 signals from several NTC reactions and adding 3 times the associated standard deviation. The 206 average time to threshold, defined as the time corresponding to the intersection of the 207 amplification curve with the threshold value, was determined for each gene.

208

#### 209 2.3. Synthesis of RNA standards for SARS-CoV-2 E and RdRP genes

The plasmid cDNA encoding for the E and RdRP genes were digested using a pair of
restriction sites of the plasmid. Double digestion allowed to isolate the sequence of interest
and get linear DNA. The product of digestion was run on a 1% agarose gel with a DNA
ladder. The band of interest was excised from the gel and the DNA was purified. To generate
positive-sense RNA transcripts, a T7 promoter sequence was added via PCR amplification

215	with the promoter sequence on the forward primer (Supplementary Fig. 2a). The PCR
216	products were verified on an agarose gel (Supplementary Fig. 2b). In vitro transcription was
217	done with 2.5 hours incubation, with several rounds of DNase I treatment to remove the DNA
218	template, and the RNA was purified. The RNA was tested by PCR using the RPA primers
219	(also suitable for PCR) to check for traces of DNA impurities (Supplementary Fig. 2c). The
220	concentration of the RNA transcripts was measured using the Qubit, then the RNA was
221	diluted in DEPC-treated water and stored at -80°C with RNase inhibitor. A dilution series
222	was used to measure the analytical sensitivity of the molecular test.
223	
224	2.4. Multiplex RT-RPA with real-time fluorescence detection
225	Amplification and detection of both genes was done using the multi-channel portable reader
226	(Axxin) using the FAM and HEX channels.
227	The 50 $\mu$ L reactions contained TwistAmp® exo RPA pellets resuspended in 29.5 $\mu$ L
228	Rehydration Buffer (TwistDX), 2.1 $\mu$ L of both forward primers (at concentration 10 $\mu$ M), 2.1
229	$\mu$ L of both reverse primers (at concentration 10 $\mu$ M), 0.6 $\mu$ L of both probes, 1 $\mu$ L of each
230	corresponding RNA samples (E and RdRP genes), 2.5 $\mu$ L of reverse transcriptase (at 200
231	U/ $\mu$ L) and 3.9 $\mu$ L of nuclease-free water. Finally, 2.5 $\mu$ L of magnesium acetate (at
232	concentration 280 mM) was added to start the reaction. The reactions were incubated at 39°C,
233	with magnetic shaking and the fluorescence was measured in real-time directly from the
234	tubes.
235	
236	2.5. Multiplex RT-RPA with dipstick detection

237 RPA primers for E and RdRP genes were modified (Supplementary Table 1) for duplex

238 detection on the dipsticks, which incorporate carbon nanoparticles conjugated to neutravidin.

239 The E gene primers were modified with biotin and digoxigenin for detection on test line (1),

240	whereas the RdRP gene primers were modified with FAM and biotin for detection on test line
241	(2). To eliminate non-specific binding due to dimers forming, the assay was tested without
242	any template (negative controls) with modified primers at concentration 10 $\mu M,$ 2 $\mu M,$ 1 $\mu M$
243	and 0.5 $\mu$ M. Eventually, the 50 $\mu$ L reactions contained TwistAmp® basic RPA pellets
244	resuspended in 29.5 $\mu$ L Rehydration Buffer (TwistDX), 2.1 $\mu$ L of both forward primer (at
245	concentration 1 $\mu$ M), 2.1 $\mu$ L of both reverse primer (at concentration 1 $\mu$ M), 1 $\mu$ L of each
246	corresponding RNA sample (E and RdRP genes), 2.5 $\mu$ L of reverse transcriptase (at 200
247	U/ $\mu$ L) and 5.1 $\mu$ L of nuclease-free water. Finally, 2.5 $\mu$ L of magnesium acetate (at
248	concentration 280 mM) was added to start the reaction. The reactions were incubated at 37°C
249	in an incubator for 20 minutes, with shaking at 250 rpm. Then, 10 $\mu$ L of reaction was mixed
250	in the well of a microplate with 140 $\mu$ L of running buffer, and the dipstick was dipped in the
251	well. The test result was read after 10 minutes. A photograph of the strips was taken at this
252	time and image analysis was done on Matlab (R2020b).
253	Detection of RNA transcripts spiked in human saliva was done following the protocol for
254	RT-RPA with dipstick readout, yet the 5.1 $\mu$ L of nuclease free-water were replaced by human

255 256 saliva.

#### 257 **2.6.** Calculation of fluorescence thresholds and analytical sensitivity

258 Two thresholds were calculated for the RT-RPA protocol using the FAM and HEX dyes. The

thresholds were computed from eight NTC reactions. The maximum fluorescence values

260 were taken after background subtraction. The average of these values and the standard

261 deviation were calculated. Finally, the thresholds were calculated as followed:

262  $Threshold = average(NTC) + 4.785 \times standard deviation(NTC)$ 

- 263 The multiplication factor 4.785 corresponds to the 99.9% confidence interval of the t-
- distribution with seven degrees of freedom, as per the equation 1 for determining limit of

- blank (Holstein, Griffin, Hong, & Sampson, 2015). This high confidence interval was chosen
  to strengthen the specificity of the assay.
- 267 The analytical sensitivity of the RT-RPA with real-time fluorescence readout was done using
- these thresholds. Repeats were run five times for a range of RNA inputs: 1, 2.5, 5, 7.5, 10,
- $10^2$  and  $10^3$  (only for the RdRP gene). The fraction of positive reactions (reactions which
- 270 reached the threshold in less than 20 minutes) was calculated separately for both genes and
- 271 probit analysis was done on Matlab (R2020b).
- 272 The EC<sub>95</sub> was calculated from the probit analysis with its 95% CI. The EC<sub>95</sub> was defined as
- the analytical sensitivity of the test.
- 274
- 275 **2.7.** Testing of coronavirus specificity panel
- 276 RT-RPA protocol (for both real-time and dipstick readout) was followed to test cross-
- 277 reactivity of the assay with other coronaviruses, namely SARS-CoV, MERS-CoV, HCoV-
- 278 NL63, HCoV-OC43 and HCoV-229E. As the RNA concentrations of the stock RNA
- 279 received from supplier was unknown, the RT-RPA assays were run with 5 µL of RNA
- 280 directly from stock. The SARS-CoV-2 RNA sample supplied with the specificity panel was

also run with 5  $\mu$ L from stock for comparison with the other coronaviruses.

