

RESEARCH ARTICLE

Methacrylate peak determination and selection recommendations using ATR-FTIR to investigate polymerisation of dental methacrylate mixtures

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Abstract

Investigation of polymerisation kinetics using ATR-FTIR systems is common in many dental studies. However, peak selection methods to calculate monomer-polymer conversion can vary, consequently affecting final results. Thus, the aim of this study is to experimentally confirm which method is less prone to systematic errors. Three commercial restorative materials were tested—Vertise Flow (VF), Constic and Activa Bioactive Restorative Kids. Firstly, Attenuated Total Reflectance Fourier Transform Infra-Red (ATR-FTIR) (Spectrum One, Perkin-Elmer, UK) spectra of monomers were acquired—10-methacryloyloxy decyl dihydrogen phosphate (10-MDP), bisphenol-A glycidyl dimethacrylate (Bis-GMA), 2-hydroxyethyl methacrylate (HEMA), triethelene glycol dimethacrylate (TEGDMA) and urethane dimethacrylate (UDMA) to investigate proportionality of methacrylate peak heights versus concentration. Spectral changes upon light exposure of 2 mm discs of the restorative materials (irradiated for 20 s, LED curing unit 1100–1330 mW/cm²) were assessed to study polymerisation kinetics ($n = 3$), with continuous acquisition of spectra, before, during and after light exposure. Peak differences and degrees of conversion (D_C %) were calculated using 1320/1336, 1320/1350 and 1636/1648 cm⁻¹ as reaction/reference peaks. Inferential statistics included a MANOVA and within-subjects repeated measures ANOVA design (5% significance level). Proportionality of methacrylate peak height to concentration was confirmed, with the 1320/1352 cm⁻¹ peak combination showing the lowest coefficient of variation (8%). Difference spectra of the polymerisation reaction showed noise interference around the 1500–1800 cm⁻¹ region. Across the different materials, D_C % results are highly dependent upon peak selection ($p < 0.001$), with higher variability associated to the 1636 cm⁻¹. Significant differences in the materials were only detected when the 1320 cm⁻¹ peak was used ($p < 0.05$). Within the same materials, methods were significantly different for Constic and Activa ($p < 0.05$). It is possible to conclude that the 1320 cm⁻¹ peak is more adequate to assess polymerisation of methacrylates and is therefore recommended.

OPEN ACCESS

Citation: Delgado AHS, Young AM (2021) Methacrylate peak determination and selection recommendations using ATR-FTIR to investigate polymerisation of dental methacrylate mixtures. PLoS ONE 16(6): e0252999. <https://doi.org/10.1371/journal.pone.0252999>

Editor: Parag A. Deshpande, Indian Institute of Technology Kharagpur, INDIA

Received: February 18, 2021

Accepted: May 26, 2021

Published: June 9, 2021

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Data Availability Statement: All relevant data are within the paper and its [Supporting Information](#) files.

Funding: A.D. thanks Fundação para a Ciência e Tecnologia (FCT), Portugal for the PhD Grant SFRH/BD/136406/2018 which supported this research.

Competing interests: The authors have declared that no competing interests exist.

Introduction

Fourier Transform Infra-Red Spectroscopy (FTIR) is able to quantify infra-red light absorbance and transmittance, resulting from changes in the dipole moment of bonds in molecules, which display vibrational patterns [1]. It is a technique widely used for material characterization, namely organic materials such as polymers, with high applicability in many different fields [2, 3]. In dentistry specifically, it is understood as a reference technique for the study of polymerisation kinetics of dental materials, especially useful when coupled with Attenuated Total Reflectance (ATR) accessories, as recognized by the Academy of Dental Materials [4].

Resin composites, a universally used restorative material in dentistry, are made of an organic resin phase of methacrylate derivatives (such as Bisphenol-A glycidyl dimethacrylate–Bis-GMA, triethylene glycol dimethacrylate–TEGDMA or urethane dimethacrylate–UDMA), combined with a filler phase of glass particles and a photoinitiator system [5]. Typically, free-radical addition polymerisation reactions in these materials are activated by blue light, and they can be monitored using real-time ATR-FTIR systems [6]. Over the past years, several studies across the dental literature have successfully measured the degree of conversion (D_C %) of methacrylate monomer bond changes, using such technique [7–10]. Methacrylate polymerisation monitoring is researched not only with resin composites but also with other dental materials containing resin monomers, such as dental adhesive systems, resin-modified glass ionomers and compomers [11–14].

To calculate this parameter, in most studies, the ratio between the reactionary methacrylate 1640 cm^{-1} [$\nu(\text{C}=\text{C})$] and the 1610 cm^{-1} [$\nu(\text{C}=\text{C})$] peak as the internal standard reference, are used in Bis-GMA mixtures. However, as O-H bending vibrations absorb in the same region, and spectral contributions of carbonyl groups may affect the 1640 cm^{-1} peak, alternative peak selections are recommended [15]. The 1320 cm^{-1} [$\nu(\text{C}-\text{O})$] has been successfully employed for the study of polymerisation in dental composites and has been preferred over the 1640 cm^{-1} peak in a number of cases [9, 11, 16]. Despite having some studies acknowledge the variability regarding peak selection, the 1320 cm^{-1} peak is still underappreciated [17]. Repeatability of the ATR-FTIR technique also demands investigation, as it is important in confirming its ability to detect small changes within sample repetitions or between different time points, in scenarios such as reactions or material aging [18, 19].

To measure D_C % in light-curable materials, other direct measuring techniques have been used in past studies, such as Raman spectroscopy [15]. Raman shows comparable results to FTIR in resin composites [20], but it is seldom used to acquire continuous spectra which are useful for the study of the evolution of the polymerisation reaction and its kinetics. It may also be time consuming, due to Raman scattering being a weak effect, with signal strength issues, leading to a steeper learning curve [21]. ATR-FTIR sample preparation and method is a simple, rapid and easy access tool that allows spectra to be acquired before, during and after light curing, allowing the operator to cure *in situ* without interfering with the measurement [13]. ATR-FTIR has also been proven convenient to study setting kinetics in glass ionomer cements, calcium silicates and bone cements [11, 12, 22, 23].

The aim is then to assess whether final D_C (%) is dependent upon peak selection method, by investigating which peak choices are less prone to systematic errors, shedding light on which method should be used to determine D_C (%) in polymerisation of methacrylates.