282

#### 283 **2.8. Smartphone application**

- 284 The "CovidApp" smartphone application was developed in Android Studio using java
- libraries. Screenshots were taken from the emulator using a Galaxy Nexus API 28. The
- 286 complete code for the Android application is available on request.
- 287 The application opens onto a homepage where the users can choose between three activities
- 288 "Test", "Alerts" or "Map outbreak". The "Test" activity includes first recording of patient
- information (patient ID, date of birth, GPS and symptoms). The GPS coordinates are

290 captured in real-time by clicking the button and time and date are also automatically captured. Then, the user can click on the "Take Test Picture" button to get access to the 291 292 smartphone camera and take a photograph of the lateral flow test. Manual cropping is 293 required to crop onto the result area of the test (where the lines are). Another activity enables 294 image analysis of the cropped image for enhanced visualisation of the test lines and plotting of the test line intensity. Finally, the user can select between the options "three lines", "two 295 lines", "one line", "no line" which records the test result as "positive", "presumptive 296 297 positive", "negative" or "invalid". If the user test result is "positive" or "presumptive positive", the user is taken to the "Contacts" page when clicking on the "Next step" button. 298 299 This will enable to record the contacts of the positive case so then can be later reached by the 300 local contact tracing system. Finally, the activity "Map outbreak" opens to visualise the location of the tested case on the map. In the "Alerts" activity, the information of the patient, 301 302 with the test result, can be seen.

303

#### 304 **2.9.** Comparison of four incubation methods

305 RT-RPA for visual detection on dipstick was commonly done using a laboratory incubator (New Brunswick<sup>™</sup> Innova<sup>®</sup> 42) at 37°C with shaking at 250 rpm. Other incubation methods 306 307 were tried and compared including incubation in a water bath at 37°C, incubation on a hand warmer bag (HotHands<sup>®</sup> air activated) and by holding the tube in the hand. The temperature 308 309 released by the hand warmer bag was recorded using a K-type thermocouple with model 310 CL25 calibrator thermometer (Omega). The positive and negative reactions using these 311 different incubation methods were all done in parallel with an incubation time of 20 minutes. 312 Then, the reactions were analysed on dipsticks following the dipstick readout protocol.

313

#### 314 **3. Results**

315	3.1. Gene screening for detection of SARS-CoV-2 by real-time fluorescence
316	A pair of RPA primers and a fluorescent "exo" probe (Supplementary Table 1) were designed
317	to target four conserved regions of the SARS-CoV-2 genome in the nucleocapsid (N) gene,
318	the envelope (E) gene, the RNA-dependent RNA polymerase (RdRP) gene and the open-
319	reading frame 1a/b (Orf1ab). The RPA assay design was optimised for amplicon size of ~200
320	bp and long primers of ~30 bp. BLAST analysis indicated that these pairs and probes
321	specifically detect SARS-CoV-2 (100% identity). In addition, primers and probes sequences
322	were also screened through BLAST against seasonal coronaviruses, SARS-CoV and MERS-
323	CoV which revealed low identity score and high E value.
324	A preliminary gene screening aimed to identify the best two primers/probe sets among these
325	four targets, able to achieve rapid and sensitive detection of SARS-CoV-2 in a real-time RPA
326	assay. The gene screening was conducted with cDNA controls rapidly made available by
327	suppliers (Supplementary Fig. 3a). A single fluorescence threshold was used to compare the
328	four targets. All reactions using template, except one (50 copies for the N gene), showed
329	successful amplification of 50, 500 and 5,000 copies with fluorescent signals reaching the
330	threshold in less than 30 minutes (Supplementary Fig. 3b). Then, the average time to
331	threshold was determined for each gene and it was used to compare them (Supplementary
332	Fig. 3c). The two genes with the shortest average time to threshold with 50 copies of cDNA
333	were the E gene, in 14 minutes, and the RdRP gene, in 19 minutes. The Orf1ab gene was
334	slightly slower than RdRP gene, while the N gene showed particularly low sensitivity in the
335	RPA protocol and did not reach the threshold with 50 copies. Eventually, the E and RdRP
336	genes were selected and multiplexed to make an in-house duplex RT-RPA protocol to detect
337	SARS-CoV-2 virus. An analysis of genome variations (determined from 5139 sequenced
338	genomes deposited on https://www.gisaid.org/) for the selected primers and probes confirmed

that they target conserved regions of the SARS-CoV-2 genome with low variability

340 comprised between 0.1-0.5% (Supplementary Fig. 4).

341

#### 342 **3.2.** Development of the duplex RT-RPA platforms

343 The RT-RPA assay was developed with two complementary detection systems (Fig. 1a). 344 First, an optical fluorescent readout similar to qRT-PCR that uses fluorescent probes to monitor real-time amplification of the target was made by multiplexing fluorophores to 345 346 simultaneously detect the amplicons of the E gene with FAM and RdRP gene with HEX (Fig 347 1.c). The fluorescent probe was designed as a short ~45-50 oligonucleotide sequence, 348 complementary to the target sequence. The fluorescent probe included a fluorophore and a 349 proximal quencher, separated by a tetrahydrofuran (THF) residue. When the fluorescent 350 probe recognised the target sequence, it annealed and was cleaved at the THF site by the 351 exonuclease contained in the exo RPA reaction. As the fluorophore was released from its 352 quencher, a fluorescent signal was produced and recorded on a multi-channel and portable 353 fluorescence reader.

354 A second detection method was developed using dipsticks to detect the amplicons on a 355 nitrocellulose strip using nanoparticle labels. Dipsticks are lateral flow tests which are not 356 enclosed in a cassette; hence they are lower cost and can be dipped directly in the analyte. 357 The dipstick-based platform was developed to be as low-cost and minimalist as possible. The 358 primer sequences used were the same as for the real-time fluorescence readout above, but 359 these primers were modified with small molecules to mediate capture of the amplicons on the 360 test lines of the dipstick (Supplementary Table 1). Optimisation of the primer concentration 361 was needed to eliminate non-specific binding on the test lines (Supplementary Fig. 5) 362 attributed to binding of dimerised primers when used in excess (> 1  $\mu$ M). After the 363 amplification was performed, detection of the two amplicons was possible on two distinct test

lines: (1) for the E gene, (2) for the RdRP gene and a control line (C) provided confirmationthat the test had worked properly (Fig. 1d).

366

#### 367 3.3. Evaluation of the RT-RPA assay with real-time fluorescence detection

The analytical sensitivity was measured for the real-time RT-RPA assay and defined as the concentration of analyte, here synthetic SARS-CoV-2 viral RNA copies per reaction, that can be detected  $\geq$  95% of the time (< 5% false negative rate).

371 To determine the analytical sensitivity of the RT-RPA fluorescence readout two thresholds

372 were calculated, to account for the different background fluorescence of the FAM and HEX

373 fluorophores (see Material and methods section). The resulting thresholds were 112 for the E

374 gene (FAM) and 13 for the RdRP gene (HEX). RT-RPA reactions were run for different

375 RNA inputs ranging from 1 copy to  $10^5$  copies and real-time fluorescence was recorded. The

time to threshold was determined for reactions reaching threshold in 20 minutes of

amplification (Fig. 2a). The amplification time was fixed at 20 minutes, as the assay was able

to detect as little as 1 RNA. To measure the analytical sensitivity of both genes, we calculated

379 the fraction positive to find and plot the  $EC_{95}$  (see "Methods" section). The analytical

380 sensitivity was 9.5 RNA copies per reaction (95% CI: 7.0-18) for the E gene and 17 RNA

381 copies per reaction (95% CI: 11-93) for the RdRP gene (Fig. 2b).

382 The specificity of the RT-RPA assay was tested with model samples against common

383 seasonal coronaviruses, namely HCoV-NL63, HCoV-OC63 and HCoV-229E, as their

384 symptoms could be easily confused with COVID-19, and we also tested cross-reactivity with

385 SARS-CoV and MERS-CoV, as they are closely related viruses.

386 No cross-reactivity was observed with the primers/probe set targeting the E gene and the

387 RdRP gene when tested with SARS-CoV- and MERS-CoV and the common colds (Fig. 2c

and Fig. 2d). A slight increase in background signal could be observed, although remaining

comparable to the non-template control (NTC) reaction and the signal remained below thethresholds.

391

# Fig. 2 Evaluation of the sensitivity and specificity of the RT-RPA assay with real-time fluorescence detection.

394

#### 395 **3.4.** Evaluation of the RT-RPA assay with visual dipstick detection

396 The analytical sensitivity of the dipstick detection method was approximated by running a

397 range of RNA inputs, from 1 to  $10^5$  copies. Six replicates were performed (Supplementary

398 Fig. 6) of which one representative dipstick per RNA concentration is shown in Fig. 3a. The

399 test line intensity analysis was used to quantify test line intensity. Single-copy detection was

400 possible for 2/6 repeats (33%), giving in a positive result, defined as both test lines visible by

401 eye or with image analysis. The probit analysis was performed to determine the analytical

402 sensitivity of the assay using the fraction positive (Fig. 3b). The analytical sensitivity of the

403 dipstick method was 130 (95% CI: 82-500) RNA copies per reaction.

404 The specificity of the dipstick detection method was assessed against the common seasonal

405 coronaviruses, SARS-CoV and MERS-CoV (Fig. 3c). The dipstick showed high specificity

406 for only SARS-CoV-2 viral RNA and no cross-reactivity was seen with the other

- 407 coronaviruses.
- 408

409 Fig. 3 Evaluation of the sensitivity and specificity of the RT-RPA assay with dipstick
410 detection.

411

412 **3.5.** Exploration of point-of-care testing with the RT-RPA dipstick method

We investigated the potential of the RT-RPA assay for detection of SARS-CoV-2 at the point-of-care with the dipstick readout, a format that could dramatically widen access to testing in decentralised settings.

416 The tests could be read visually by eye. In addition, we developed a smartphone application 417 as a prototype towards a connected-diagnostic dipstick test. The architecture and screenshots 418 of the prototype application are presented in Fig. 4a. The smartphone application proposed allowed input and storage of patient's information, symptoms, capture of geo-location, test 419 420 lines intensity analysis of the dipstick and a record of the test results. If the test is "Positive" 421 or "Presumptive Positive" the user could insert the names of close contacts for contact tracing purposes. The application also included geographic visualisation of the tested patients to map 422 423 'hotspots'.

424

The major advantage of RPA, compared to other approaches such as PCR and LAMP, is its 425 426 isothermal amplification at ~37°C. We investigated the potential of different incubation 427 methods which could be more suitable for point-of-care settings. RT-RPA was performed to 428 detect 100 copies of RNA using four incubation approaches: an incubator, a water bath, a 429 disposable hand warmer bag and simply holding the tube in our hands. Incubators and water 430 baths are often found in well-equipped laboratories, but we also tried using a low-cost hand 431 warmer bag (based on an exothermic reaction shown to deliver a constant temperature of 432  $\sim$ 36-37°C for several hours (Wang, 2010)) and holding the tube in one hand (using body 433 temperature  $\sim$ 37°C) to show inexpensive and equipment-free alternatives. The results are 434 shown in Fig. 4b. While amplification in the incubator seemed to show the best results with 435 two test lines visible on the dipstick, two test lines were also visible for the reaction incubated 436 in the water bath, although slightly fainter. The reactions incubated on a hand warmer bag 437 and handheld appeared less sensitive, showing only a signal on test line (1). However, we

438 proved that very simple methods could be successfully used to amplify SARS-CoV-2 RNA
439 via RT-RPA and visual dipstick detection.

440

441 We investigated further the hand warmer bag as an affordable incubation method for RPA 442 reactions. We recorded the temperature on the bag surface and in the solution contained in 443 the PCR tube (Supplementary Fig. 7). We observed that the temperature on the bag surface falls within the RPA range (grey shaded area) after 15 minutes of air-activation and remained 444 445 in the right range for hours (at least 2 hours). Moreover, we showed the solution temperature 446 inside the tube (incubated on the flat hand warmer bag) reached the RPA temperature range. 447 To assess the cost-effectiveness of the assay, we estimated the cost of the reagents for the 448 RT-RPA assay (for both readouts) and compared them to two commercial kits for qRT-PCR 449 protocols (Supplementary Table S2). The RPA reagents cost between ~£4-5.7 which from 450 estimation was half the price of qRT-PCR reagents.