Materials and methods

Raw spectral acquisition

Individual monomers 10-methacryloyloxydecyl dihydrogen phosphate (10-MDP, DMHealth-care, San Diego, CA, USA, code P01030), 2-hydroxyethyl methacrylate HEMA (DMG,

Hamburg, Germany code 11220), Bis-GMA (Polysciences, Warrington, PA, USA, code 03344), UDMA (DMG, Hamburg, Germany, code 100112) and TEGDMA (DMG, Hamburg, Germany, code 100102) were purchased for FTIR spectral acquisition, using a diamond ATR accessory (Golden Gate ATR, Specac Ltd., Orpington, UK) attached to a FTIR spectrometer (Spectrum One, Perkin-Elmer, MA, USA). All spectra were acquired from 700–4000 cm^{-1} at a resolution of 4 cm^{-1} . Spectrum TimeBase v. 3.1.4 (Perkin-Elmer, MA, USA) was used for data processing.

ChemBioDraw Pro v.19.1 (Perkin-Elmer, MA, USA) was used to draw the chemical structure of each monomer for peak assignments and interpretation.

In order to confirm methacrylate peak heights are proportional to the concentration of methacrylate groups in each monomer, an equation relating to the moles of monomer per unit volume was used,

$$\frac{P_r - P_b}{\left(\frac{N_{meth} \times \rho}{M_w}\right)} \quad (1)$$

where P_r represents the peak height of the reaction peak, and P_b represents the peak height of the baseline peak, in absorbance units. N_{meth} represents the number of methacrylate groups in the monomer, ρ represents the density (g/cc), while M_w represents the molecular weight (g/mol).

Polymerisation kinetics using ATR-FTIR

Three different restorative materials were tested in this study. Two metal circlips (1 mm thickness x 10 mm internal diameter) were used to contain resin composite samples of 2 mm thickness, total, of each material ($n = 3$)—Vertise Flow (VF) (Kerr/KaVo, Orange, Ca, USA), Constic (DMG, Hanau, Germany) and Activa Bioactive Restorative Kids (Pulpdent, Watertown, MA, USA) (Table 1). Each material was dispensed into the circlips, which were on an ATR (Specac Ltd., UK) diamond crystal plate. An acetate sheet was placed on top of the circlips, and a glass slide was used to apply pressure to the material. The top surface of the material was irradiated with a single emission peak light emitting diode (LED) light curing unit (LCU) (Demi Plus, Kerr, Orange, CA, USA) with a power output between 1100 mW/cm^2 –1330 mW/cm^2 , and spectral emission ranging from 450 to 470 nm. FTIR spectra were obtained before, during and after 20 s of light exposure, for a total time period of 1200 s, originating an average of 193 spectra for each repetition. These were acquired over a wavenumber range of 700 to 4000 cm^{-1} at a resolution of 4 cm^{-1} , at 37°C. The light curing began 20 ± 5 s after placement of the material and the start of the spectral acquisition.

Table 1. Material composition for commercial restorative materials used in this study.

MATERIAL	TYPE	COMPOSITION	
Vertise™ Flow (Kerr, USA) VF	Flowable resin composite	5–10% HEMA, N/A% Bis-GMA, 5–10% UDMA and 1–5% GPDM	Ytterbium fluoride and barium aluminosilicate (66 wt%)
Constic (DMG, GER)	Flowable resin composite	15–35% Bis-GMA, <45% TEGDMA and N/A% 10-MDP	Barium aluminosilicate
Activa™ Kids (Pulpdent, USA)	Resin modified glass ionomer	44.6% blend of UDMA and other methacrylates with modified polyacrylic acid	Sodium fluoride and silica (56 wt%)

10-MDP: 10-methacryloyloxy decyl dihydrogen phosphate; Bis-GMA: Bisphenol-A glycidyl dimethacrylate; GPDM: glycerophosphate dimethacrylate; HEMA: 2-hydroxyethyl methacrylate; TEGDMA: triethylene glycol dimethacrylate; UDMA: urethane dimethacrylate.

<https://doi.org/10.1371/journal.pone.0252999.t001>

To calculate the D_C (%), the following equation was used (2), where (h_0) and (h_t) represent the height of a reactionary methacrylate peak above baseline (reference peak), initially and at time, t , after start of polymerisation respectively.

$$D_C = \frac{100(h_0 - h_t)}{h_0} \quad (2)$$

For this study, different reaction peaks and bases were selected, to test their effect on determining conversions, and to look at the variability of the data.

- 1320 cm^{-1} [v(C-O)] with 1336 cm^{-1} as baseline
- 1320 cm^{-1} [v(C-O)] with 1350 cm^{-1} as baseline
- 1636 cm^{-1} [v(C = C)] with 1650 cm^{-1} as baseline

A continuous spectral acquisition during polymerisation, without disconnection from the ATR diamond, allows for the continuous monitoring of the exact same material volume during polymerisation. Normalisation by a reference peak is thus not needed.

To investigate spectral changes between the initial and the final time point, while spectra were continuously being acquired, the difference between the final and the initial spectra were taken and studied for the repetitions of the three different materials. To collect and analyse the resulting spectra, a spectral treatment software was used—Spectrum TimeBase (v.3.1.4, Perkin-Elmer, MA, USA). This allowed calculation of the ratio of intensity, on the ATR diamond, obtained with versus without the sample and posterior conversion. Of the data to absorbance versus wavenumber (cm^{-1}).

The reaction extent was calculated using the following Eq (3), for the 1320 cm^{-1} reaction peak, without baseline subtraction

$$\zeta = \frac{(A_i - A_t)}{(A_i - A_f)} \quad (3)$$

where A is the absorbance of the 1320 cm^{-1} peak without baseline subtraction; i , t and f indicate initial, at time t and final absorbance (determined by extrapolation of absorbance versus inverse time to zero), respectively.

Statistical analysis

To ensure sufficient sample size, an a priori test of the difference of means of K independent groups, using a one-way ANOVA design, was conducted with statistical software G*Power v.3.1.9.6 for Mac (HHU Düsseldorf, Germany). An alpha of **0.05** was used, with a total sample size of **9** ($n = 3$ for 3 groups), yielding >95% power to detect differences. To assess peak changes, across the repetitions of each sample, mean band maxima of the peaks described above, and standard deviations were calculated for the initial and final spectra. Statistical software package Statistical Package for the Social Sciences—SPSS v. 26.0 (IBM Corporation, Armonk, NY, USA) was used for hypothesis testing. A multivariate analysis of variance (MANOVA) design was employed to compare final D_C (%) between different materials, across three independent peak determination methods, while a within-subjects design repeated measures ANOVA was used to compare different peak determination methods within the same materials. Games-Howell post-hoc test was used for the MANOVA, while a Bonferroni multiple comparison post-hoc was used for the repeated measures ANOVA. Assumptions were checked prior to both analyses of variance designs. All inferential analyses were conducted using a significance level of 5%.

Results

The chemical structure and corresponding FTIR spectra of the individual monomers, with methacrylate peak assignments, used in the chemical composition of the materials that were tested (Table 1) are given in Fig 1.