451

452 Finally, preliminary analysis was performed to assess the potential of the dipstick test to be 453 compatible with mock clinical samples, using human saliva with spiked RNA transcripts to mimic mouth swabs (Fig. 4c). Saliva is an easy specimen for self-collection that has been 454 455 FDA-approved for molecular testing of COVID-19 (U.S. Food and Drug Administration, 456 2020b). The E gene was clearly detectable on test line (1) with  $\geq$  1 RNA copy per reaction, 457 and a faint signal was seen on test line (2) for the RdRP gene with 1 and 100 RNA copies per reaction. Two strong test lines were visible for  $10^5$  copies per reaction. Therefore, the 458 459 findings of this small study suggest that conducting the assay in saliva compared to buffer did 460 not have a substantial impact on the assay sensitivity.

461

#### 462 Fig. 4 Exploration of point-of-care testing with the RT-RPA dipstick method.

#### 463 **4. Discussion**

Herein we report the development and evaluation of a rapid (20-30 minutes), multi-gene 464 molecular diagnostic for SARS-CoV-2 by RT-RPA. The test was presented with two 465 466 complementary detection methods: real-time fluorescence using a portable reader and visual dipstick readout on a low-cost nitrocellulose strip. The assay was optimised to just 1-2 steps, 467 468 allowing a fast time to result. The test showed high sensitivity and high specificity for both 469 readouts. The detection method by dipstick was further investigated for point-of-care and 470 decentralised testing using different incubation methods and a smartphone application to 471 capture, analyse and connect test results.

472

The development of the multiplex isothermal RT-RPA assay started by selecting two optimal
targets, in the E gene and RdRP gene, for rapid and ultrasensitive detection of SARS-CoV-2.
Detecting several targets in a multiplex test was done to increase the robustness of the assay,
especially to mitigate the risk of genetic variants escaping detection.

477

478 Isothermal fluorescence readers are usually available in centralised laboratories; however, 479 they are not necessarily found in decentralised laboratories and low-resource settings. For this 480 reason, we developed a second readout format, using a dipstick. Dipsticks are portable, cost-481 effective and user-friendly tools that can detect RPA amplicons with minimal equipment and 482 the test result can be seen with the naked eye. Here only a tube or microplate to mix the RT-RPA reaction with the buffer and a pipette to apply the mix on the dipstick was needed. A 483 484 disadvantage of this method may be the risk for environmental contamination due to the 485 transfer of post-amplification products to the dipstick. Giving the option of two alternative 486 readouts with their own advantages aimed to make molecular testing more widely accessible 487 and suitable for decentralised testing.

488 489 Incubation using an inexpensive hand warmer bag (~ \$0.5) showed less sensitivity, but 490 further characterisation of this method suggests that optimisation of the protocol could 491 improve performance in future. Notably, herein the bag was used 5-10 minutes after airactivation, while this demonstrated feasibility, it appeared the bag reached optimal RPA 492 493 temperature after 15-30 minutes. Additional work to optimise this incubation method will be 494 pursued as it showed it can provide suitable conditions for RPA reactions. It is a low-cost 495 incubation strategy which can be re-used over several hours. 496 We also showed that the assay was lower cost than qRT-PCR protocols, since it does not

497 require a sophisticated thermocycler and reagents cost less than some common qRT-PCR498 commercial kits.

499

500 The amplification time for the RT-RPA assay was set to run for 20 minutes since it was 501 sufficient to achieve single-copy detection of the E gene with real-time fluorescence and 502 visual dipstick readouts, showing the ultrasensitive potential of the test. High sensitivity is necessary to detect viral loads that are clinically relevant for COVID-19. The World Health 503 504 Organisation considers as acceptable an analytical sensitivity for confirmation of acute SARS-CoV-2 infection when equivalent to  $10^3$  genomic copies/mL (~50 copies per reaction) 505 506 (World Health Organization, 2020a). 507 The analytical sensitivities for the E and RdRP genes comparable with those reported by 508 Charité-Berlin for its qRT-PCR assay, which were 3.9 copy per reaction (95% CI: 2.8-9.8) 509 for the E gene and 3.6 copy per reaction (95% CI: 2.7-11.2) for the RdRP gene; in 510 comparison to 9.5 RNA copies per reaction (95% CI: 7.0-18) for the E gene and 17 RNA 511 copies per reaction (95% CI: 11-93) for the RdRP gene reported herein. Notably, the difference for the E gene is non-significant, with a 95% CI overlapping our reported mean. 512

513	Compared to PCR-based test, the point-of-care assay we developed herein could overcome
514	some of the inherent delays associated with shipping samples to centralised laboratories for
515	gold standard tests and waiting for test results.
516	Our RT-RPA assay was shown to be highly specific to SARS-CoV-2, with no observed
517	cross-reactivity with the closely related coronaviruses tested, such as SARS-CoV, MERS-
518	CoV, HCoV-NL63, HCoV-OC43 and HCoV-229E. This high specificity was demonstrated
519	for both detection methods and reduces the risk of false positives with closely related viruses
520	
521	The prototype smartphone application was proposed as a powerful tool for data capture,

522 analysis and visualisation when testing in decentralised settings. Smartphones are widely 523 accessible, easy-to-use and can act as a substitute to sophisticated laboratory equipment as 524 they integrate a high-resolution camera, large data storage space, real-time location and 525 connectivity.

526 Moreover, the use of inexpensive methods for incubation at ~37°C of the RT-RPA reaction 527 for detection on dipsticks, especially with a hand warmer bag, emphasises the simplicity of 528 the assay for resource limited settings.

529

#### 530 **5.** Conclusion

To close, we have developed an ultrasensitive and specific multi-gene diagnostic for SARS-CoV-2 viral RNA using isothermal RPA technology, and proposed two different detection methods, both showing high accuracy. While real-time fluorescence detection developed here offers more sensitivity and faster results (10 minutes faster than dipstick method), the proposed detection on dipsticks appeared as the preferred method for decentralised testing. We showed this method has the potential to meet the ASSURED and REASSURED criteria; it is affordable, rapid, has high analytical sensitivity and specificity, it is user-friendly and can

be performed with minimal equipment. We also proposed the addition of real-time

539 connectivity through a smartphone application and the potential use of saliva as a non-

540 invasive specimen. Having an alternative to qRT-PCR that has comparable analytical

541 performance, but with a shorter time to result, using different supply chains, requiring less

542 equipment and non-extensive laboratory experience, could help to alleviate the pressure on

543 healthcare systems and curb the COVID-19 pandemic worldwide.

544

545 Further test development will include clinical validation of the RT-RPA assay with clinical 546 samples with cross-validation of the developed assay with qRT-PCR results to determine the 547 clinical sensitivity and specificity of the test. In future, the adaptation of multiplexed gene 548 analysis, for example by including an S gene target could help track and discriminate new 549 variants of concern and the impact of COVID-19 vaccination programmes.

550

#### 551 **CRediT authorship contribution statement**

552 Dounia Cherkaoui: Conceptualisation, investigation, methodology, formal analysis,

553 application software, project administration, writing – original draft, writing – review &

654 editing. **Da Huang:** Conceptualisation, methodology, formal analysis, visualisation, project

administration, writing – review & editing. Benjamin S. Miller: Conceptualisation, software,

556 methodology, writing – review & editing. Valérian Turbé: Application software – review &

657 editing. Rachel A. McKendry: Conceptualisation, funding acquisition, supervision, writing

558 – review & editing

559

#### 560 **Declaration of competing interest**

561 Upon manuscript submission, all authors completed the declaration of competing interest and

562 they declared no competing interest.

563	
564	Ethics statement: Human saliva used as sample was purchased from a company and not
565	directly from patients, hence we believe no ethics statement or committee were needed for
566	this paper. The details of the sample, the company name and the catalogue number can be
567	found in the Material and Methods section of the manuscript.
568	
569	Acknowledgments
570	This research was funded by i-sense: EPSRC IRC in Agile Early Warning Sensing Systems
571	for Infectious Diseases and Antimicrobial Resistance (EP/R00529X/1) and associated
572	COVID-19 Plus Award. This research was also funded by EPSRC LCN studentship
573	(EP/N509577/1).
574	The authors would like to thank the European Virus Archive (EVAg) for providing the
575	coronavirus specificity panel free of charge. The authors thank Dr Eleanor Gray (LCN, UCL)
576	for her help with synthesis of the RNA standards. The authors would like to thank i-sense
577	Lab Manager Dr Diluka Peiris (LCN, UCL) for support in reagents and equipment
578	acquisition. The authors thank i-sense project managers Erin Manning and Jo McHugh (both
579	LCN, UCL) for support in communication and project management.
580	
581	Supplementary information
582	File: Supplementary Tables and Figures.docx
583	
584	
585	
586	
587	

### 588 **References**

- 589 Abbott. (2020). How ID NOW Tackles COVID-19. Retrieved September 16, 2020, from
- 590 https://www.abbott.com/corpnewsroom/diagnostics-testing/how-id-now-tackles-covid-
- 591 19.html
- 592 Arizti-Sanz, J., Freije, C. A., Stanton, A. C., Petros, B. A., Boehm, C. K., Siddiqui, S., ...
- 593 Myhrvold, C. (2020). Streamlined inactivation, amplification, and Cas13-based
- detection of SARS-CoV-2. *Nature Communications*, *11*(1), 1–9.
- 595 https://doi.org/10.1038/s41467-020-19097-x
- 596 Behrmann, O., Bachmann, I., Spiegel, M., Schramm, M., Abd El Wahed, A., Dobler, G., ...
- 597 Theodor Fontane, B. (2020). Rapid detection of SARS-CoV-2 by low volume real-time
- 598 single tube reverse transcription recombinase polymerase amplification using an exo
- 599 probe with an internally linked quencher (exo-IQ). *Clinical Chemistry*, 66(8), 1047–
- 600 1054. https://doi.org/10.1093/clinchem/hvaa116
- Brangel, P., Sobarzo, A., Parolo, C., Miller, B. S., Howes, P. D., Gelkop, S., ... Stevens, M.
- 602 M. (2018). A Serological Point-of-Care Test for the Detection of IgG Antibodies against
- 603 Ebola Virus in Human Survivors. *ACS Nano*, *12*(1), 63–73.
- 604 https://doi.org/10.1021/acsnano.7b07021
- Broughton, J. P., Deng, X., Yu, G., Fasching, C. L., Servellita, V., Singh, J., ... Chiu, C. Y.
- 606 (2020). CRISPR–Cas12-based detection of SARS-CoV-2. *Nature Biotechnology*, 38(7),
- 607 870–874. https://doi.org/10.1038/s41587-020-0513-4
- 608 Budd, J., Miller, B. S., Manning, E. M., Lampos, V., Zhuang, M., Edelstein, M., ...
- 609 McKendry, R. A. (2020). Digital technologies in the public-health response to COVID-
- 610 19. *Nature Medicine*, 26(8), 1183–1192. https://doi.org/10.1038/s41591-020-1011-4
- 611 Carlomagno, C., Bertazioli, D., Gualerzi, A., Picciolini, S., Banfi, P. I., Lax, A., ... Bedoni,
- 612 M. (2021). COVID-19 salivary Raman fingerprint: innovative approach for the detection