Assigned methacrylate peak heights for the individual monomers and respective bases are given in Table 2. The 1320 cm^{-1} [v(C-O)] peak, when used as the reaction peak, with the appropriate base, gives results with lower coefficient of variation (CV%), in estimating proportional level of monomer concentration, when compared to the 1636 cm^{-1} peak, showing enhanced repeatability.

FTIR spectra of each restorative material, before and after photopolymerisation, are shown in Fig 2. Spectra of VF and Constic are compatible with the presence of Bis-GMA as a main

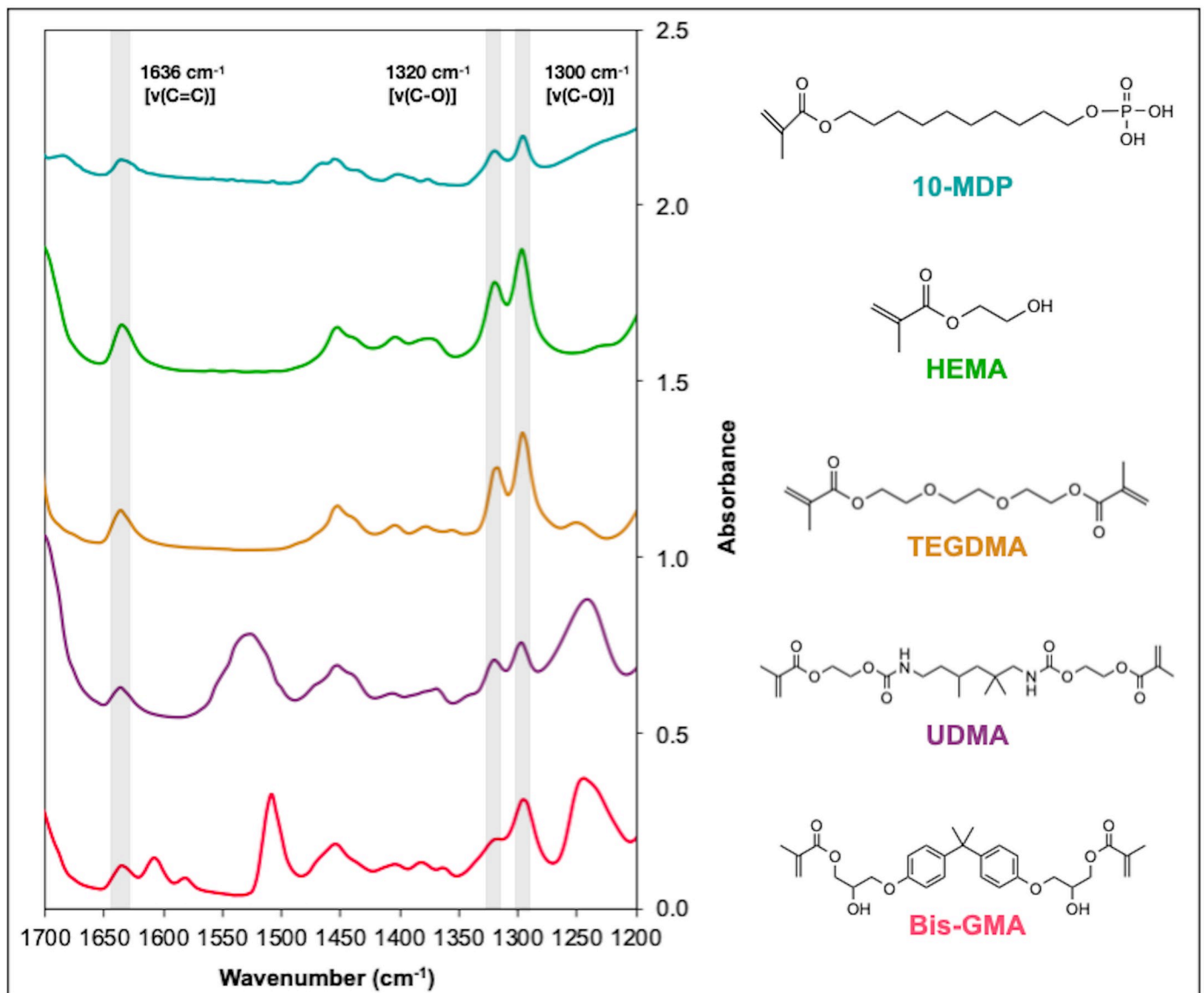


Fig 1. FTIR spectra and chemical structure of dimethacrylates Bis-GMA, UDMA, TEGDMA and monomethacrylates HEMA and 10-MDP. C-O stretch doublet can be seen at 1300 and 1320 cm^{-1} together with 1636 [v(C=C)] bond.

<https://doi.org/10.1371/journal.pone.0252999.g001>

Table 2. Peak absorbance of individual monomers (Part I), from the spectra acquired and peak height per mole per cc, derived using Eq (1) (Part II), for the different reaction peaks and peak bases.

Part I		Absorbance					
Peak wavenumber (cm ⁻¹)	10-MDP	HEMA	TEGDMA	UDMA	Bis-GMA		
Reaction 1320	0.15	0.28	0.25	0.21	0.20		
Baseline 1336	0.08	0.10	0.07	0.11	0.14		
Baseline 1352	0.06	0.07	0.07	0.09	0.10		
Reaction 1636	0.13	0.16	0.13	0.13	0.13		
Baseline 1648	0.09	0.06	0.05	0.08	0.07		
Part II		10-MDP	HEMA	TEGDMA	UDMA	Bis-GMA	
Peak/base employed	Peak height derived with Eq 1 (mole ⁻¹ cc ⁻¹)					Mean (SD) [CV%]	
1320–1336	21	21	23	20	14	20 (3.5) [18%]	
1320–1352	27	25	23	25	23	25 (2.0) [8%]	
1636–1648	12	14	10	10	13	12 (1.3) [11%]	

<https://doi.org/10.1371/journal.pone.0252999.t002>

monomer, with a distinct 1610 aromatic [$\nu(\text{C}=\text{C})$] peak, while Activa shows a dominant UDMA spectra with distinct contributions at 1535 cm⁻¹ [$\delta(\text{N-H})$] and 1240 cm⁻¹.

From Fig 2, it is also possible to confirm that the absorbance changes seen in the final spectra are very similar between the three materials, with shifts in the same regions, showing that major changes are due to methacrylate polymerisation. Taking the difference spectra between the initial and final spectrum revealed again changes associated with polymerisation, shown with all the materials in Fig 3. Additionally, the presence of noise in the 1000–1100 and 1500–1800 cm⁻¹ regions due to high glass filler content and background water vapour absorbance, respectively, could be detected in some samples. However, no noise was observed between these wavenumber regions.

Peak height differences, respective errors and D_C (%) for each material and method are given in Table 3. Final D_C (%) means and standard deviations are dependent upon the method chosen, with a statistically significant difference among the groups on a linear combination of the three dependent variables (MANOVA, $p < 0.001$, $\eta^2 > 0.99$). Material differences in respect to conversion are seen with the first two methods, whereas with the last method, conversions are not significantly different (Games-Howell post-hoc, $p > 0.05$). With the 1320–1336 cm⁻¹ method, VF is significantly different to Constic ($p = 0.008$) and to Activa ($p = 0.002$), while Constic was also

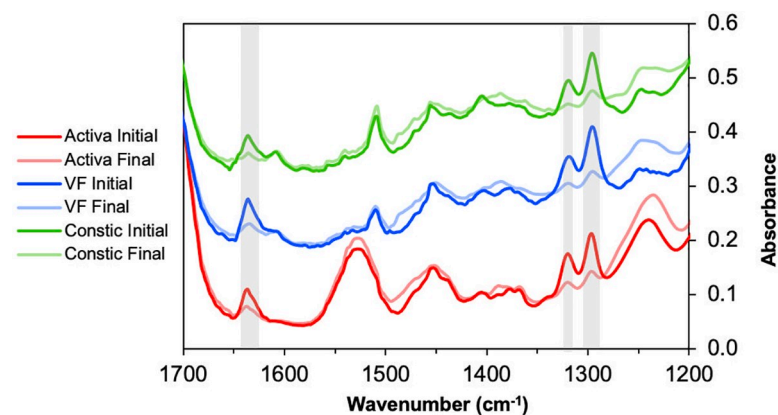


Fig 2. FTIR spectra of VF, Constic and Activa, initial and final (1200 s) spectra. Absorbance changes due to polymerisation can be seen at the C-O stretch doublet at 1300 and 1320 cm⁻¹ together with 1636 [$\nu(\text{C}=\text{C})$] bond, highlighted in grey. Samples with 2 mm thickness, light cured for 20 s ($n = 3$).

<https://doi.org/10.1371/journal.pone.0252999.g002>

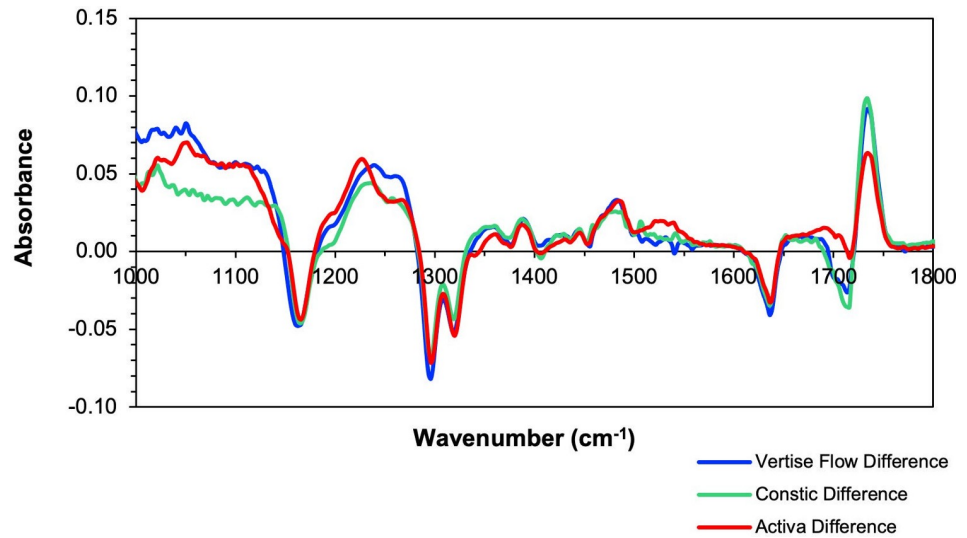


Fig 3. FTIR difference spectra (initial-final spectrum). Graph shows peak shifts owing to the polymerisation reaction. Absorbance changes are seen in the 1160 cm^{-1} [$\nu(\text{C}-\text{O}-\text{C})$], $1300\text{--}1320$ [$\nu(\text{C}-\text{O})$] which shift to lower wavenumbers, at 1230 and 1268 cm^{-1} , and absorbance change of [$\nu(\text{C}=\text{C})$] at 1640 cm^{-1} . Spectra also show noise around the $1500\text{--}1800\text{ cm}^{-1}$ region, with a smooth region between $1100\text{--}1500\text{ cm}^{-1}$.

<https://doi.org/10.1371/journal.pone.0252999.g003>

significantly different to Activa ($p = 0.001$). Considering the $1320\text{--}1350\text{ cm}^{-1}$ method, VF was significantly different to Constic ($p = 0.035$) and Activa ($p = 0.015$). Constic was also significantly different to Activa ($p < 0.001$). D_C (%) results show higher variability when the 1636 cm^{-1} peak is chosen, with higher standard deviations and coefficients of variation, compared to selecting the $1320\text{--}1336\text{ cm}^{-1}$ peaks, where standard deviations do not go above 1 (Table 3).

Differences in the overall conversion within-group, for different methods are seen in Constic and ACTIVA (Bonferroni post-hoc, $p < 0.05$). Within Constic, comparing the $1320\text{--}1336$ to the $1320\text{--}1350\text{ cm}^{-1}$, differences were found ($p = 0.11$), but also between the $1320\text{--}1350$ and the $1636\text{--}1648\text{ cm}^{-1}$ ($p = 0.044$). With Activa, differences were found between the $1320\text{--}1346$ and the $1320\text{--}1350\text{ cm}^{-1}$ ($p = 0.006$).

Regarding kinetics, reaction extent graphs over time, after the start of the light exposure are shown in Fig 4. Results show conversion surpasses 50% of the final value even before light irradiation ends (at 20 s), reaching values higher than 80% after 100 s.

Discussion

In methacrylates, polymerisation occurs with an opening of a carbon-carbon double bond, leaving a free valence available for reaction with other monomers, which may then co-

Table 3. Peak heights and resulting D_C (%) at 1200 s, for the different peak selection methods.

	VF		Constic		ACTIVA	
	Peak difference	D_C (%)	Peak difference	D_C (%)	Peak difference	D_C (%)
1320–1336	0.068 (0.006)	74 (1) [1.8] ^{aA}	0.062 (0.001)	82 (0) [0.54] ^{aB}	0.078 (0.001)	64 (1) [2.1] ^{aC}
1320–1350	0.085 (0.004)	76 (3) [4.0] ^{aA}	0.066 (0.002)	88 (0) [0.65] ^{bB}	0.094 (0.001)	62 (1) [1.8] ^{bC}
1636–1648	0.075 (0.013)	73 (5) [6.9] ^{aA}	0.050 (0.005)	76 (3) [3.93] ^{aA}	0.053 (0.003)	71 (5) [7.3] ^{abA}

Means and standard deviations (SD) of peak heights, in absorbance units, between repetitions ($n = 3$) and final D_C (%) means, (SD) and [CV%] for each method, showing differences. Different lower-case letters indicate significant differences within the same column (Bonferroni, $p < 0.05$), while different capital letters indicate differences in the same rows (Games-Howell, $p > 0.05$).