- of current and past SARS-CoV-2 infections. *Scientific Reports*, 11(1), 4943.
- 614 https://doi.org/10.1038/s41598-021-84565-3
- 615 Carrell, C., Kava, A., Nguyen, M., Menger, R., Munshi, Z., Call, Z., ... Henry, C. (2019).
- 616 Beyond the lateral flow assay: A review of paper-based microfluidics. *Microelectronic*
- 617 *Engineering*, 206, 45–54. https://doi.org/10.1016/j.mee.2018.12.002
- 618 Centers for Disease Control and Prevention. (2020). 2019-Novel Coronavirus (2019-nCoV)
- 619 *Real-time rRT-PCR Panel Primers and Probes.* Retrieved from
- 620 https://www.cdc.gov/coronavirus/2019-ncov/downloads/rt-pcr-panel-primer-probes.pdf
- 621 Chaibun, T., Puenpa, J., Ngamdee, T., Boonapatcharoen, N., Athamanolap, P., O'Mullane, A.
- 622 P., ... Lertanantawong, B. (2021). Rapid electrochemical detection of coronavirus
- 623 SARS-CoV-2. Nature Communications, 12(1), 802. https://doi.org/10.1038/s41467-021-
- 624 21121-7
- 625 Choi, J. R. (2020). Development of Point-of-Care Biosensors for COVID-19. *Frontiers in*
- 626 *Chemistry*, 8, 517. https://doi.org/10.3389/fchem.2020.00517
- 627 Choi, J. R., Hu, J., Tang, R., Gong, Y., Feng, S., Ren, H., ... Xu, F. (2016). An integrated
- 628 paper-based sample-to-answer biosensor for nucleic acid testing at the point of care. *Lab*
- 629 *Chip*, *16*(3), 611–621. https://doi.org/10.1039/C5LC01388G
- 630 Corman, V. M., Landt, O., Kaiser, M., Molenkamp, R., Meijer, A., Chu, D. K., ... Chantal,
- 631 R. (2020). Detection of 2019 novel coronavirus (2019-nCoV) by real-time RT-PCR.
- 632 *Eurosurveillance*, 25(3), 2000045. https://doi.org/10.2807/1560-
- 633 7917.ES.2020.25.3.2000045
- 634 Daher, R. K., Stewart, G., Boissinot, M., & Bergeron, M. G. (2016). Recombinase
- 635 Polymerase Amplification for Diagnostic Applications. *Clinical Chemistry*, 62(7), 947–
- 636 958. https://doi.org/10.1373/clinchem.2015.245829
- 637 Ding, X., Yin, K., Li, Z., Lalla, R. V., Ballesteros, E., Sfeir, M. M., & Liu, C. (2020).

- 638 Ultrasensitive and visual detection of SARS-CoV-2 using all-in-one dual CRISPR-
- 639 Cas12a assay. *Nature Communications*, 11(1), 1–10. https://doi.org/10.1038/s41467-

640 020-18575-6

- 641 El Wahed, A. A., Patel, P., Maier, M., Pietsch, C., Rüster, D., Böhlken-Fascher, S., ...
- 642 Weidmann, M. (2021). Suitcase Lab for Rapid Detection of SARS-CoV-2 Based on
- 643 Recombinase Polymerase Amplification Assay. Analytical Chemistry, 93(4), 2627–
- 644 2634. https://doi.org/10.1021/acs.analchem.0c04779
- 645 FIND. (2020). Testing is our first line of defence. Retrieved June 29, 2020, from
- 646 https://www.finddx.org/testing-matters/
- 647 Furukawa, N. W., Brooks, J. T., & Sobel, J. (2020). Evidence supporting transmission of
- 648 severe acute respiratory syndrome coronavirus 2 while presymptomatic or
- 649 asymptomatic. *Emerging Infectious Diseases*, 26(7).
- 650 https://doi.org/10.3201/eid2607.201595
- 651 Gorbalenya, A. E., Baker, S. C., Baric, R. S., de Groot, R. J., Drosten, C., Gulyaeva, A. A.,
- 652 ... Ziebuhr, J. (2020). The species Severe acute respiratory syndrome-related
- 653 coronavirus: classifying 2019-nCoV and naming it SARS-CoV-2. *Nature Microbiology*,
- 654 5(4), 536. https://doi.org/10.1038/s41564-020-0695-z
- 655 GOV.UK. (2020). UK reaches 200,000 coronavirus testing capacity target a day early -
- 656 GOV.UK. Retrieved September 10, 2020, from
- 657 https://www.gov.uk/government/news/uk-reaches-200000-coronavirus-testing-capacity-
- 658 target-a-day-early
- 659 Guglielmi, G. (2020). Fast coronavirus tests: what they can and can't do. *Nature*, 585(7826),
- 660 496–498. https://doi.org/10.1038/d41586-020-02661-2
- Holstein, C. A., Griffin, M., Hong, J., & Sampson, P. D. (2015). Statistical Method for
- 662 Determining and Comparing Limits of Detection of Bioassays. Anal. Chem, 87(19),

663 9795–9801. https://doi.org/10.1021/acs.analchem.5b02082

- Lau, Y. L., Ismail, I. binti, Mustapa, N. I. binti, Lai, M. Y., Tuan Soh, T. S., Haji Hassan, A.,
- 665 ... Goh, P. P. (2021). Development of a reverse transcription recombinase polymerase
- amplification assay for rapid and direct visual detection of Severe Acute Respiratory
- 667 Syndrome Coronavirus 2 (SARS-CoV-2). *PLoS ONE*, *16*(1), e0245164.
- 668 https://doi.org/10.1371/journal.pone.0245164
- Mabey, D., Peeling, R. W., Ustianowski, A., & Perkins, M. D. (2004). Diagnostics for the
  developing world. *Nature Reviews Microbiology*, 2(3), 231–240.
- 671 https://doi.org/10.1038/nrmicro841
- Miller, B. S., Bezinge, L., Gliddon, H. D., Huang, D., Dold, G., Gray, E. R., ... McKendry,
- 673 R. A. (2020). Spin-enhanced nanodiamond biosensing for ultrasensitive diagnostics.

674 *Nature*, 587(7835), 588–593. https://doi.org/10.1038/s41586-020-2917-1

- 675 Mori, Y., & Notomi, T. (2009). Loop-mediated isothermal amplification (LAMP): a rapid,
- 676 accurate, and cost-effective diagnostic method for infectious diseases. *Journal of*
- 677 *Infection and Chemotherapy*, *15*(2), 62–69. https://doi.org/10.1007/s10156-009-0669-9
- 678 National Institute for Viral Disease Control and Prevention. (2020). Specific primers and
- probes for detection of 2019 novel coronavirus. Retrieved August 25, 2020, from
- 680 http://ivdc.chinacdc.cn/kyjz/202001/t20200121\_211337.html
- 681 Patchsung, M., Jantarug, K., Pattama, A., Aphicho, K., Suraritdechachai, S., Meesawat, P.,
- 682 ... Uttamapinant, C. (2020). Clinical validation of a Cas13-based assay for the detection
- 683 of SARS-CoV-2 RNA. *Nature Biomedical Engineering*, *4*(12), 1140–1149.
- 684 https://doi.org/10.1038/s41551-020-00603-x
- 685 Peñarrubia, L., Ruiz, M., Porco, R., Rao, S. N., Juanola-Falgarona, M., Manissero, D., ...
- 686 Pareja, J. (2020). Multiple assays in a real-time RT-PCR SARS-CoV-2 panel can
- 687 mitigate the risk of loss of sensitivity by new genomic variants during the COVID-19