<https://doi.org/10.1371/journal.pone.0252999.t003>

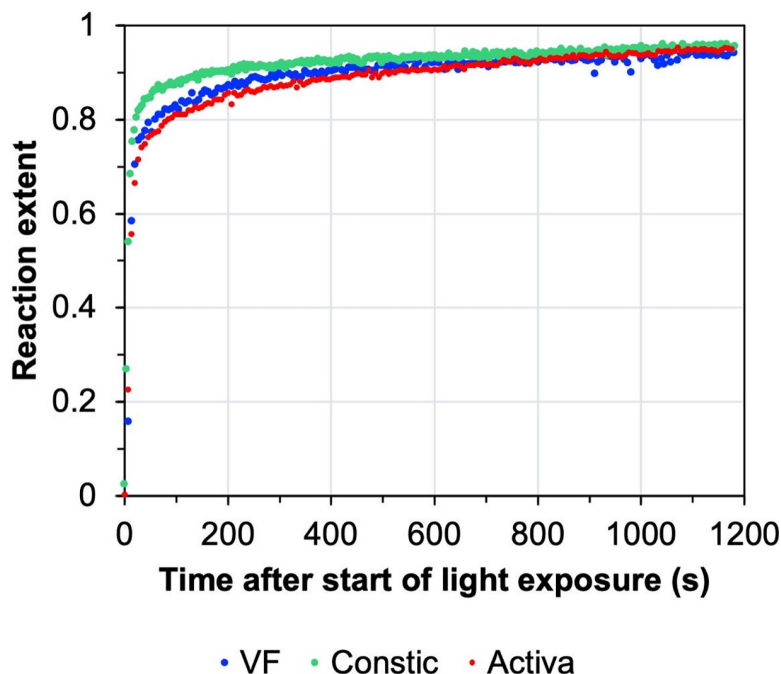


Fig 4. Reaction extent for VF, Constic and Activa. Graph indicates how far the reaction has gone towards its final value at each given time point. Reaction extent reaches 95% of the final value (determined by extrapolation of data versus inverse time to zero) by 1200 s for all the materials.

<https://doi.org/10.1371/journal.pone.0252999.g004>

polymerise. Absorbance changes include shifts in the 1700 cm^{-1} carbonyl region, loss of the $1635\text{--}1640\text{ cm}^{-1}$ [$\nu(\text{C}=\text{C})$] peak, and loss of the $1300\text{--}1320\text{ cm}^{-1}$ [$\nu(\text{C}-\text{O})$] doublet, with consequent shift to lower wavenumbers [13].

Using the $1635\text{--}1640\text{ cm}^{-1}$ peak to monitor this reaction is overshadowed by limiting factors. Firstly, O-H bending vibrations absorb at this wavenumber, invalidating the determination of D_C (%) in formulations which contain water [13, 15]. Many published studies measuring D_C (%) of dental adhesives using this peak exist, and the results should be cautiously interpreted as they are most probably biased [24–27]. Secondly, shifts in adjacent regions such as the carbonyl $1700\text{--}1750\text{ cm}^{-1}$ region affect the [$\nu(\text{C}=\text{C})$] peak band maxima [15]. The findings of this present study also suggest the 1320 cm^{-1} peak to be more reproducible and less prone to systematic errors, when compared to the variability associated with the $1635\text{--}1640\text{ cm}^{-1}$ peak region. Such results favour the recommendation of this peak for future D_C (%) measurements. Furthermore, in general, most studies use the $1635\text{--}1640/1610$ combination as the reaction peak and internal reference, respectively, in Bis-GMA, but also, erroneously in UDMA mixtures [28]. The 1610 cm^{-1} is an exclusively aromatic peak, not present in UDMA (Fig 1). Other studies have mentioned the use of the 1535 cm^{-1} bending vibration as the internal reference standard for UDMA D_C (%) calculations [29]. However, such peak is also subject to changes during polymerisation, as can be seen in the spectra of Activa. The 1320 cm^{-1} reaction peak and the reference baseline peaks at 1336 and 1350 cm^{-1} chosen in this study are valid for all methacrylates. Despite not being used by the majority of the studies in the dental field, this method has been validated by a considerable number of studies [11, 13, 30–33].

Peak selection is important and will affect not only the results within the same material, but also differences between the materials. This was verified when the $1636\text{--}1648\text{ cm}^{-1}$ peak

differences were used instead of the 1320 cm^{-1} peak differences, as the former failed to detect differences between the materials, which were present with the other two methods. D_C (%) differences are expected as the chemistry of the organic phase of the formulations and filler properties, included in each, differs greatly from material to material [28]. Such differences in specific monomer ratios, their reactivity and glass transition temperatures (T_g), viscosity of the mixture and also filler load impacts polymerisation kinetics, favouring or limiting reactions [34–36].

Considering D_C (%), Activa registered the lowest values, significantly different to VF and Constic when the 1320 cm^{-1} reaction peak method was used. Activa is a dual cure system (light and chemically activated polymerisation), and such systems tend to gradually improve their conversion rates to periods which can go up to 24 h [37, 38]. Besides from chemical and light cure, Activa is claimed to have polyacid components of the glass ionomer family, which undergo an acid-base neutralization reaction. This would mean that Activa has in fact three different setting mechanisms [39]. A triple cure system may be advantageous in scenarios where the material has to be placed in bulk and light activation cannot reach the bottom layers of the material [40]. However, having a mixture of dimethacrylates in a polyacid matrix may not have competing monomer reactivity as seen with other systems, thus decreasing conversion. These results are in line with previous investigations that determined the conversion upon light curing of Activa, which was described as poor [41]. When comparing results achieved with VF in previous studies, their final conversion values were inferior to what was found in this study [42, 43]. Differences may be explained by material thickness and peak selection variability, confirmed with this study. As for Constic, this was the first known study to measure its D_C (%). These restoratives belong to a newer class of materials coined self-adhesive composites, which are yet to achieve commercial breakthrough, and are currently being studied [44, 45]. As these materials are formulated with an aim to surpass the need of a dental adhesive, they should come in contact with the tooth and achieve fast polymerisation rates with sufficient monomer-polymer conversion. This allows a densely cross-linked network formation which achieves its final properties, being able to withstand stresses resulting from forces applied in the oral cavity, resistance to degradation and prevention of monomer elution which raises toxicity concerns [34, 46]. Materials which aspire biomimetism should limit their toxicity, which, in this case, can be achieved by reducing the free-monomer elution owing to incomplete polymerisation [47, 48].