- 688 outbreak. International Journal of Infectious Diseases, 97, 225–229.
- 689 https://doi.org/10.1016/j.ijid.2020.06.027
- 690 Public Health England. (2020). Investigation of novel SARS-COV-2 variant Variant of
- 691 *Concern 202012/01*. Retrieved from
- 692 https://assets.publishing.service.gov.uk/government/uploads/system/uploads/attachment
- 694 Qian, J., Boswell, S. A., Chidley, C., Lu, Z., Pettit, M. E., Gaudio, B. L., ... Springer, M.
- 695 (2020). An enhanced isothermal amplification assay for viral detection. *Nature*
- 696 *Communications*, 11(1), 5920. https://doi.org/10.1038/s41467-020-19258-y
- 697 Rodriguez, N. M., Wong, W. S., Liu, L., Dewar, R., & Klapperich, C. M. (2016). A fully
- 698 integrated paperfluidic molecular diagnostic chip for the extraction, amplification, and
- 699 detection of nucleic acids from clinical samples. *Lab on a Chip*, *16*(4), 753–763.
- 700 https://doi.org/10.1039/C5LC01392E
- 701 Sheridan, C. (2020). COVID-19 spurs wave of innovative diagnostics. *Nature Biotechnology*,
- 702 *38*(7), 769–772. https://doi.org/10.1038/s41587-020-0597-x
- 703 Simoska, O., & Stevenson, K. J. (2019). Electrochemical sensors for rapid diagnosis of
- 704 pathogens in real time. *Analyst*, *144*(22), 6461–6478.
- 705 https://doi.org/10.1039/C9AN01747J
- 706 U.S. Food and Drug Administration. (2020a). Coronavirus (COVID-19) Update: FDA
- 707 Authorizes First COVID-19 Test for Self-Testing at Home. Retrieved November 18,
- 708 2020, from https://www.fda.gov/news-events/press-announcements/coronavirus-covid-
- 709 19-update-fda-authorizes-first-covid-19-test-self-testing-home
- 710 U.S. Food and Drug Administration. (2020b). Coronavirus (COVID-19) Update: FDA
- 711 Authorizes First Diagnostic Test Using At-Home Collection of Saliva Specimens.
- 712 Retrieved October 15, 2020, from https://www.fda.gov/news-events/press-

- 713 announcements/coronavirus-covid-19-update-fda-authorizes-first-diagnostic-test-using-
- 714 home-collection-saliva
- 715 University of Liverpool. (2020). Liverpool COVID-19 Community Testing Pilot. Interim
- evaluation report, 23 December 2020. Retrieved April 22, 2021, from
- 717 https://www.liverpool.ac.uk/media/livacuk/coronavirus/Liverpool,Community,Testing,P
- 718 ilot,Interim,Evaluation.pdf
- 719 Vandenberg, O., Martiny, D., Rochas, O., van Belkum, A., & Kozlakidis, Z. (2020).
- 720 Considerations for diagnostic COVID-19 tests. *Nature Reviews Microbiology*, 1–13.
- 721 https://doi.org/10.1038/s41579-020-00461-z
- Wang, L. (2010). What's inside disposable hand warmers? *Chemical and Engineering News*.
- 723 Retrieved from https://cen.acs.org/articles/88/i4/Hand-Warmers.html
- WHO. (2020). Laboratory testing for coronavirus disease 2019 (COVID-19) in suspected
- human cases, (March), 1–7. Retrieved from https://www.who.int/publications-
- 726 detail/laboratory-testing-for-2019-novel-coronavirus-in-suspected-human-cases-
- 727 20200117
- 728 Wood, C. S., Thomas, M. R., Budd, J., Mashamba-Thompson, T. P., Herbst, K., Pillay, D.,
- 729 ... Stevens, M. M. (2019). Taking Mobile Health Connected Infectious Disease
- 730 Diagnostics to the Field. *Nature*, *566*(7745), 467–474. https://doi.org/10.1038/s41586-
- 731 019-0956-2
- 732 World Health Organization. (2020a). COVID-19 Target product profiles for priority
- diagnostics to support response to the COVID-19 pandemic v.1.0. Retrieved January 23,
- 734 2021, from https://www.who.int/publications/m/item/covid-19-target-product-profiles-
- for-priority-diagnostics-to-support-response-to-the-covid-19-pandemic-v.0.1
- World Health Organization. (2020b). Laboratory testing of 2019 novel coronavirus (2019-
- nCoV) in suspected human cases: interim guidance, 17 January 2020. Retrieved August

- 738 25, 2020, from https://www.who.int/publications/i/item/laboratory-testing-of-2019-
- novel-coronavirus-(-2019-ncov)-in-suspected-human-cases-interim-guidance-17-

740 january-2020

- 741 World Health Organization. (2020c). WHO Director-General's opening remarks at the media
- briefing on COVID-19 13 April 2020. Retrieved June 29, 2020, from
- 743 https://www.who.int/dg/speeches/detail/who-director-general-s-opening-remarks-at-the-
- 744 media-briefing-on-covid-19--13-april-2020
- 745 World Health Organization. (2020d). WHO Director-General's remarks at the media briefing
- on 2019-nCoV on 11 February 2020. Retrieved August 25, 2020, from
- 747 https://www.who.int/dg/speeches/detail/who-director-general-s-remarks-at-the-media-
- 748 briefing-on-2019-ncov-on-11-february-2020
- 749 World Health Organization. (2021). WHO Coronavirus Disease (COVID-19) Dashboard.
- 750 Retrieved from https://covid19.who.int
- 751 Wu, F., Zhao, S., Yu, B., Chen, Y.-M., Wang, W., Song, Z.-G., ... Zhang, Y.-Z. (2020). A
- new coronavirus associated with human respiratory disease in China. *Nature*, *579*(7798),
  265–269.
- Xia, S., & Chen, X. (2020). Single-copy sensitive, field-deployable, and simultaneous dual-
- gene detection of SARS-CoV-2 RNA via modified RT–RPA. *Cell Discovery*, 6(1), 1–4.
- 756 https://doi.org/10.1038/s41421-020-0175-x
- 757 Xue, G., Li, S., Zhang, W., Du, B., Cui, J., Yan, C., ... Yuan, J. (2020). Reverse-
- 758 Transcription Recombinase-Aided Amplification Assay for Rapid Detection of the 2019
- 759 Novel Coronavirus (SARS-CoV-2). *Analytical Chemistry*, 92(14), 9699–9705.
- 760 https://doi.org/10.1021/acs.analchem.0c01032
- 761 Yousefi, H., Mahmud, A., Chang, D., Das, J., Gomis, S., Chen, J. B., ... Kelley, S. O. (2021).
- 762 Detection of SARS-CoV-2 Viral Particles Using Direct, Reagent-Free Electrochemical