The extent of the reaction was similar for all the materials tested, although Constic reached higher initial values, which is in accordance with its polymerisation profile, having achieved a higher final degree of conversion when compared to the other materials. Furthermore, reaction extent results prove that a peak base is not required [11].

The difference spectra shown in this study confirm that the changes seen during the time of spectral acquisition are mainly due to the polymerisation reaction of methacrylates, corroborating findings from previous studies [11, 13]. This is a simple and useful method to understand peak shifts during setting kinetics, although it can be used for a variety of different studies such as changes upon reaction of different materials, biological samples before and after treatment, material mixtures or aging processes [49, 50].

As the ATR-FTIR is highly sensitive to change, factors like atmospheric vapours, such as water, or carbon dioxide from breathing, near the sample measurement, are known to induce noise interference effects on the spectra. These will be observed in the $1700\text{--}1600\text{ cm}^{-1}$ region, affecting the $1635\text{--}1640\text{ cm}^{-1}$ [$\delta(\text{O-H})$] bend, and also around $3300\text{--}3500\text{ cm}^{-1}$ [$\nu(\text{O-H})$] for water, or at 2400 cm^{-1} [$\nu(\text{O=C=O})$] for carbon dioxide [51]. This may be what was seen in the difference spectra of the materials, further strengthening the need to avoid selecting this peak to monitor conversion in methacrylates. When working with ATR-FTIR systems there is

increased difficulty in guaranteeing that there are no variations in water content or temperature during the time of study, as it may not be possible to close the lid of instrument while using ATR accessories, and the sample needs to be accessed for light curing. Atmospheric vapours can thus create noise effects. Instrument manufacturers have tried overcoming this problem by reducing background effects due to water, however this is easily achieved by using the 1320 cm^{-1} peak over the $1635\text{--}1640\text{ cm}^{-1}$ region.

These results are also considered highly repeatable, when the appropriate reaction peak/reference are chosen, and are in line with past findings using the ATR technique, that found CV % lower than 2 [52]. This confirms that the ATR-FTIR technique is adequate and sensitive to study polymerisation kinetics of dental composites, and larger variations within the same subset are not expected. Methods of composite preparation should guarantee homogeneity for bulk preparation and packaging [53]. Although heterogeneity may occur in composites, and often results from different filler dispersion within the resin phase, which may lead to differences in light scattering [54]. Within sample variations can also be higher when studying material changes over time [19].

Conclusion

The ATR-FTIR technique to characterise the polymerisation reaction of methacrylates gives reproducible, sound, results when it is used with the correct peak selection. The 1320 cm^{-1} [$\nu(\text{C-O})$] gives reproducible results with less systematic errors, in what concerns variability within repetitions, compared to the traditional 1636 cm^{-1} [$\nu(\text{C}=\text{C})$]. Calculation of parameters such as DC (%) is largely affected by the peak selection, with material differences being evident only with the 1320 cm^{-1} peak. It is therefore possible to conclude that to assess polymerisation in methacrylates, the 1320 cm^{-1} peak is recommended.

Supporting information

S1 Dataset. Raw data: Monomers, dental composites and kinetics.
(XLSX)

Author Contributions

Conceptualization: António H. S. Delgado, Anne M. Young.

Data curation: Anne M. Young.

Formal analysis: Anne M. Young.

Investigation: António H. S. Delgado, Anne M. Young.

Methodology: António H. S. Delgado, Anne M. Young.

Supervision: Anne M. Young.

Writing – original draft: António H. S. Delgado.

Writing – review & editing: Anne M. Young.

References

1. Khan AS, Khalid H, Sarfraz Z, Khan M, Iqbal J, Muhammad N, et al. Vibrational spectroscopy of selective dental restorative materials. *Appl Spectrosc Rev.* 2017; 52: 507–540. <https://doi.org/10.1080/05704928.2016.1244069>