- 763 Sensing. Journal of the American Chemical Society, 143(4), 1722–1727.
- 764 https://doi.org/10.1021/jacs.0c10810

765

Journal Pression

### 1 Figure captions

- 2
- <sup>3</sup> Harnessing recombinase polymerase amplification for
- 4 rapid detection of SARS-CoV-2 in resource-limited

### 5 settings

- 6 Dounia Cherkaoui<sup>a,b,1</sup>, Da Huang<sup>a,1</sup>, Benjamin S. Miller<sup>a</sup> & Rachel A. McKendry<sup>a,b</sup>\*
- <sup>a</sup> London Centre for Nanotechnology, University College London, London, United Kingdom
- 8 <sup>b</sup> Division of Medicine, University College London, London, United Kingdom
- 9
- <sup>1</sup>These authors contributed equally to this work.
- 11 \* Corresponding author
- 12 Name: Professor Rachel McKendry
- 13 Address: London Centre for Nanotechnology, University College London, 19 Gordon Street,
- 14 London, United Kingdom
- 15 E-mail: <u>r.a.mckendry@ucl.ac.uk</u>
- 16 Telephone number: +44 (0)20 7679 9995

#### 17 Fig. 1 Schematic representation of the rapid and multiplex RT-RPA assay with real-

#### 18 time fluorescence and dipstick detection.

a One-pot RT-RPA assay including reverse transcription of the viral RNA and amplification
by RPA at constant temperature (37-39°C). b Sequences of the primers/probe sets used for
SARS-CoV-2 E gene and RdRP gene in the multiplex RT-RPA assay with real-time
detection (blue) and sequences of the modified primers used for the multiplex dipstick
detection (orange). c Real-time fluorescence detection by exonuclease cleavage of the probes
for E gene and RdRP gene at their THF residue. d Design of the dipstick for multiplexed
detection of the E gene and the RdRP gene.

## Fig. 2 Evaluation of the sensitivity and specificity of the RT-RPA assay with real-time fluorescence detection.

29 a Time to threshold for positive RT-RPA reactions with real-time fluorescence detection. The 30 dots represent individual values for the positive reactions reaching threshold for the E gene 31 (in green) and for the RdRP gene (in orange). The bars represent the average time to 32 threshold for the positive reactions and the error bars represent the standard deviation. Each 33 RNA concentration was run in five replicates (N=5), only the positive reactions are 34 represented. **b** Probit analysis for the E gene (left, green) and RdRP gene (right, orange) with 35 their 95% confidence interval (CI). The fraction positive was determined from the RT-RPA 36 reactions in **a** and the probit analysis was done to find the effective concentration at 95% 37  $(EC_{95})$  for both genes. c Validation of the specificity of the E gene primers/probe set against 38 SARS-CoV, MERS-CoV (top) and the seasonal coronaviruses (bottom). d Validation of the 39 specificity of the RdRP gene primers/probe set against SARS-CoV, MERS-CoV (top) and the 40 seasonal coronaviruses (bottom). NTC: non-template control.

## Fig. 3 Evaluation of the sensitivity and specificity of the RT-RPA assay with dipstick

#### 43 detection.

42

44 a Evaluation of the sensitivity of the RT-RPA with multiplex dipstick detection. Captures of 45 the dipsticks run with a range of RNA inputs are shown with the associated test line intensity 46 analysis. Dipsticks were annotated (- -) if no test line was visible ("Negative"), (+ -) or (- +) 47 if only one test line was visible ("Presumptive positive") and (++) if both test lines (1) and (2) were visible ("Positive"). One representative dipstick capture is shown here. **b** Probit 48 49 analysis and determination of the  $EC_{95}$  for the dipstick detection method (taking both genes 50 into account) with the 95% confidence interval (CI). The fraction positive was determined 51 from six replicates (N=6) RT-RPA reactions. c Specificity of the dipstick detection method 52 against SARS-CoV, MERS-CoV (left) and the seasonal coronaviruses (right). Photographs of the dipsticks are shown (top) with the associated test line intensity analysis (bottom). NTC: 53 54 non-template control.

55

#### 56 Fig. 4 Exploration of point-of-care testing with the RT-RPA dipstick method.

57 a Architecture of the prototype smartphone application "CovidApp". The design of the 58 smartphone application is represented along with screenshots of the different activities of the 59 application. The main activities, including "Homepage", "Test", "Contact", "Alerts" and "Map Outbreak" are described. b Comparison of incubation of four methods for RT-RPA at 60 61  $\sim$ 37°C with dipstick readout, including incubation using a traditional laboratory incubator 62 with shaking, water bath, hand warmer bag and handheld (using body temperature) 63 (photographs on the top). The lateral flow test captures are shown (middle) with the 64 associated test line intensity analysis (bottom). c Detection of RT-RPA reactions with mock 65 clinical samples (saliva spiked with RNA). Photographs of the lateral flow test captures are shown (top) with the associated test line intensity analysis (bottom). b and c dipsticks were 66

- 67 annotated (- -) if no test line was visible ("Negative"), (+ -) or (- +) if only one test line was
- 68 visible ("Presumptive positive") and (++) if both test lines (1) and (2) were visible
- 69 ("Positive"). NTC: non-template control; PC: positive control (100 copies RNA/reaction).











Highlights:

- Rapid nucleic acid testing of SARS-CoV-2 simultaneously targeting multiple genes •
- Isothermal amplification by RT-RPA using two complementary readouts •
- Simple and equipment-free incubation methods for point-of-care application •
- Towards a smartphone-connected dipstick test for decentralised testing •

at