2. Liu L, Gong D, Bratasz L, Zhu Z, Wang C. Degradation markers and plasticizer loss of cellulose acetate films during ageing. *Polym Degrad Stab*. 2019; 168: 108952. <https://doi.org/10.1016/j.polymdegradstab.2019.108952>
3. Chalmers JM, Everall NJ. FTIR, FT-Raman and chemometrics: Applications to the analysis and characterisation of polymers. *TrAC—Trends Anal Chem*. 1996; 15: 18–25. [https://doi.org/10.1016/0165-9936\(96\)88033-2](https://doi.org/10.1016/0165-9936(96)88033-2)
4. Ferracane JL, Hilton TJ, Stansbury JW, Watts DC, Silikas N, Ilie N, et al. Academy of Dental Materials guidance—Resin composites: Part II—Technique sensitivity (handling, polymerization, dimensional changes). *Dent Mater*. 2017; 33: 1171–1191. <https://doi.org/10.1016/j.dental.2017.08.188> PMID: 28917571
5. Ferracane JL. Resin composite—State of the art. *Dent Mater*. 2011; 27: 29–38. <https://doi.org/10.1016/j.dental.2010.10.020> PMID: 21093034
6. Scherzer T. Depth Profiling of the Degree of Cure during the Photopolymerization of Acrylates Studied by Real-Time FT-IR Attenuated Total Reflection Spectroscopy. *Appl Spectrosc*. 2002; 56: 1403–1412. <https://doi.org/10.1366/00037020260377698>
7. Zhang Y, Wang Y. Photopolymerization of phosphoric acid ester-based self-etch dental adhesives. *Dent Mater J*. 2013; 32: 10–18. <https://doi.org/10.4012/dmj.2012-108> PMID: 23370865
8. Okulus Z, Buchwald T, Szybowicz M, Voelkel A. Study of a new resin-based composites containing hydroxyapatite filler using Raman and infrared spectroscopy. *Mater Chem Phys*. 2014; 145: 304–312. <https://doi.org/10.1016/j.matchemphys.2014.02.012>
9. Walters NJ, Xia W, Salih V, Ashley PF, Young AM. Poly(propylene glycol) and urethane dimethacrylates improve conversion of dental composites and reveal complexity of cytocompatibility testing. *Dent Mater*. 2016; 32: 264–277. <https://doi.org/10.1016/j.dental.2015.11.017> PMID: 26764174
10. Denis AB, Diagone CA, Plepis AMG, Viana RB. Kinetic Parameters during Bis-GMA and TEGDMA Monomer Polymerization by ATR-FTIR: The Influence of Photoinitiator and Light Curing Source. *J Spectrosc*. 2016; 2016. <https://doi.org/10.1155/2016/6524901>
11. Young AM, Rafeeka SA, Howlett JA. FTIR investigation of monomer polymerisation and polyacid neutralisation kinetics and mechanisms in various aesthetic dental restorative materials. *Biomaterials*. 2004; 25: 823–833. [https://doi.org/10.1016/s0142-9612\(03\)00599-4](https://doi.org/10.1016/s0142-9612(03)00599-4) PMID: 14609671
12. Young AM. FTIR investigation of polymerisation and polyacid neutralisation kinetics in resin-modified glass-ionomer dental cements. *Biomaterials*. 2002; 23: 3289–3295. [https://doi.org/10.1016/s0142-9612\(02\)00092-3](https://doi.org/10.1016/s0142-9612(02)00092-3) PMID: 12102200
13. Delgado AH, Young AM. Modelling ATR-FTIR Spectra of Dental Bonding Systems to Investigate Composition and Polymerisation Kinetics. *Materials (Basel)*. 2021; 14: 760. <https://doi.org/10.3390/ma14040760> PMID: 33562837
14. Carvalho CN, Lanza MDS, Dourado LG, Carvalho EM, Bauer J. Impact of Solvent Evaporation and Curing Protocol on Degree of Conversion of Etch-and-Rinse and Multimode Adhesives Systems. *Int J Dent*. 2019; 2019. <https://doi.org/10.1155/2019/5496784> PMID: 31097965
15. Pianelli C, Devaux J, Bebelman S, Leloup G. The micro-Raman spectroscopy, a useful tool to determine the degree of conversion of light-activated composite resins. *J Biomed Mater Res*. 1999; 48: 675–681. [https://doi.org/10.1002/\(sici\)1097-4636\(1999\)48:5<675::aid-jbm11>3.0.co;2-p](https://doi.org/10.1002/(sici)1097-4636(1999)48:5<675::aid-jbm11>3.0.co;2-p) PMID: 10490681
16. Liaqat S, Aljabo A, Khan M, Nuba H, Bozec L, Ashley P, et al. Characterization of Dentine to Assess Bond Strength of Dental Composites. *Materials (Basel)*. 2015; 8: 2110–2126. <https://doi.org/10.3390/ma8052110>
17. Collares FM, Portella FF, Leitune VCB, Samuel SMW. Discrepancies in degree of conversion measurements by FTIR. *Braz Oral Res*. 2014; 28: 9–15. <https://doi.org/10.1590/S1806-83242013000600002>
18. Hofko B, Alavi MZ, Grothe H, Jones D, Harvey J. Repeatability and sensitivity of FTIR ATR spectral analysis methods for bituminous binders. *Mater Struct Constr*. 2017; 50: 1–15. <https://doi.org/10.1617/s11527-017-1059-x>
19. Hofko B, Porot L, Falchetto Cannone A, Poulikakos L, Huber L, Lu X, et al. FTIR spectral analysis of bituminous binders: reproducibility and impact of ageing temperature. *Mater Struct Constr*. 2018; 51: 1–16. <https://doi.org/10.1617/s11527-018-1170-7>
20. Par M, Gamulin O, Marovic D, Klaric E, Tarle Z. Raman spectroscopic assessment of degree of conversion of bulk-fill resin composites-changes at 24 hours post cure. *Oper Dent*. 2015; 40: E92–E101. <https://doi.org/10.2341/14-091-L> PMID: 25275961
21. Jones RR, Hooper DC, Zhang L, Wolverson D, Valev VK. Raman Techniques: Fundamentals and Frontiers. *Nanoscale Research Letters*. Springer New York LLC; 2019. pp. 1–34. <https://doi.org/10.1186/s11671-018-2843-4> PMID: 30607516

22. Alotaibi J, Saji S, Swain M V. FTIR characterization of the setting reaction of biodentine™. *Dent Mater.* 2018; 34: 1645–1651. <https://doi.org/10.1016/j.dental.2018.08.294> PMID: 30219594
23. Hofmann MP, Young AM, Gbureck U, Nazhat SN, Barralet JE. FTIR-monitoring of a fast setting brushite bone cement: Effect of intermediate phases. *J Mater Chem.* 2006; 16: 3199–3206. <https://doi.org/10.1039/b603554j>
24. Barbosa MO, de Carvalho RV, Demarco FF, Ogliari FA, Zanchi CH, Piva E, et al. Experimental self-etching HEMA-free adhesive systems: cytotoxicity and degree of conversion. *J Mater Sci Mater Med.* 2015; 26: 1–8. <https://doi.org/10.1007/s10856-014-5370-6> PMID: 25589203
25. Tichy A, Hosaka K, Abdou A, Nakajima M, Tagami J. Degree of Conversion Contributes to Dentin Bonding Durability of Contemporary Universal Adhesives. *Oper Dent.* 2020; 19–165–L. <https://doi.org/10.2341/18-230-C> PMID: 31034347
26. Borges BCD, Souza E, Brandt WC, Loguercio AD, Majr M, Puppini-Rontani RM, et al. Degree of conversion of simplified contemporary adhesive systems as influenced by extended air-activated or passive solvent volatilization modes. *Oper Dent.* 2012; 37: 246–252. <https://doi.org/10.2341/11-248-L> PMID: 22313268
27. Arrais CAG, Pontes FM, dos Santos LPS, Leite ER, Giannini M. Degree of conversion of adhesive systems light-cured by LED and halogen light. *Braz Dent J.* 2007; 18: 54–59. <https://doi.org/10.1590/s0103-64402007000100012> PMID: 17639202
28. Bolaños-Carmona V, Benavides-Reyes C, González-López S, González-Rodríguez P, Alvarez-Lloret P. Influence of spectroscopic techniques on the estimation of the degree of conversion of bulk-fill composites. *Oper Dent.* 2020; 45: 92–103. <https://doi.org/10.2341/18-095-L> PMID: 31750799
29. Guerra RM, Durán I, Ortiz P. FTIR monomer conversion analysis of UDMA-based dental resins. *J Oral Rehabil.* 1996; 23: 632–637. <https://doi.org/10.1111/j.1365-2842.1996.tb00903.x> PMID: 8890065
30. Agha A, Parker S, Patel M. Polymerization shrinkage kinetics and degree of conversion of commercial and experimental resin modified glass ionomer luting cements (RMGICs). *Dent Mater.* 2020; 36: 893–904. <https://doi.org/10.1016/j.dental.2020.04.010> PMID: 32461097
31. Aljabo A, Xia W, Liaqat S, Khan MA, Knowles JC, Ashley P, et al. Conversion, shrinkage, water sorption, flexural strength and modulus of re-mineralizing dental composites. *Dent Mater.* 2015; 31: 1279–1289. <https://doi.org/10.1016/j.dental.2015.08.149> PMID: 26361809
32. Panpisut P, Liaqat S, Zacharaki E, Xia W, Petridis H, Young AM. Dental composites with calcium / strontium phosphates and polylysine. Mishra YK, editor. *PLoS One.* 2016; 11: e0164653. <https://doi.org/10.1371/journal.pone.0164653> PMID: 27727330
33. Kangwankai K, Sani S, Panpisut P, Xia W, Ashley P, Petridis H, et al. Monomer conversion, dimensional stability, strength, modulus, surface apatite precipitation and wear of novel, reactive calcium phosphate and polylysine-containing dental composites. *PLoS One.* 2017; 12: 1–19. <https://doi.org/10.1371/journal.pone.0187757> PMID: 29136013
34. Stansbury JW. Dimethacrylate network formation and polymer property evolution as determined by the selection of monomers and curing conditions. *Dent Mater.* 2012; 28: 13–22. <https://doi.org/10.1016/j.dental.2011.09.005> PMID: 22192248
35. Algamaiah H, Silikas N, Watts DC. Conversion kinetics of rapid photo-polymerized resin composites. *Dent Mater.* 2020; 36: 1266–1274. <https://doi.org/10.1016/j.dental.2020.07.008> PMID: 32798046
36. Abu-Elenain DA, Lewis SH, Stansbury JW. Property evolution during vitrification of dimethacrylate photopolymer networks. *Dent Mater.* 2013; 29: 1173–1181. <https://doi.org/10.1016/j.dental.2013.09.002> PMID: 24080378
37. Bandéca MC, El-Mowafy O, Saade EG, Rastelli ANS, Bagnato VS, Porto-Neto ST. Changes on degree of conversion of dual-cure luting light-cured with blue LED. *Laser Phys.* 2009; 19: 1050–1055. <https://doi.org/10.1134/S1054660X09050302>
38. Yan YL, Kim YK, Kim K-H, Kwon T-Y. Changes in Degree of Conversion and Microhardness of Dental Resin Cements. *Oper Dent.* 2010; 35: 203–210. <https://doi.org/10.2341/09-174-L> PMID: 20420064
39. Croll TP, Berg JH, Donly KJ. Dental repair material: a resin-modified glass-ionomer bioactive ionic resin-based composite. *Compend Contin Educ Dent.* 2015; 36: 60–65. PMID: 25822408
40. Kim YK, Kim KH, Kwon TY. Setting Reaction of Dental Resin-Modified Glass Ionomer Restoratives as a Function of Curing Depth and Postirradiation Time. *J Spectrosc.* 2015; 2015. <https://doi.org/10.1155/2015/462687>
41. Koutroulis A, Kuehne SA, Cooper PR, Camilleri J. The role of calcium ion release on biocompatibility and antimicrobial properties of hydraulic cements. *Sci Rep.* 2019; 9: 1–10. <https://doi.org/10.1038/s41598-018-37186-2> PMID: 30626917

42. Czasch P, Ilie N. In vitro comparison of mechanical properties and degree of cure of a self-adhesive and four novel flowable composites. *J Adhes Dent*. 2013; 15: 229–236. <https://doi.org/10.3290/j.jad.a29530> PMID: 23560255
43. de Araujo LOF, Barreto O, de Mendonça AAM, França R. Assessment of the degree of conversion in light-curing orthodontic resins with various viscosities. *Appl Adhes Sci*. 2015; 3: 26. <https://doi.org/10.1186/s40563-015-0055-z>
44. Yao C, Ahmed MH, Zhang F, Mercelis B, Van Landuyt KL, Huang C, et al. Structural/Chemical Characterization and Bond Strength of a New Self-Adhesive Bulk-fill Restorative. *J Adhes Dent*. 2020; 22: 85–97. <https://doi.org/10.3290/j.jad.a44000> PMID: 32030379
45. Lohbauer U, Belli R. The Mechanical Performance of a Novel Self-Adhesive Restorative Material. *J Adhes Dent*. 2020; 22: 47–58. <https://doi.org/10.3290/j.jad.a43997> PMID: 32030375
46. Barszczewska-Rybarek IM. A guide through the dental dimethacrylate polymer network structural characterization and interpretation of physico-mechanical properties. *Materials*. MDPI AG; 2019. p. 4057. <https://doi.org/10.3390/ma12244057> PMID: 31817410
47. Makkar H, Verma SK, Panda PK, Jha E, Das B, Mukherjee K, et al. In Vivo Molecular Toxicity Profile of Dental Bioceramics in Embryonic Zebrafish (*Danio rerio*). *Chem Res Toxicol*. 2018; 31: 914–923. <https://doi.org/10.1021/acs.chemrestox.8b00129> PMID: 30058326
48. Makkar H, Verma SK, Panda PK, Pramanik N, Jha E, Suar M. Molecular insight to size and dose-dependent cellular toxicity exhibited by a green synthesized bioceramic nanohybrid with macrophages for dental applications. *Toxicol Res (Camb)*. 2018; 7: 959–969. <https://doi.org/10.1039/c8tx00112j> PMID: 30310673
49. Gezici O, Demir I, Demircan A, Ünlü N, Karaarslan M. Subtractive-FTIR spectroscopy to characterize organic matter in lignite samples from different depths. *Spectrochim Acta—Part A Mol Biomol Spectrosc*. 2012; 96: 63–69. <https://doi.org/10.1016/j.saa.2012.05.004> PMID: 22652543
50. Derenne A, Verdonck M, Goormaghtigh E. The effect of anticancer drugs on seven cell lines monitored by FTIR spectroscopy. *Analyst*. 2012; 137: 3255–3264. <https://doi.org/10.1039/c2an35116a> PMID: 22673795
51. Zou Y, Ma G. A new criterion to evaluate water vapor interference in protein secondary structural analysis by FTIR spectroscopy. *Int J Mol Sci*. 2014; 15: 10018–10033. <https://doi.org/10.3390/ijms150610018> PMID: 24901531
52. Cateto CA, Barreiro MF, Rodrigues AE. Monitoring of lignin-based polyurethane synthesis by FTIR-ATR. *Ind Crops Prod*. 2008; 27: 168–174. <https://doi.org/10.1016/j.indcrop.2007.07.018>
53. Aminoroaya A, Esmaeely Neisiany R, Nouri Khorasani S, Panahi P, Das O, Ramakrishna S. A Review of Dental Composites: Methods of Characterizations. *ACS Biomater Sci Eng*. 2020; 6: 3713–3744. <https://doi.org/10.1021/acsbiomaterials.0c00051> PMID: 33463319
54. Pratap B, Gupta RK, Bhardwaj B, Nag M. Resin based restorative dental materials: characteristics and future perspectives. *Jpn Dent Sci Rev*. 2019; 55: 126–138. <https://doi.org/10.1016/j.jdsr.2019.09.004> PMID: 31687052